# Miss the Point: Targeted Adversarial Attack on Multiple Landmark Detection

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Abstract. Recent methods in multiple landmark detection based on deep convolutional neural networks (CNNs) reach high accuracy and improve traditional clinical workflow. However, the vulnerability of CNNs to adversarial-example attacks can be easily exploited to break classification and segmentation tasks. This paper is the first to study how fragile a CNN-based model on multiple landmark detection to adversarial perturbations. Specifically, we propose a novel Adaptive Targeted Iterative FGSM (ATI-FGSM) attack against the state-of-the-art models in multiple landmark detection. The attacker can use ATI-FGSM to precisely control the model predictions of arbitrarily selected landmarks, while keeping other stationary landmarks still, by adding imperceptible perturbations to the original image. A comprehensive evaluation on a public dataset for cephalometric landmark detection demonstrates that the adversarial examples generated by ATI-FGSM break the CNN-based network more effectively and efficiently, compared with the original Iterative FGSM attack. Our work reveals serious threats to patients' health. Furthermore, we discuss the limitations of our method and provide potential defense directions, by investigating the coupling effect of nearby landmarks, i.e., a major source of divergence in our experiments. Our source code is available at https://github.com/qsyao/attack\_landmark\_detection.

Keywords: Landmark Detection  $\cdot$  Adversarial Examples.

## 1 Introduction

Multiple landmark detection is an important pre-processing step in therapy planning and intervention, thus it has attracted great interest from academia and industry [26,27,13,22]. It has been successfully applied to many practical medical clinical scenarios such as knee joint surgery [23], orthognathic and maxillofacial

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<sup>\*</sup> This work is supported in part by the Youth Innovation Promotion Association CAS (grant 2018135) and Alibaba Group through Alibaba Innovative Research Program.

surgeries [3], carotid artery bifurcation [24], pelvic trauma surgery [2], bone age estimation [5]. Also, it is an important step in medical imaging analysis [16,12,10], e.g., registration or initialization of segmentation algorithms.

Recently, CNN-based methods has rapidly become a methodology of choice for analyzing medical images. Compared with expert manual annotation, CNN achieves high accuracy and efficiency at a low-cost [3], showing great potential in multiple landmark detection. Chen et al. [3] use cascade U-Net to launch a two-stage heatmap regression [16], which is widely used in medical landmark detection. Zhong et al. [25] accomplish the task by regressing the heatmap and coordinate offset maps at the same time.

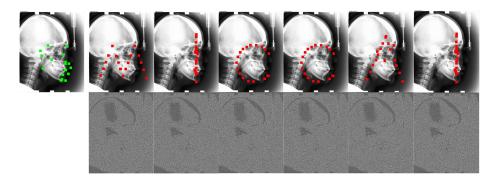
However, the vulnerability of CNNs to adversarial attacks can not be overlooked [19]. The attacks are legitimate examples with human-imperceptible perturbations, which attempt to fool a trained model to make incorrect predictions [7]. Goodfellow et al. [6] develop a fast gradient sign method (FGSM) to generate perturbations by back-propagating the adversarial gradient induced by an intended incorrect prediction. Kurakin et al. [9] extend it to Targeted Iterative FGSM by generating the perturbations iteratively to hack the network to predict the attacker desired target class. Adversarial attacks against CNN models become a real threat not only in classification tasks but also in segmentation and localization [21]. The dense adversary generation (DAG) algorithm proposed in [21] by Xie et al. aims to force the CNN based network to predict all pixels to target classes without  $L_{\infty}$  norm limitation. Other works that apply the adversarial attack to classification and segmentation [14,7,15] hack the network in both targeted and non-targeted manners with a high success rate.

A targeted attack on landmark detection is stealthy and disastrous as the detection precision is tightly related to a patient's health during surgical intervention, clinical diagnosis or measurement, etc. To study the vulnerability of landmark detection systems, we propose an approach for targeted attack against CNN-based models in this paper. Our main contributions are:

- 1. A simple yet representative multi-task U-Net to detect multiple landmarks with high precision and high speed.
- 2. The first targeted adversarial attack against multiple landmark detection, to the best of our knowledge, which exposes the great vulnerability of medical images against adversarial attack.
- 3. An Adaptive Targeted Iterative FGSM (ATI-FGSM) algorithm that makes the attack more effective and efficient than the standard I-FGSM.
- 4. A comprehensive evaluation of the proposed algorithm to attack the land-mark detection and understanding its limitations.

## 2 Multi-task U-Net for multiple landmark detection

Existing approaches for multiple landmark detection use a heatmap [16,25] and/or coordinate offset maps [3] to represent a landmark and then a U-Net-like network [17] is learned to predict the above map(s), which are post-processed



**Fig. 1.** An example of targeted adversarial attack against multiple landmark detection in a cephalometric radiograph. By adding imperceptible perturbations to the original image (left most), we arbitrarily position 19 landmarks to form the letters 'MICCAI'. The perturbation is magnified by a factor of 8 for visualization.

to derive the final landmark location. Here we implement a multi-task U-Net to predict both heatmap and offset maps simultaneously and treat this network as our target model to attack.

For the  $i^{th}$  landmark located at  $(x_i, y_i)$  in an image X, its heatmap  $Y_i^h$  is computed as a Gaussian function  $Y_i^h(x,y) = exp[-\frac{1}{2\sigma^2}((x-x_i)^2+(y-y_i)^2)]$  and its x-offset map  $Y_i^{o_x}$  predicts the relative offset vector  $Y_i^{o_x} = (x-x_i)/\sigma$  from x to the corresponding landmark  $x_i$ . Similarly, its y-offset map  $Y_i^{o_y}$  is defined. Different from [25], we truncate the map functions to zero for the pixels whose  $Y_i^h(x,y) \geq 0.6$ . We use a binary cross-entropy loss  $L^h$  to punish the divergence of predicted and ground-truth heatmaps, and an  $L_1$  loss  $L^o$  to punish the difference in coordinate offset maps. Here is the loss function  $L_i$  for the  $i^{th}$  landmark:

$$L_{i}(Y_{i}, g_{i}(X, \theta)) = \alpha L_{i}^{h}(Y_{i}^{h}, g_{i}^{h}(X, \theta)) + sign(Y_{i}^{h}) \sum_{o \in \{o_{x}, o_{y}\}} L_{i}^{o}(Y_{i}^{o}, g_{i}^{o}(X, \theta))$$
(1)

where  $g_i^h(X,\theta)$  and  $g_i^o(X,\theta)$  are the networks that predict heatmaps and coordinate offset maps, respectively;  $\theta$  is the network parameters;  $\alpha$  is a balancing coefficient, and  $sign(\cdot)$  is a sign function which is used to ensure that only the area highlighted by heatmap is included for calculation.

To deal with the limited data problem, we fine-tune the encoder of U-Net initialized by the VGG19 network [18] pretrained on ImageNet [4]. In the test phase, a majority-vote for candidate landmarks is conducted among all pixels with heatmap value  $g_i^h(X,\theta) \geq 0.6$ , according to their coordinate offset maps in  $g_i^o(X,\theta)$ . The winning position in the  $i^{th}$  channel is the final predicted  $i^{th}$  landmark [3]. The whole framework is illustrated in Fig. 2.

## 3 Adversarial attack on multiple landmark detection

A general formulation. Given an original image  $X_0$ , the attacker attempts to generate a small perturbation P, such that (i) P is not perceptible to human

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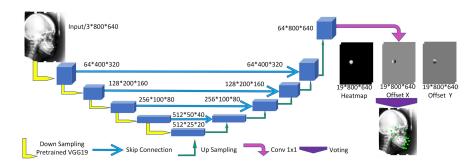


Fig. 2. Overview of our Multi-Task U-Net. For coordinate offset maps, we only focus on the areas with heatmap value  $\geq 0.6$ . We set the value of the other areas to 0.

beings and (ii) for the perturbed image, i.e.,  $X = X_0 + P$ , its model prediction g(X) is entirely controlled by the adversary. Follow the convention, we model the non-perceptive property of the perturbation as a constraint that the  $L_{\infty}$  norm of  $P = X - X_0$  is less than  $\epsilon$ . In the context of targeted adversarial attack on multiple landmark detection, taking full control of the model prediction means that, for an image with K landmarks, the attacker is able to move N arbitrary target landmarks to desired locations while leaving the remaining (K - N) landmarks stationary.

We denote that the index set of all landmarks is given by  $\Omega = \{1, 2, ..., K\}$  and is split into two complementary subsets:  $\mathcal{T} = \{t_1, t_2, ..., t_N\}$  for the indices of target landmarks and  $\mathcal{S} = \{s_1, s_2, ..., s_{K-N}\}$  for the indices of stationary landmarks. We model the adversarial attack against the model prediction as minimizing the Euclidean distance between any target landmark  $g_t(X, \theta)$  w.r.t. its corresponding adversarial target location  $(x_t, y_t)$ , while keeping any stationary landmark  $g_s(X, \theta)$  close to its original location  $(x_s, y_s)$ :

$$\min_{X} \sum_{t \in \mathcal{T}} ||g_t(X, \theta) - (x_t, y_t)||_2 + \sum_{s \in \mathcal{S}} ||g_s(X, \theta) - (x_s, y_s)||_2$$

$$s.t. \quad ||P||_{\infty} = ||X - X_0||_{\infty} \le \epsilon, X \in [0, 256]^{C \times H \times M} \tag{2}$$

To accommodate the map-based landmark representation, the attacker sets an adversarial heatmap  $Y_t^h$  and coordinate offset maps  $Y_t^o$  based on the desired position. We then replace the corresponding  $Y_i^h$  and  $Y_i^o$  with  $Y_t^h$  and  $Y_t^o$  in Eq. (1). For a stationary landmark, we use heatmap  $g^h(X, \theta)$  and coordinate offset maps  $g^o(X, \theta)$  predicted by the original network as ground truth  $Y_s$ .

$$\min_{X} L(Y, g(X, \theta)) = \sum_{t \in \mathcal{T}} L_t(Y_t, g_t(X, \theta)) + \sum_{s \in \mathcal{S}} L_s(Y_s, g_s(X, \theta)). \tag{3}$$

Targeted iterative FGSM [9]. Targeted iterative FGSM is an enhanced version of Targeted FGSM [9], increasing the attack effectiveness by iteratively

tuning an adversarial example. We adapt Targeted iterative FGSM from the classification task to multiple landmark detection task by revising its loss function L in Eq. (3). As L decreases, the predicted heatmaps and coordinate offset maps converge to the adversarial ones. This moves the targeted landmark to the desired position while leaving the stationary landmarks at their original positions. The process of an adversarial example generation, i.e., decreasing L, is given by:

$$X_0^{adv} = X_0, \quad X_{i+1}^{adv} = clip[X_i^{adv} - \eta \cdot sign(\nabla_{X_i^{adv}} L(Y, g(X_i^{adv}, \theta))), \epsilon]$$
(4)

$$L^{ada}(Y, g(X, \theta)) = \sum_{t \in \mathcal{T}} \alpha_t \cdot L_t(Y_t, g_t(X, \theta)) + \sum_{s \in \mathcal{S}} \alpha_s \cdot L_s(Y_s, g_s(X, \theta))$$

$$\alpha_j = L_j / mean(L(Y, g(X, \theta))) \quad j \in [1, K]$$
(5)

where  $L(Y, g(X, \theta))$  is calculated by Eq. (3). The new  $L^{ada}(Y, g(X, \theta))$ , rather than the original  $L(Y, g(X, \theta))$ , is differentiated to generate gradient map in each iteration of our proposed ATI-FGSM attack.

## 4 Experiments

Dataset and implementation details. We use a public dataset for cephalometric landmark detection, provided in IEEE ISBI 2015 Challenge [20], which contains 400 cephalometric radiographs. Each radiograph has 19 manually labeled landmarks of clinical anatomical significance by the two expert doctors. We take the average annotations by two doctors as the ground truth landmarks. The image size is  $1935 \times 2400$ , while the pixel spacing is 0.1mm. The radiographs are split to 3 sets (Train, Test1, Test2) according to the official website, whose numbers of images are 150, 150, 100 respectively. We use mean radial error (MRE) to measure the Euclidean distance between two landmarks and successful detection

**Table 1.** Comparison of five state-of-the-art methods and our proposed multi-task U-Net on the IEEE ISBI 2015 Challenge [20] datasets. We use the proposed multi-task U-Net as the target model to hack.

Model		Tes	t Datas	et 1		Test Dataset 2						
	MRE	2mm	2.5mm	$3 \mathrm{mm}$	4mm	MRE	2mm	2.5mm	$3 \mathrm{mm}$	4mm		
Ibragimov et al. [8]	1.87	71.70	77.40	81.90	88.00	-	62.74	70.47	76.53	85.11		
Lindner et al. [11]	1.67	74.95	80.28	84.56	89.68	-	66.11	72.00	77.63	87.42		
Arik et al. [1]	-	75.37	80.91	84.32	88.25	-	67.68	74.16	79.11	84.63		
Zhong et al. [25]	1.14	86.74	92.00	94.71	97.82	-	-	-	-	-		
Chen et al. [3]	1.17	86.67	92.67	95.54	98.53	1.48	75.05	82.84	88.53	95.05		
Proposed	1.24	84.84	90.52	93.75	97.40	1.61	71.89	80.63	86.36	93.68		

rate (SDR) in four radii (2mm, 2.5mm, 3mm, 4mm), which are designated by the official challenge, to measure the performance for both adversarial attack and multi-task U-Net. As MRE can be affected by extreme values, we report median radial error (MedRE) for adversarial attacks additionally. Our multi-task U-Net is trained on a Quadro RTX 8000 GPU and optimized by the Adam optimizer with default settings. We set  $\sigma=40$ . The learning rate is set to 1e-3 and decayed by 0.1 every 100 epochs. After multiple trials, we select  $\alpha=1.0$  for heatmaps in Eq. (1). We resize the input image to  $800\times640$  and normalize the values to [-1, 1]. Finally, we train our multi-task U-Net for 230 epochs with a batch size of 8. In the adversarial attack phase, we set  $\eta=0.05$  in Eq. (4) for the iterative increment of perturbations in our experiments.

**Detection performance of multi-task U-Net.** We report the performance of our multi-task U-Net and compare it with five state-of-the-art methods [8,11,1,25,3] in Table 1. Our proposed approach predicts the positions of the landmarks only by regressing heatmaps and coordinate offset maps, which are widely used in the landmark detection task [16,25,3]. In terms of performance, our approach is close to the state-of-the-art methods [3,25] and significantly ahead of the IEEE ISBI 2015 Challenge championship [11].

#### 4.1 Performance of ATI-FSGM

We evaluate the performance of the ATI-FGSM attack against the multi-task U-Net. To simulate the hardest scenario, our evaluation is established in a completely random setting. For each raw image in the two test datasets (250 images in total), we repeat twice the following: First randomly select a number of landmarks as targeted landmarks, leaving the rest as stationary landmarks. Then the target coordinates are randomly generated for the selected landmarks, from a huge rectangle ( $x \in [100, 600], y \in [250, 750]$ ). So we have 500 attack attempts in total. This high level of randomness introduces significantly difficult cases for the adversarial attack. We generate adversarial examples by iterating 300 times (unless otherwise specified), under the constraint that  $\epsilon = 8$ . As in Fig. 3, the adversarial example moves the targeted landmarks (red) to the target positions (green) by fooling the network to generate incorrect heatmaps and coordinate

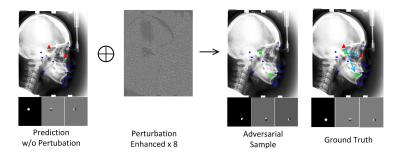


Fig. 3. An example of a targeted two-landmarks adversarial attack using our proposed Adaptive Targeted Iterative FGSM (ATI-FGSM). Red points highlight the predicted landmarks by the model on the original image, which are very close to the ground truth landmarks. After adding imperceptible perturbation to the input image, the model predicts the green points as the corresponding landmark positions. The green points are far away from their original positions (red), and can be controlled by the adversary. On the other hand, all other stationary points (blue) remain close to their original positions.

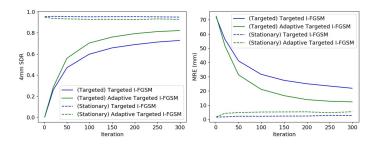


Fig. 4. Comparison between TI-FGSM and our ATI-FGSM. Our ATI-FGSM can arbitrarily move targeted landmarks away more efficiently and keep most of stationary landmarks in their original positions.

offset maps. The small perturbation between the adversarial example and raw radiograph is hard to percept by humans. As in Table 2, the goals of our adversarial attack are quickly achieved in 300 iterations, and continuously optimized for the remaining 700 iterations. Evidently, the widely used method like heatmap regression [16] for landmark detection is very vulnerable to our attack.

Attack performance vs perturbation strength. We evaluate our method under different constraints of perturbation intensity. Table 2 shows that the adversarial examples generated by our method can achieve low MedRE and high 4mm SDR by attacking randomly targeted landmarks successfully, while keeping most of the stationary landmarks at their original positions. Moreover, as the  $L_{\infty}$  norm constraint relaxes, MRE drops rapidly with more difficult landmarks hacked, but a few stationary landmarks are moved away.

**Table 2.** Attack performance at different iterations and  $L_{\infty}$  constraints.

# of iterations ( $\epsilon = 8$ )	1	20	50	100	150	200	250	300	400	600	750	1000
Targeted MRE (mm)		51.7	33.0	22.2	18.0	15.5	14.1	12.3	11.5	10.7	9.9	9.1
Stationary MRE (mm)		4.43	6.23	5.21	5.49	5.07	5.00	5.31	5.63	5.43	5.38	5.06
Targeted MedRE (mm)	69.2	49.6	1.32	0.67	0.55	0.42	0.42	0.42	0.42	0.42	0.36	0.33
Stationary MedRE (mm)	1.08	1.21	1.17	1.09	1.09	1.08	1.08	1.08	1.08	1.09	1.09	1.09
Targeted 4mm SDR (%)	0.7	31.1	55.2	68.2	73.8	77.5	79.6	82.2	83.4	84.9	86.2	87.3
Stationary 4mm SDR (%)	95.9	94.4	92.9	93.5	93.3	93.3	93.9	92.8	93.2	93.3	94.1	93.8
$\epsilon$ -value (# of iterations=300)	-	-	-	0.5	1	2	4	8	16	32	-	-
Targeted MRE (mm)	-	-	-	71.1	65.0	43.3	22.7	12.3	9.0	7.9	-	-
Stationary MRE (mm)	-	-	-	1.72	1.86	3.10	6.86	5.31	5.73	5.72	-	-
Targeted MedRE (mm)	-	-	-	72.2	65.1	34.1	0.5	0.42	0.42	0.42	-	-
Stationary MedRE (mm)	-	-	-	1.05	1.08	1.08	1.09	1.08	1.09	1.08	-	-
Targeted 4mm SDR (%)	-	-	-	1.17	9.69	38.3	68.5	82.2	87.3	88.2	-	-
Stationary 4mm SDR (%)	-	-	-	95.4	95.1	94.3	93.1	92.8	92.9	92.1	-	-

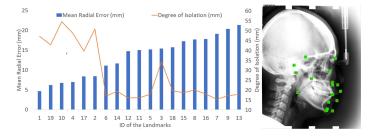


Fig. 5. Relationship between attack performance (measured by MRE) of each of 19 landmarks and its degree of isolation.

The effect of adaptiveness in ATI-FGSM. We compare the evaluation metrics and convergence speed of our method (green line) against Targeted I-FGSM (blue line) by generating 500 random adversarial examples with  $\epsilon=8$ . The MRE and 4mm SDR (at 300 iterations) of our method are 12.28mm and 82% while Targeted I-FGSM convergences to 21.84mm and 72%, respectively. Besides, our method compromises the network more quickly, results in a shorter attack time. The results in Fig. 4 show the advantages of our method lie in not only the attack effectiveness but also efficiency. Note that the attacker can not keep all of the stationary landmarks still, a few stationary landmarks are moved away by our method.

Attack performance vs degree of isolation. As some landmarks are closely related, such as landmarks on the chin or nose, which are adjacent in all images, we set up an experiment to investigate the relationship between MRE and the degree of isolation. We define the degree of isolation of a landmark as the average distance between its five nearest neighbors. As shown in Fig. 5, we observe that MRE and degree of isolation are negatively correlated. Therefore, moving a couple of adjacent landmarks to random positions is more difficult

than moving isolated ones. This is the major source of target deviation in our experiment, which may lead to potential defense.

A fancy attack. We draw 'MICCAI' on the same radiograph by attacking all of the 19 landmarks to the targeted position with  $\epsilon=8$  and 3000 iterations, which take 600s (per image) to compute on the GPU. As in Fig. 1, most landmarks are hacked successfully, which justifies that the CNN-based landmark detection is vulnerable to adversarial attacks.

## 5 Conclusion

We demonstrate vulnerability of CNN-based multiple landmark detection models when facing the adversarial-example attack. We show that the attacker can arbitrarily manipulate landmark predictions by adding imperceptible perturbations to the original image. Furthermore, we propose the adaptive targeted iterative FGSM, a novel algorithm to launch the adversarial attack more efficiently and effectively. At last, we investigate the relationship between vulnerability and coupling of landmarks, which can be helpful in future defense.

## References

- 1. Arik, S.Ö., Ibragimov, B., Xing, L.: Fully automated quantitative cephalometry using convolutional neural networks. Journal of Medical Imaging 4(1), 014501 (2017)
- 2. Bier, B., Unberath, M., Zaech, J.N., Fotouhi, J., Armand, M., Osgood, G., Navab, N., Maier, A.: X-ray-transform invariant anatomical landmark detection for pelvic trauma surgery. In: MICCAI. pp. 55–63. Springer (2018)
- 3. Chen, R., Ma, Y., Chen, N., Lee, D., Wang, W.: Cephalometric landmark detection by attentive feature pyramid fusion and regression-voting. In: MICCAI. pp. 873–881. Springer (2019)
- 4. Deng, J., Dong, W., Socher, R., Li, L.J., Li, K., Fei-Fei, L.: Imagenet: A large-scale hierarchical image database. In: CVPR. pp. 248–255 (2009)
- Gertych, A., Zhang, A., Sayre, J., Pospiech-Kurkowska, S., Huang, H.: Bone age assessment of children using a digital hand atlas. Computerized Medical Imaging and Graphics 31(4-5), 322–331 (2007)
- 6. Goodfellow, I., Shlens, J., Szegedy, C.: Explaining and harnessing adversarial examples. In: ICLR (2015)
- He, X., Yang, S., Li, G., Li, H., Chang, H., Yu, Y.: Non-local context encoder: Robust biomedical image segmentation against adversarial attacks. In: AAAI. vol. 33, pp. 8417–8424 (2019)
- 8. Ibragimov, B., Likar, B., Pernus, F., Vrtovec, T.: Computerized cephalometry by game theory with shape-and appearance-based landmark refinement (2015)
- Kurakin, A., Goodfellow, I., Bengio, S.: Adversarial machine learning at scale. ICLR (2017)
- 10. Li, H., Han, H., Li, Z., Wang, L., Wu, Z., Lu, J., Zhou, S.K.: High-resolution chest x-ray bone suppression using unpaired ct structural priors. IEEE Transactions on Medical Imaging (2020)
- 11. Lindner, C., Cootes, T.F.: Fully automatic cephalometric evaluation using random forest regression-voting. Scientific Reports 6, 33581 (2016)

- Litjens, G., Kooi, T., Bejnordi, B.E., Setio, A.A.A., Ciompi, F., Ghafoorian, M., Van Der Laak, J.A., Van Ginneken, B., Sánchez, C.I.: A survey on deep learning in medical image analysis. Medical Image Analysis 42, 60–88 (2017)
- 13. Liu, D., Zhou, S.K., Bernhardt, D., Comaniciu, D.: Search strategies for multiple landmark detection by submodular maximization. In: CVPR. pp. 2831–2838 (2010)
- Ozbulak, U., Van Messem, A., De Neve, W.: Impact of adversarial examples on deep learning models for biomedical image segmentation. In: MICCAI. pp. 300– 308. Springer (2019)
- 15. Paschali, M., Conjeti, S., Navarro, F., Navab, N.: Generalizability vs. robustness: Investigating medical imaging networks using adversarial examples. In: MICCAI. pp. 493–501. Springer (2018)
- 16. Payer, C., Štern, D., Bischof, H., Urschler, M.: Regressing heatmaps for multiple landmark localization using cnns. In: MICCAI. pp. 230–238. Springer (2016)
- 17. Ronneberger, O., Fischer, P., Brox, T.: U-net: Convolutional networks for biomedical image segmentation. In: MICCAI. pp. 234–241. Springer (2015)
- 18. Simonyan, K., Zisserman, A.: Very deep convolutional networks for large-scale image recognition. In: ICLR (2015)
- 19. Szegedy, C., Zaremba, W., Sutskever, I., Bruna, J., Erhan, D., Goodfellow, I., Fergus, R.: Intriguing properties of neural networks. In: ICLR (2014)
- Wang, C.W., Huang, C.T., Lee, J.H., Li, C.H., Chang, S.W., Siao, M.J., Lai, T.M., Ibragimov, B., Vrtovec, T., Ronneberger, O., et al.: A benchmark for comparison of dental radiography analysis algorithms. Medical Image Analysis 31, 63–76 (2016)
- Xie, C., Wang, J., Zhang, Z., Zhou, Y., Xie, L., Yuille, A.: Adversarial examples for semantic segmentation and object detection. In: CVPR. pp. 1369–1378 (2017)
- Yang, D., Xiong, T., Xu, D., Huang, Q., Liu, D., Zhou, S.K., Xu, Z., Park, J., Chen, M., Tran, T.D., et al.: Automatic vertebra labeling in large-scale 3d ct using deep image-to-image network with message passing and sparsity regularization. In: IPMI. pp. 633–644 (2017)
- 23. Yang, D., Zhang, S., Yan, Z., Tan, C., Li, K., Metaxas, D.: Automated anatomical landmark detection ondistal femur surface using convolutional neural network. In: ISBI. pp. 17–21 (2015)
- 24. Zheng, Y., Liu, D., Georgescu, B., Nguyen, H., Comaniciu, D.: 3d deep learning for efficient and robust landmark detection in volumetric data. In: MICCAI. pp. 565–572. Springer (2015)
- 25. Zhong, Z., Li, J., Zhang, Z., Jiao, Z., Gao, X.: An attention-guided deep regression model for landmark detection in cephalograms. In: MICCAI. pp. 540–548. Springer (2019)
- 26. Zhou, S.K. (ed.): Medical image recognition, segmentation and parsing: machine learning and multiple object approaches. Academic Press (2015)
- 27. Zhou, S.K., Greenspan, H., Shen, D. (eds.): Deep learning for medical image analysis. Academic Press (2017)