

Detection of Artificial Occlusal Caries in a Phosphor Imaging Plate System with Two Types of LCD Monitors Versus Three Different Films

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The aim of this study was to determine diagnostic performance of a storage phosphor plate system Digora® Optime (Soredex, Helsinki, Finland) with two types of LCD monitor in the detection of artificial caries when compared to Ultraspeed (D), Ektaspeed Plus (E), and Insight (F) radiographic films. Seventy extracted human molars—with artificial caries—were radiographed under identical standardized conditions using (1) a storage phosphor plate system Digora (Soredex, Helsinki, Finland), (2) Insight, (3) Ektaspeed Plus, and (4) Ultraspeed (Carestream Health Inc, Rochester, NY). All digital images and radiographs were examined by three observers for the presence or absence of artificial caries using a five-point confidence scale. Digital images were evaluated both on a LCD computer monitor (Philips 170S, Holland) and medical monitor—3 megapixel monochrome display (Me355i2, Totoku, Tokyo)—with brightness and contrast enhancement. Observer responses were evaluated using ROC analysis and other measurements for diagnostic accuracy. Storage phosphor images with medical monitor demonstrated higher mean A_z values (0.70 ± 0.08) than digital images with computer monitor and conventional films. Storage phosphor images with medical monitor presented the highest score, 0.97, 0.90, 0.94, for each observer, respectively. Also, true positive observations (0.82) and positive likelihood ratios (2.71) were higher in enhanced storage phosphor images with medical monitor. Caries detection of mechanically created lesions by experienced radiologists is roughly comparable when examining D-speed film images and Digora images on both the computer and medical LCD monitors, and appears to be poorer on E- and F-speed film images.

KEY WORDS: Diagnostic evaluation, digital display, digital imaging

INTRODUCTION

Conventional intraoral radiography is frequently preferred to detect caries. Since

faster films are desirable from the standpoint of exposure reduction, manufacturers are developing films with increased sensitivity to radiation.¹

Eastman Kodak's intraoral film, named Insight, builds on existing emulsion technology used for Ektaspeed Plus film, but has been classified as an E/F-speed film, depending on the processing conditions.² Previous studies indicated that the film in speed group F has contrast equal to or greater than Ektaspeed Plus, with an exposure dose reduction of at least 20%.³⁻⁵ Although an increase in speed implies dose reduction for the dental patient, D-speed film is the most preferred one among the dentists.^{3,6} Previous studies have been carried out about performance of F-speed film with respect to carious detection and depth measurement.⁷⁻¹⁴

Digital radiographic system was introduced as an alternative to conventional radiography. This system supplies approximately 80% exposure reduction compared to D-speed films.¹⁵⁻¹⁷ Digital images generated with storage phosphor techniques have been shown to be diagnostically comparable to film images for detecting caries.^{18,19} Easy access to image processing which may enhance the diagnostic value or facilitate the diagnostic interpretation is one of the advantages of digital radiography.²⁰⁻²⁵

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Several studies have shown that digital contrast enhancement increase diagnostic accuracy for detection of lesions.^{20,25–26}

More recently, liquid crystal display (LCD) monitors have been used as a display device for medical digital images, and LCD monitors are currently most common types used in diagnostic radiology systems.^{27–31} But to our knowledge, no comparison exists about the effects of LCD monitors on the observer's performance in dentistry. There are studies in the literature on the efficiency of various radiographic systems for the diagnosis of proximal caries which includes the surface of the tooth facing with the adjacent tooth, reporting a wide range of levels of diagnostic performance.^{12,13,32} However; there is no information available concerning artificial occlusal caries which includes only the masticator surface.

Thus, this study was carried out to obtain additional information on the diagnostic performance of a storage phosphor plate system Digora Optime[®] (Soredex, Helsinki, Finland) with two different LCD monitors in the detection of artificial occlusal caries when compared to Ultraspeed (D), Ektaspeed Plus (E) and Insight (F) radiographic films.

MATERIALS AND METHODS

Extracted Teeth and Simulation of Caries Lesions

Seventy extracted noncarious unrestored human molar teeth were used in this study. The teeth had been stored in a 10% formalin solution and the reason of their extraction was unknown. The experimental teeth were randomly divided in two groups. The study sample comprised 50 teeth; standardized occlusal cavities were prepared with 1.5 mm into dentin and 4 mm buccal–palatal and 6 mm mesio–distal diameters. A round bur, 0.7 mm in diameter, was used for preparing a hole on the pulpal surface of the occlusal cavity to simulate an artificial recurrent caries. The locations of the artificial holes on the base of the cavity were produced randomly. After filling the holes of each tooth in the study group with a modeling wax (Kemdent, Tenatex Red, UK), the occlusal restorations were made by using a hybrid composite resin (3M Espe Filtek Z 250, USA). The control group

consisted of 20 teeth with only occlusal composite restorations having the same dimensions as the study group. The experimental teeth of the study and control groups were randomly embedded in wax blocks as 35 pairs (each block consisting of two teeth) at the level of cemento–enamel junction (Fig. 1). Each block consisted of additional two teeth which represented neighbors at both ends (premolars, second, or third molars). These teeth were not included in the experiments.

Exposures

A Trophy (Novalix, Croissy-Beaubourg—France) intraoral X-ray unit, operating at 65 kV 8 mA with 2.5 mm aluminum equivalent filtration was used. Table 1 shows the characteristics of the film used and the two displays. To make X-ray projection geometry identical within each specimen, an arrangement was used (Fig. 2). A 15-mm thick polymethylmethacrylate plate was used to simulate soft tissue in the path of the beam at 220 mm from the focal spot. For the positioning, the place of the wax blocks were marked 5 mm from the film holding groove. The resulting focus-to-film distance was 255 mm. Ultraspeed, Ektaspeed Plus, and Insight dental films (Carestream Health Inc, Rochester, NY, USA) were used to image each set of teeth. Exposed films were automatically processed (Velopex Extra-X [Medivance Instrument Limited, London, UK]) using Kodak developer and fixer solutions. To determine the appropriate exposure times, one experimental block was exposed over a wide time range (0.10–1.0 s) with each film type.



Fig 1. Wax block.

Table 1. The Characteristics of the Films Used and the Two Displays

	Medical monitor	Computer monitor	Digora Optime	D-speed	E-speed	F-speed
lp/mm			12.5	20	20	20
Pixel Pitch mm	0.264	0.207				
Contrast ratio	900:1	800:1				
Available resolution	2,048 × 1,536	1,280 × 1,024				
Color	Grayscale	Color				
Maximum luminance cd/m ²	410	300				

An optical densitometer (Gretag Macbeth, TD 932, NY) was used to find the maximum optical density values. Exposure times, which produced a density of approximately 2.0 in background—as recommended by ISO 5799–1991—were selected for each film.^{3,3} The resulting exposure times for evaluated radiographs were 0.40, 0.30, 0.25, and 0.18 s for Ultraspeed, Ektaspeed Plus, Insight, and for Digora, respectively. The exposure times for Digora images were determined subjectively by blind consensus of the observers for optimal diagnostic quality. Consequently, radiographs of 35 blocks were taken with Digora and three types of films.

Evaluation of Radiographs and Digital Images

In the present study, 105 radiographs and 35 digital images were evaluated. The conventional radiographs were mounted on black cardboards with 35 size-adapted windows in randomized order. Three observers having 8, 7, and 5 years experiences as specialists in oral radiology, respectively, evaluated the radiographs in a darkened

quite room on a viewing box (50×75 cm) using a ×3 magnifier (Maped, China). Digital images were evaluated both on a LCD computer monitor (Philips, 170S, 1,280×1,024 resolution, Holland) and medical monitor—3 megapixel monochrome display (Me355i2, Totoku, Tokyo) using the toolbox in the same way for each (Digora[®] software for Windows 2.0[®], Soredex) in a darkened quite room, similar environment for evaluating the conventional radiographs. One viewing session was limited to 30 min. Care was taken to ensure that 24 h elapsed between each session. The observers were not informed about film types but they were free to use the brightness and contrast enhancement to be best in their view for digital images. All images and radiographs were assessed by the observers in terms of the visibility of artificial caries on the pulpal surface of the restoration. Visibility was classified on a five-point confidence scale: 1 = definitely no lesion present, 2 = probably no lesion present, 3 = uncertain whether or not a lesion is present, 4 = probably lesion present, 5 = definitely lesion present. The digital images and radiographs were evaluated by the observers for a second time after 1 week.

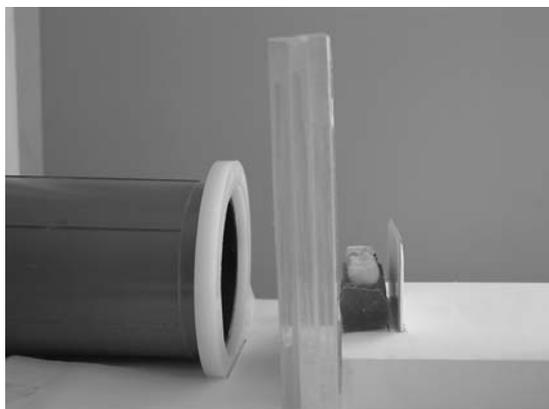


Fig 2. The arrangement for identical X-ray projection.

Statistical Analysis

Statistical analysis was performed using NCSS-PASS 2007 package program (Dr. Jerry L. Hintze & NCSS, Kaysville, UT) and ROCFIT computer program (Metz CE, Chicago, IL). Kappa test was used for detection observer reading and re-reading reliability. A rating of “3” (“uncertain whether or not a carious lesion is present”) was accepted as the missing value. Receiver operating characteristic (ROC) analysis was used to evaluate diagnostic accuracy for each radiograph and digital image. Kruskal–Wallis (KW) and Dunn’s multiple comparison tests were applied to mean A_z values. To

obtain information on a possible overlap, 95% confidence intervals (CI) of the areas beneath the curve (A_z) were included. After converting the confidence ratings into binary data (lesion/no lesion), true positive (TP), false positive (FP), true negative (TN), and false negative (FN) observations were calculated for radiographs and digital images pooled from all observers using all rating categories. Sensitivity (SNT) and specificity (SPF) were computed from these results. Positive likelihood (LR+) and negative likelihood (LR-) ratios were calculated. The LR+ is the ratio of the probability of obtaining a positive test result when the lesion is present to the probability of obtaining a positive test result when the lesion is absent.³⁴

RESULTS

In this study, 175 images with two teeth on each radiograph were evaluated. Table 2 shows that observers' readings and re-readings are consistent according to Kappa test ($p=0.0001$).

Table 3 presents intraclass coefficients and interobserver consistency for radiographs and digital images. These results reflect the reliability of observers with inter-ratings which explains that the observers gave similar ratings within the repeated observations for each image types. Enhanced storage phosphor images with medical monitor presented the highest score, 0.97, 0.90, 0.94, for each observer, respectively. For all film types, all observers gave similar ratings (mean=0.81).

On the other hand, a clear overlap existed between the 95% CIs of the areas of the radiographs and digital images (Table 4). In Table 3, the ROC curve area for the radiographs and digital images demonstrated that storage phosphor images with medical monitor had higher diagnostic accuracy than others. The mean A_z values were lower for E-speed film. The storage phosphor images

with computer monitor, Insight, and D-speed film produced similar A_z results.

Kruskal-Wallis (KW) test results revealed that the mean A_z values have a significant difference between the film types and digital images ($p=0.004$; Table 5).

Table 6 shows the comparison of mean A_z values for each film type and digital image. Only the differences between E- ($p<0.05$) and F-speed ($p<0.01$) films, according to the medical monitor, are statistically significant.

According to Table 7, sensitivity-specificity values and the positive likelihood ratio (LR+) were high for storage phosphor images with the medical monitor (0.65, 0.76, and 2.71, respectively). Ultraspeed was the second successful film type while finding artificial caries lesion according to positive likelihood ratio (LR+). Results for Insight and Ektaspeed Plus were similar. The negative likelihood ratio (LR-) was lowest (0.46) for storage phosphor images medical monitor and 0.65 for Ultraspeed.

DISCUSSION

In recent studies, conventional radiographic images were compared with the digital images and no differences were found in the measurement of the images and verified similar performance for the caries diagnosis.^{13,35-43} The performance of LCD monitor types is little known. The ME355i2 is a 3 megapixel 20.8" grayscale display and is widely used by radiologists due to its versatility for multi-modality workstations. This monitor includes luminance uniformity compensation for edge to edge uniformity and is capable of displaying 2,048 shades of gray, simultaneously. The display functions of the LCD medical monitor are much better than a computers'. While the contrast ratio is 900:1, the available resolution is 2,048 × 1,536 and maximum luminance is 410 cd/m² for

Table 2. Kappa Test Results

	Observer 1	Observer 2	Observer 3
Observer 1	$\kappa_w = 0.65$ $p = 0.0001$	$\kappa_w = 0.43$ $p = 0.0001$	$\kappa_w = 0.43$ $p = 0.0001$
Observer 2		$\kappa_w = 0.74$ $p = 0.0001$	$\kappa_w = 0.49$ $p = 0.0001$
Observer 3			$\kappa_w = 0.67$ $p = 0.0001$

Table 3. Intraclass Coefficiency and Interobserver Consistency

	All film types	D-speed	E-speed	F-speed	Digora® (Computer monitor)	Digora® (Medical monitor)
Observer 1	0.81 (0.76–0.85)	0.73 (0.57–0.83)	0.74 (0.58–0.84)	0.74 (0.58–0.84)	0.84 (0.794–0.891)	0.97 (0.95–0.98)
Observer 2	0.85 (0.81–0.88)	0.82 (0.71–0.90)	0.81 (0.70–0.88)	0.84 (0.75–0.90)	0.82 (0.732–0.882)	0.90 (0.84–0.90)
Observer 3	0.78 (0.72–0.83)	0.73 (0.57–0.83)	0.68 (0.56–0.79)	0.69 (0.57–0.80)	0.84 (0.798–0.873)	0.94 (0.90–0.96)
All observers	0.81 (0.79–0.84)	0.79 (0.68–0.86)	0.74 (0.61–0.83)	0.76 (0.65–0.84)	0.83 (0.795–0.867)	0.97 (0.95–0.98)

the medical monitor; these are 800:1, 1,280×1,024 and 300 cd/m² for the computer monitor.^{44,45}

Tyndall⁴⁶ et al. observed that when each observer used the brightness and contrast enhancement, it damaged the image when compared with conventional X-rays and digital image due to lack of skills for handling images. Wenzel⁴⁷ suggested that the distinction of the image used incorrectly could reduce the accuracy in the radiographic diagnosis.

In addition, there are studies which reported better results in the evaluation of the digital images with brightness and contrast enhancement.

In the present study, three observers having 8, 7, and 5 year's experiences as specialists in oral radiology, respectively, who have the skills for handling images, evaluated the digital images. It was observed that E- and F-speed films did not show significant differences comparing the quality for diagnosis.^{13,38,47,48} Similar to these results, E-speed and F-speed films revealed the same lower SPF when compared to other image types (0.49) in this study. According to these results, a question may be raised regarding the performance of Insight with respect to correct detection of carious lesions. Calculation of both SNT and SPF neglects the confidence of a given observer in his rating. Thus, it is more informative to look at the area under the ROC curve (A_z), which is a measure for accuracy of a diagnostic system. When comparing one ROC curve with another, however,

it is important to include information on the 95% CIs of A_z .³⁴ Our results reveal an obvious overlap of the 95% CIs among radiographs and digital images (Table 3), indicating that the test accuracies of all evaluated images are comparable. This is consistent with the study of Schulze.⁷

In Table 5, the mean A_z scores of E- and F-speed films are similarly lower than the others. Medical monitor has the highest score (mean A_z =0.70). The D-speed film and computer monitor have similar scores.

Positive (LR+) and negative (LR-) likelihood ratios were included to obtain information on the probability of the respective diagnostic system to obtain a positive or negative test result. The former is called the likelihood of a positive test result, whereas the latter is described as the probability of a negative test result. LR- was 0.46 for digital image with medical monitor. LR+ is also named the diagnostic power of a test.³⁴ In the present study, it ranged from 1.06 (Ektaspeed) to 2.71 (digital image with medical monitor). For D-speed film and digital image with medical monitor, both values (LR+, LR-) indicate a large overlap of ratings for the carious and noncarious teeth (Table 4). The results of storage phosphor images with medical monitor for artificial occlusal caries diagnosis may be due to its display properties.

Deeper lesions were easier to detect than relatively superficial ones.^{49,50} It is natural that

Table 4. Areas Between the 95% CIs

	Area	Asymptotic 95% Confidence Interval	
		Lower bound	Upper bound
D-speed film	0.62	0.53	0.71
E-speed film	0.57	0.48	0.66
F-speed film	0.61	0.52	0.69
Digital images			
(computer monitor)	0.65	0.56	0.72
Digital images			
(Medical monitor)	0.71	0.63	0.78

Table 5. Kruskal–Wallis (KW) Test

	Mean A_z
D	0.64 ± 0.06
E	0.5 ± 0.06
F	0.47 ± 0.05
DRC	0.65 ± 0.10
DR	0.70 ± 0.08
KW	17.43
P	0.004

Table 6. Dunn's Multiple Comparison Test

Dunn's multiple comparison test	$A_z(p)$
D/E	>0.05
D/F	>0.05
D/DR	>0.05
D/DRC	>0.05
E/F	>0.05
E/DR	<0.05
E/DRC	>0.05
F/DR	<0.01

cavity depth positively affected the odds of diagnosis; a radiographic image is a record of density difference, and the deeper the caries, the greater the caries–sound tooth ratio.⁵¹ Kang et al.⁵² demonstrated that mechanically created defects usually have higher contrast than natural carious cavities. Koistra¹² stated that radiographic diagnosis using an F-speed film significantly underestimated the true clinical extent of Class II carious lesions by 0.66–0.91 mm. In the present study, a round bur, 0.7 mm in diameter, was used to simulate an artificial caries.

According to Metz⁵³, an A_z value of approximately 0.75–0.80 can be regarded as reasonable for clinical imaging modalities. Borg⁵⁴ stated that the highest A_z values were found for the deeper lesion size, which gives a more tunnel-like appearance. Hence, corresponding to our generally low A_z values which may be due to small cavity size, the diagnostic power of E- and F-speed films was low in this investigation. This is perfectly in accordance with the statement of Schulze⁷, that the diagnostic power of conventional radiographs was low.

Kang et al.⁵¹ reported that the contrast-enhancing process seemed to make the borders of mechanical enamel defects even clearer when it was applied to Digora images. Mechanical defects

were more detectable than natural caries lesions on enhanced images. When attempts were made to discriminate between mechanical defects and natural dental caries, the former defects were easier to diagnose exactly on both enhanced and un-enhanced images. This is attributable to both the difference between mechanical defects and natural dental caries with respect to border characteristics and the contrast sensitivity of the human observer's eye.⁵⁵ In the present study, contrast- and brightness-enhancing processes were used for all digital images and the correct diagnosis of artificial caries with the medical monitor may be due to its high contrast ratio and resolution.

In conclusion, our results indicate that;

1. Caries detection of mechanically created lesions by experienced radiologists is roughly comparable when examining D-speed film images and Digora images on both the computer and medical LCD monitors, and appears to be poorer on E- and F-speed film images.
2. The positive likelihood ratio is very high for digital images viewed on the medical monitor.
3. Resolution, contrast ratio, and luminance are different between the two LCD monitors and the differences in diagnostic accuracy between the monitors may be related to some of these characteristics.
4. These findings may not be completely applicable to naturally occurring caries under restorations because of the different physical characteristics of bur-created lesions.
5. The large 95% confidence intervals suggest some variation in diagnostic ability of the examiners, but they are consistent in inter-items as indicated by the high kappa scores.

Decrease in patient exposure is a very important goal and alternative imaging modalities should prove their performances in order to be utilized

Table 7. Average Sensitivity, Average Specificity, Positive (LR+) and Negative (LR-) Likelihood Ratios

Film types	Sensitivity	Specificity	LR(+)	LR(-)
D-speed	0.63	0.57	1.47	0.65
E-speed	0.55	0.49	1.06	0.94
F-speed	0.57	0.49	1.11	0.88
Digital images with computer monitor	0.64	0.55	1.39	0.84
Digital images with medical monitor	0.65	0.76	2.71	0.46

routinely in daily practice. This study indicates one more time that usage of accurate equipments with digital imaging systems increases the diagnostic performance of the dentist.

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