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# Axonal transport rate decreased at the onset of optic neuritis in EAE mice

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# Abstract

Optic neuritis is frequently the first symptom of multiple sclerosis (MS), an inflammatory demyelinating neurodegenerative disease. Impaired axonal transport has been considered as an early event of neurodegenerative diseases. However, few studies have assessed the integrity of axonal transport in MS or its animal models. We hypothesize that axonal transport impairment occurs at the onset of optic neuritis in experimental autoimmune encephalomyelitis (EAE) mice. In this study, we employed manganese-enhanced MRI (MEMRI) to assess axonal transport in optic nerves in EAE mice at the onset of optic neuritis. Axonal transport was assessed as (a) optic nerve Mn<sup>2+</sup> accumulation rate (in % signal change/hour) by measuring the rate of increased total optic nerve signal enhancement, and (b)  $Mn^{2+}$  transport rate (in mm/hour) by measuring the rate of change in optic nerve length enhanced by Mn<sup>2+</sup>. Compared to sham-treated healthy mice, Mn<sup>2+</sup> accumulation rate was significantly decreased by 19% and 38% for EAE mice with moderate and severe optic neuritis, respectively. The axonal transport rate of  $Mn^{2+}$  was significantly decreased by 43% and 65% for EAE mice with moderate and severe optic neuritis, respectively. The degree of axonal transport deficit correlated with the extent of impaired visual function and diminished microtubule-associated tubulins, as well as the severity of inflammation, demyelination, and axonal injury at the onset of optic neuritis.

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# Introduction

Multiple sclerosis (MS) is a common inflammatory demyelinating disorder of the central nervous system (CNS) causing significant neurological dysfunction that accumulates over a lifetime (Compston and Coles, 2008; Trapp and Nave, 2008). Experimental autoimmune encephalomyelitis (EAE) is a widely used animal model of MS exhibiting many MS-like neurological dysfunctions including optic neuritis (ON) (Bettelli et al., 2003; Shao et al., 2004), which is often an early symptom of MS (Beck et al., 1993; Beck et al., 2003; Pascual et al., 2009; Shams and Plant, 2009). Inflammatory demyelination and axonal injury in the optic nerve that are commonly seen in MS patients are also frequently present in EAEaffected mice (EAE mice) (Diem et al., 2008; Gold et al., 2006; Sun et al., 2007). Accumulation of amyloid precursor protein (APP) is regarded as an early marker of axonal injury in MS patients and EAE mice (Bitsch et al., 2000; Fairless et al., 2012; Ferguson et al., 1997; Linker et al., 2010; MacKenzie-Graham et al., 2012; Petratos et al., 2012). Interruption of axonal transport in injured axons results in the accumulation of APP, which can be detected by immunohistochemistry (IHC) (Ferguson et al., 1997; Smith et al., 2003). Hence, axonal transport disruption could be an early event in EAE and in some patients with MS. However, few reports have assessed axonal transport in MS or its EAE models.

Manganese-enhanced MRI (MEMRI) has been applied in the rodent CNS (Bearer et al., 2007; Chan et al., 2011; Olsen et al., 2010; Pautler et al., 1998; Thuen et al., 2008) to investigate ion homeostasis and axonal transport. Manganese ion (Mn<sup>2+</sup>), as a calcium analogue, is taken up by neurons through voltage-gated  $Ca^{2+}$  channels. In the mouse visual system, Mn<sup>2+</sup> is taken up by retinal ganglion cells, packaged in vesicles, and transported along microtubules down the axonal tract (Pautler and Koretsky, 2002). As a paramagnetic ion.  $Mn^{2+}$  reduces tissue water T1 relaxation time and its presence in tissues can be identified as hyper-intensities in the T1W image (Silva et al., 2004). Recently, MEMRI has been applied to examine pathologies of the optic nerve, including blood-brain barrier integrity or inflammation, in EAE rats and mice (Boretius et al., 2008; Gadjanski et al., 2009; Guy, 2008). In this study, MEMRI was further extended as a dynamic tracer to investigate in vivo axonal transport integrity assessing axonal transport rates quantitatively. Our results support that axonal transport impairment is present at the onset of optic neuritis in EAE mice, and correlates with impaired visual function and the underlying optic nerve pathologies. To the best of our knowledge, this is the first quantification of axonal transport rate in optic nerve of EAE mice at the onset of optic neuritis. Our finding directly validated the previous axonal transport rate assessed by Mn<sup>2+</sup>-accumulation. We believe that the current report may provide a critical link between previous and future MEMRI assessed axonal transport rate in mice.

# **Materials and Methods**

All experimental procedures involving animals were approved by Washington University's Animal Studies Committee and conformed to the Public Health Service Policy on Humane Care and Use of Laboratory Animals (http://grants.nih.gov/grants/olaw/olaw.htm).

## Experimental autoimmune encephalomyelitis (EAE)

Sixteen 7-week old C57BL/6J mice were obtained from Jackson Laboratory (Bar Harbor, ME, USA). Ten mice were randomly selected to be immunized with 50 µg MOG<sub>35–55</sub> peptide emulsified (1:1) in incomplete Freund's adjuvant (IFA) and Mycobacterium tuberculosis. Pertussis toxin (300 ng; PTX, List Laboratories, Campbell, CA, USA) was injected intravenously on the day of  $MOG_{35–55}$  immunization and two days later. The remaining six sham mice underwent the same immunization procedure with only IFA without  $MOG_{35–55}$ . Mice were assessed daily for neurological disabilities using a standard clinical score (CS) system: 1 = limp tail; 2 = hind limb weakness sufficient to impair righting; 3 = one limb paralyzed; 4 = two limbs paralyzed; 5 = 3 or more limbs paralyzed or the animal is moribund (mice were euthanized if they reach grade 5).

## Visual acuity (VA)

The VA of mice was measured daily starting before immunization using the Virtual Optometry System (Optomotry, Cerebral Mechanics, Inc., Canada). Briefly, the virtual rotating columns were projected on the LCD monitors with different spatial frequencies in cycles/degree (c/d). The mouse head movement in response to the virtual column rotations was noted. The spatial frequency was increased starting from 0.1 c/d with step size of 0.05 c/d until the mouse stopped responding. The VA was defined as the highest spatial frequency of the virtual rotating columns to which the mouse was able to respond. We have previously reported that VA of normal C57BL/6 mice to be 0.38  $\pm$  0.03 c/d (mean  $\pm$  SD, n=30) and defined VA 0.25 c/d as the onset of acute ON for EAE mice (Chiang et al., 2012). MEMRI was performed on the day when mice exhibited VA 0.25 c/d. The mice in sham group did not develop impaired visual function and underwent the same MEMRI procedure at the same day as EAE group.

# Intravitreal MnCl<sub>2</sub> injection

MnCl<sub>2</sub> was injected in the eye that had a measured VA 0.25 c/d. Mice were anesthetized using 1.5-2% isoflurane/oxygen. After the appropriate level of anesthesia was achieved, assessed by the lack of response to toe pinch, mice were placed on a custom-made head holder. A 34-gauge needle, connected to a micro-injection pump (WPI Instrument, FL, US), was inserted into the posterior vitreous at 1–1.3 mm posterior to limbus. A dose of 50 nmol MnCl<sub>2</sub>, given as 0.25 µL of 0.2 M solution (Bearer et al., 2007), was delivered at a rate of 3 µL/min. At the conclusion of injection, the needle was left in the place for an extra 1 minute before withdrawal and then a drop of antibiotic gel was applied to both injected and uninjected eyes (Chen et al., 2012; Lin et al., 2014).

#### Manganese-enhanced MRI (MEMRI)

MEMRI was performed immediately after MnCl<sub>2</sub> administration on a 4.7 T Agilent DirectDrive small-animal MRI system (Agilent Technologies, Santa Clara, CA) equipped with Magnex/Agilent HD image gradient coil (Magnex, Oxford, UK) with pulse gradient strength up to 58 G/cm and a gradient rise time 295 µs. Mice were anesthetized by 1.5% isoflurane/oxygen. During experiments, respiratory rate and body temperature were monitored using a MR compatible animal monitoring system (SA Instrument, Inc., Stony

Brook, NY, US) and maintained at 130 - 150 breaths/min and  $37^{\circ}$ C with a regulated circulating warm water pad underneath mouse body along with regulated warm air blown into the magnet bore, respectively. A pair of 8-cm diameter volume (transmit) and 1.7-cm diameter surface (receive) active-decoupled coils were used.

A standard 3D gradient echo sequence was employed for T1-weighted (T1W) image of the whole mouse brain with the following parameters: repetition time (TR) = 15 ms, echo time (TE) = 2.63 ms, flip angle = 20°, number of averages = 16, field-of-view (FOV) =  $15 \times 15 \times 22 \text{ mm}^3$ , matrix size =  $128 \times 128 \times 64$  (zero-filled to  $256 \times 256 \times 128$ ), acquisition time = 32.8 minutes. Ten successive sets of 3D-T1W image were captured approximately from 0.55 – 5.5 hours post-injection.

#### **B1-inhomogeneity correction**

A 3D-T1W image of a phantom (uniform  $13 \times 9 \times 25 \text{ mm}^3$  of 2% agar gel placed underneath the active-decoupled surface coil with the distance between gel and coil similar to the *in vivo* study) was acquired using the same MEMRI parameters with 64 averages to obtain the profile of surface coil sensitivity (acquisition time was 131.2 minutes). To correct B1 inhomogeneity, the raw 3D-T1W image of the mouse brain was divided by the 3D-T1W image of 2% agar phantom voxel by voxel directly using image calculator in ImageJ (Schneider et al., 2012) and the corrected 3D-T1W image data set was generated for analyzing MEMRI data.

#### MEMRI data analysis

Surface-coil sensitivity profile corrected T1W image data set of the final time point was displayed using volume viewer plugin version 1.31 in ImageJ (http://rsbweb.nih.gov/ij/ plugins/volume-viewer.html, NIH, US) with z-aspect factor of 2 resulting in isotropic  $256 \times 256$  data matrix. The 3D data matrix was adjusted by rotating about x- and z-axis and distance slider to make oblique image plan bisecting both optic nerves. The oblique image containing both nerves was saved and converted to 8-bit gray scale. The corrected 3D-T1W image data sets of other previous time points were rotated using the same rotation parameters. The final result was a stack of oblique corrected T1W images (ten images) from each mouse (from 0.55 – 5.5 hours post-injection) for accumulation and transport rate calculation.

To derive the rate of total  $Mn^{2+}$  accumulation, ROI of optic nerves were drawn on the oblique corrected T1W image for each mouse. The average size of the optic nerve ROI was  $188 \pm 27$  voxels (n=160, mean  $\pm$  SD). A  $20 \times 20$ -voxel reference area ROI was drawn 30 voxels away from optic nerve head. This reference area ROI was pure muscle, not affected by intravitreal  $Mn^{2+}$  loading. The ROI information of optic nerves and reference area was saved and then applied to oblique corrected T1W images of other previous time points. Finally, the normalization was performed by taking the ratio of signal intensity of optic nerve ROIs and their respective reference ROI.

To calculate  $Mn^{2+}$  transport rate, a line ROI was drawn along the signal-enhanced and the contralateral optic nerves at the final time point, taking advantage of the increased contrast

for the ROI definition. The same line ROIs were applied to the corrected T1W images. The average size of  $Mn^{2+}$ -loaded and reference line ROI was  $54 \pm 3.3$  and  $53 \pm 3.2$  voxels (n = 160, mean  $\pm$  SD) respectively. The arrival of  $Mn^{2+}$  at the loaded nerve was defined by counting voxels with the signal intensity mean + 2 SD of the signal intensity of the contralateral optic nerve. After determining the number of voxels in the length of  $Mn^{2+}$ -enhanced optic nerves was converted to millimeter by combining the known in-plane image resolution, the geometric transformation associated with the oblique slice plane and the Pythagorean equation (Sally and Sally, 2007). Transport rate was defined as the slope of  $Mn^{2+}$ -enhanced length over time by linear fitting.

# Immunohistochemistry (IHC) of optic nerves

Following MEMRI experiments, mice underwent intra-cardiac perfusion with 1% phosphate buffered saline (PBS, pH = 7.4) followed by 4% paraformaldehyde in 0.01 M PBS. Brains were excised and post-fixed in the same fixative for 24 hours then transferred to 0.01 M PBS for storage at 4 °C until histological analysis was performed. Mouse optic nerves were dissected from each brain and embedded in 2% agar blocks (Blewitt et al., 1982). Then, the agar blocks were embedded in paraffin wax and 5-µm thick transverse slices were sectioned for IHC staining. Sectioned slices were deparaffinized, rehydrated, and blocked using solution mixed with 1% bovine serum albumin (BSA, Sigma-Aldrich, MO, USA) and 5% normal goat-serum solution (Invitrogen, CA, USA) for 20 minutes at room temperature to prevent non-specific binding and to increase antibody permeability. Slides were incubated with monoclonal antiphosphorylated neurofilament antibody (SMI-31; 1:1000, Covance, NJ, USA) to stain noninjured axons, or with rabbit anti-myelin basic protein antibody (MBP, 1:1000, Sigma-Aldrich, MO, USA) to stain myelin sheath (Budde et al., 2009; Song et al., 2003; Sun et al., 2007), or monoclonal microtubule-associated βIII tubulin (TUJ1, 1: 1500, Covance, IN, USA) to stain base structure of motor protein movement at 4°C overnight. After rinsing, goat anti-mouse IgG or goat anti-rabbit IgG conjugated Alexa 488 (1:800, Invitrogen, CA, USA) were applied to visualize immunoreactivity of phosphorylated neurofilaments and MBP. Finally, slides were covered using Vectashield Mounting Medium with 4',6-diamidino-2-phenylindole (DAPI) (Vector Laboratory, CA, USA) to stain nuclei (Budde et al., 2009; Wang et al., 2011). Histological slides were examined with Nikon Eclipse 80i fluorescence microscope equipped with a  $60 \times$  water objective, and images were captured with a black-and-white CCD camera using MetaMorph software (Universal Imaging Corporation, Sunnyvale, CA, USA) at the center of optic nerve.

#### Histological data analysis

The whole field of SMI-31, MBP, TUJ1, and DAPI staining images at 60× magnification were captured with the same fluorescence light intensity and exposure time. All captured images were converted to 8- bit gray scale and analyzed using threshold, analyze particles and gray level watershed segmentation functions in ImageJ (http://bigwww.epfl.ch/sage/ soft/watershed/).

#### Statistical analysis

Linear repeated measures models were used to test normalized  $Mn^{2+}$ -enhancement signal intensities at each time point (from 0.55 – 5.5 hours post-injection with 0.55-hour step size)

for pairwise comparison among shame and EAE mice with moderate and severe ON: sham vs. moderate, sham vs. severe, and moderate vs. severe groups.

Multiple comparisons for accumulation rate, transport rate, TUJ1, SMI-31, MBP, and DAPI by each study group (sham/moderate/severe) were performed using a linear regression model of each outcome. P-values for the three pairwise tests (sham vs. moderate, sham vs. severe, and moderate vs. severe) were adjusted using Tukey's HSD (honest significant difference). The correlation coefficients for accumulation or transport rate with each TUJ1, SMI-31, MBP, and DAPI or for accumulation rate with transport rate were analyzed by Spearman's rank correlation coefficient, which includes one observation per mouse (independent assumption was met).

# Results

# Visual acuity

After immunization, daily visual acuity (VA) of sham and EAE mice was measured. When mice exhibited VA 0.25 c/d (Chiang et al., 2012), MEMRI was performed ( $12 \pm 2.1 \text{ days}$  post-immunization, mean  $\pm$  SD, n=10). In this study, CS appeared in some EAE mice at the same day as the first sign of impaired VA. VA at ON onset was different among mice examined and was used to separate mice into three groups: sham (VA = 0.35 or 0.4 c/d; CS = 0), moderate ON (VA = 0.2, CS = 1 for one mouse; VA = 0.25 c/d, CS = 0 for the rest four mice), and severe ON (VA = 0 c/d, CS = 0 for two mice and CS = 2.5 for the rest 3 in this group; Fig. 1A).

# The optic nerve Mn<sup>2+</sup> accumulation rate

Since the image intensity was used to detect  $Mn^{2+}$  arrival, the B1-inhomogeneity correction of the surface coil was performed (Lin et al., 2003, Hou, 2006) using the 3D T1W image of 2% agar gel (Fig. 2). After correction, the averaged intensity of randomly selected line profiles on the corrected T1W images was comparable in both vertical and horizontal directions suggesting a reasonable B1-field inhomogeneity correction (Fig. 2D and 2E).

A series of time-lapse representative B1-profile corrected oblique T1W images of sham, moderate and severe ON mice exhibited different degrees of  $Mn^{2+}$ -enhancement suggesting different axonal transport rates in optic nerves. The hyper-intensity of optic nerve resulting from axonal transport of  $Mn^{2+}$  was readily visible (Fig. 1B). The optic-nerve and reference ROI were defined (Fig. 3A). The time course of group averaged signal intensity ratios of optic-nerve to reference ROI exhibited different rate of signal enhancement among the sham and EAE mice with moderate and severe ON (Fig. 3B). The accumulation rate of  $Mn^{2+}$  in the optic nerve was defined as the slope of the linear fit of the data over time. The group averaged optic nerve  $Mn^{2+}$  accumulation rate (the slopes) of sham, moderate ON, and severe ON mice was 0.16, 0.13, and 0.10 a.u./hour, respectively (Table 1; Fig. 3C). The accumulation rate in EAE mice was significantly slower than that of the sham by 19% (moderate ON, p < 0.005), and 38% (severe ON, p < 0.005). The accumulation rate was 23% (p < 0.05) slower in the EAE mice with severe ON than that with the moderate ON. The accumulation rate correlated with VA (r = 0.87, p < 0.0001, data not shown).

# Transport rate of Mn<sup>2+</sup>

The Mn<sup>2+</sup>-loaded and contralateral optic nerve reference line ROIs were defined (Fig. 4A). The enhanced T1W intensity of the optic nerve after Mn<sup>2+</sup> loading was readily discernible after the subtraction of mean line ROI intensity of the reference optic nerve (Fig. 4B - 4D). Representative difference images of sham and EAE mice with moderate ON exhibited different length of the Mn<sup>2+</sup>-enhanced optic nerve. The entire optic nerve was enhanced at 3.3 and 5.5 hours post-injection for sham (Fig. 4B) and EAE mice with moderate ON (Fig. 4C), respectively. In EAE mice with severe ON, only partially enhanced optic nerve was seen (Fig. 4D). The time course suggested that the group-averaged time to enhance the entire optic nerve took 3.3 and 4.95 hours for sham and EAE mice with moderate ON, respectively (Fig. 4E). The slope of each group represents the transport rate (% of optic nerve/hour). The group averaged Mn<sup>2+</sup> transport rate of sham, moderate ON, and severe ON mice was 26, 14, and 8 % of optic nerve/hour (Fig. 4E). The Mn<sup>2+</sup> transport rate converted to mm/hour was: 0.92, 0.52, and 0.32 mm/hour for the sham, moderate ON, and severe ON mice, respectively (Table 1). The transport rate of EAE mice was decreased compared with sham mice by 43% (p < 0.05) and 65% (p < 0.005) respectively for moderate and severe ON groups. EAE mice with moderate ON exhibited a nonsignificant trend of faster transport rate than severe ON mice (p = 0.15). The transport rate correlated well with the VA (r = 0.85, p <0.0001, data not shown).

## Immunohistochemistry (IHC) of optic nerve

Post-image TUJ1, SMI-31, MBP, and DAPI staining of optic nerves from sham and EAE mice with moderate and severe ON was used to assess the integrity of microtubules, axons myelin sheaths, and the extent of cellularity (Fig. 5A). Increased number of DAPI positive nuclei in EAE optic nerves was observed (Fig. 5A). The positive TUJ1 stains significantly decreased in optic nerves from the severe EAE mice  $(4.2 \pm 1.3 \times 10^5, p = 0.006, Fig. 5B)$ , insignificantly decreased in moderate EAE ( $4.9 \pm 1.4 \times 10^5$ , p = 0.059, Fig. 5B), when comparing to the sham group  $(6.5 \pm 0.7 \times 10^5)$ . The SMI-31 positive axon counting showed a significantly diminished intact axon density in optic nerves from EAE mice with moderate  $(5.6 \pm 0.5 \times 10^5, p < 0.005, Fig. 5B)$  and severe  $(4.5 \pm 0.9 \times 10^5, p < 0.005, Fig. 5B)$  ON. The significant loss of MBP positive axons expressed as area fraction in optic nerves with moderate (41.6  $\pm$  2.0 %, p < 0.05, Fig. 5B) and severe (34.0  $\pm$  3.4 %, p < 0.005, Fig. 5 B) ON was also observed compared with the sham group ( $48.3 \pm 3.9$  %). DAPI positive cell nuclear staining was significantly increased in optic nerves from mice with severe ON (9.1  $\pm$  $3.3 \times 10^3$ ) when compared with the sham ( $3.9 \pm 0.6 \times 10^3$ , p < 0.005, Fig. 5B) and moderate ON (5.4  $\pm$  1.0  $\times$  10<sup>3</sup>, p < 0.05, Fig. 5 B) mice. However, the difference between sham (3.9  $\pm$  $0.6 \times 10^3$ ) and mice with moderate ON ( $5.4 \pm 1.0 \times 10^3$ , p = 0.1, 5B) was not significant. The  $Mn^{2+}$  accumulation rate correlated well with  $Mn^{2+}$  transport rate (r = 0.78, p = 0.0003, Fig. 6A). The Mn<sup>2+</sup> accumulation and transport rate correlated well with the extent of TUJ1positive microtubule-associated tubulin integrity (r =0.68 and r = 0.76, respectively,  $p < 10^{-10}$ 0.005), intact axonal density (r = 0.85 and r = 0.86, respectively, p < 0.0001) assessed by the density of SMI-31 positive axons, myelin injury (r = 0.91 and r = 0.82, respectively, p < 0.820.0001) assessed by the MBP positive axons, and inflammation (r = -0.83 and r = -0.84, respectively) assessed by the density of DAPI-positive nuclear staining (Fig. 6A - 6I).

# Discussion

In this study, we assessed VA by optokinetic response (Fig. 1A) and quantified axonal transport in optic nerves using MEMRI in EAE mice at the onset of ON (Fig. 1B). The rate of Mn<sup>2+</sup> transport in EAE-affected optic nerves was significantly impaired (Figs. 1, Fig. 3 and 4) indicating defective fast axonal transport at the onset of ON (Millecamps and Julien, 2013). Immunohistochemistry of these tissues also indicated the presence of microtubule impairment, demyelination, inflammation, and axonal injury in optic nerves with ON (Fig. 5B). Each of these axonal pathologies correlated well with decreased axonal transport rate.

The rate of axonal Mn<sup>2+</sup> accumulation has been reported to reflect axonal transport in mice (Massaad et al., 2010; Sharma et al., 2010; Smith et al., 2007; Wang et al., 2012). In the literature, a linear fit of the MEMRI data over a short time course (< 1 hour) was commonly employed. In this study, a 5.5-hour time course was pursued. A linear repeated measures model accounting for the correlation between observations over time applied to the serial 10 measurements suggested that a linear fit was reasonable (data not shown). Thus, a more complex modeling (Cross et al., 2008; Olsen et al., 2010) was not pursued in this study to analyze the MEMRI time course data. In addition to this widely employed Mn<sup>2+</sup> accumulation rate, the current study also assessed axonal transport rate in optic nerves at the onset of ON caused by EAE. The reported fast axonal transport rate ranges between 3 - 16mm/hour (De Vos et al., 2008; Millecamps and Julien, 2013). The Mn<sup>2+</sup> transport rate by MEMRI has been reported ranging between 0.64 - 5 mm/hour, estimated by a two-point time-lapse measurement (Bearer et al., 2007; Chan et al., 2008; Leergaard et al., 2003; Pautler et al., 1998; Saleem et al., 2002; Van der Linden et al., 2002; Watanabe et al., 2004). In the present study, the Mn<sup>2+</sup> transport rate in sham optic nerves was  $0.92 \pm 0.14$  mm/hour, at the lower end of published values. Animals in the current study were under isoflurane anesthesia throughout the course of the measurements. The lower axonal transport rate estimated herein may result from the long period of anesthesia (Jevtovic-Todorovic et al., 2013; Kameyama et al., 1999). The transport rate estimated using data from the initial 0.55 hours, i.e., less severely affected by anesthesia, was 1.33, 1.49, and 1.31 mm/hour in sham, moderate and severe ON groups, respectively. The higher initial rate supported the possible effect of prolonged anesthesia on the measured transport rate. The varied rate of transport using the initial time-lapse data immediately after injection may reflect the variable severity of ON among mice, or the variable response of individual mice to the induction of anesthesia, masking the transport rate difference among groups. The linear increase over time of MEMRI length of the optic nerve between 0.55 - 5.5 hours from all groups suggested that a steady-state of anesthesia was reached 0.55 hours after the injection of  $Mn^{2+}$ .

The axonal  $Mn^{2+}$  transport rate between moderate and severe ON groups was not statistically different (Fig. 3F). This may be due to the variation in axonal pathologies of the severe ON group, leading to a high variance in that group. It may also be due to imprecision of the method of VA measurement (Ridder and Nusinowitz, 2006). Optic nerves from three EAE mice with severe ON were not fully enhanced at the end of 5.5 hours post-injection (Fig. 3 E) while the rest two exhibited whole optic nerve enhancement at 4.4 and 4.95 hours. These two mice also exhibited axonal injury (25% decrease in SMI-31 staining compared

with the control) comparable to that in the moderate ON mice  $(22 \pm 7\%)$ . IHC results indicated that the mice with higher transport rates suffered less axon and myelin damage than those with slower transport rates. It is possible that acute vasogenic edema at the ON onset impeded action potential propagation and thus reduced VA without significant axonal pathologies (Guy, 2008; Hickman et al., 2004). It is also worth noting that VA was employed herein to serve as a "clinical" sign of optic neuritis in EAE mice because the conventional clinical score reflecting spinal cord injury does not correspond to visual functions. The mechanistic correlation between VA and the axonal transport remains to be elucidated. One obvious link would be that the impaired axonal transport causes axonal injury leading to visual function impairment (which may or may not be directly reflected by VA).

Intravitreal injection of  $MnCl_2$  is a common practice for MEMRI studies. The toxicity of intravitreal injection of  $MnCl_2$  in mice and rats has been investigated previously (Bearer et al., 2007; Haenold et al., 2012; Luo et al., 2012; Thuen et al., 2008). In a preliminary study (Lin et al., 2014), we have concluded that intravitreal injection (0.25  $\mu$ L of 0.2 M MnCl<sub>2</sub>) slightly affected visual acuity with full recovery a day later without causing axonal injury or loss in C57BL/6 mice. Thus, the observed axonal transport deficit in EAE mice optic nerves is not likely an artifact resulting from MnCl<sub>2</sub> injection.

Why might axonal transport be affected in early inflammatory demyelination? Axonal transport depends on energy supplied by mitochondria (Ohno et al., 2011). In MS and its animal model EAE, several pathologies conspire to reduce energy supply. Nitric oxide and the free radical/reactive oxygen species are increased, including within axons, and inhibit mitochondrial function (Smith and Lassmann, 2002) reducing energy production. Sodium channel redistribution in demyelinated axons reduces internode length, thereby increasing the energy consumption needed for signal propagation (Dutta et al., 2006; Kornek et al., 2001; Waxman, 2006). The potential energy deficit would eventually lead to failure of the Na<sup>+</sup>/K<sup>+</sup>-ATPase pump (which requires energy for maintenance) and increased intracellular Na<sup>+</sup>, thus triggering the reversal of Na<sup>+</sup>/Ca<sup>2+</sup> exchanger. The resultant influx and accumulation of intracellular Ca<sup>2+</sup> may then lead to further mitochondrial dysfunction and axonal damage (Andrews et al., 2005; Craner et al., 2005; Mao and Reddy, 2010; Stys, 2005; Su et al., 2009). Excessive glutamate production by inflammatory cells, coupled with reduced buffering capacity of glial cells leads to glutamate-induced excitotoxicity of axons (which express glutamate receptors) (Mark et al., 2001; Pitt et al., 2000; Stys, 2005; Su et al., 2009; Trapp and Nave, 2008), results in inhibition of mitochondrial mobility and function (Macaskill et al., 2009; Rintoul et al., 2003). Therefore, a vicious cycle of disruption of ion homeostasis, energy deficits, and axonal transport deficits could play a crucial role in axonal degeneration (De Vos et al., 2008; Hollenbeck and Saxton, 2005; Mao and Reddy, 2010; Millecamps and Julien, 2013).

In this study, positive TUJ1 staining was applied (Fig. 5) to reflect  $\beta$ III tubulin, associated with fast axonal transport of molecules and organelles (Jouhilahti et al., 2008; Niwa et al., 2013). Our data showed that accumulation and transport rates correlated well with TUJ1 staining results (Fig. 6B and C), supporting that MEMRI is appropriate for investigating axonal transport integrity in optic nerves. Although the current data are not sufficient to

determine whether the impaired axonal transport is the result or the cause of axonal injury at the onset of ON (Fig. 6D – 6I), its association with various axonal pathologies was apparent. Excess nitric oxide and reactive oxygen species are produced during neuroinflammation. These species have been shown to decrease axonal transport *in vitro* (Fang et al., 2012; Stagi et al., 2005). In other studies, excessive nitric oxide was shown to reversibly block impulse conduction in demyelinated CNS axons of rodents (Redford et al., 1997) while reduction in nitric oxide at the inflammation site prevented further axonal degeneration (Smith et al., 2001). Demyelination was also reported to result in axonal transport disruption in EAE mice (O'Neill et al., 1998; Rodriguez, 2003). Phosphorylated neurofilaments play a role in regulating axonal transport (Roy et al., 2000; Shea et al., 2003). Our current findings that decreased axonal transport correlated with reduced SMI-31 and MBP, and increased DAPI staining are consistent with these literature reports.

In summary, this study demonstrated the presence of impaired optic nerve axonal transport in the early stages of ON in EAE mice. The decreased axonal transport rate correlated with impaired visual function, diminished tubulins, and axonal pathologies including axonal injury, demyelination, and inflammation.

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# Highlights

• Optic nerve axonal transport rate was quantified using MEMRI

- Axonal transport rate significantly decreased at the onset of optic neuritis
- Decreased axonal transport rates correlated with axonal pathologies
- Decreased axonal transport rate correlated with visual acuity



#### Figure 1.

Group averaged visual acuity (VA) of sham (n=6) and EAE (n=10) eyes before MEMRI experiments. EAE mice were grouped based on VA to moderate (VA = 0.25/0.20 c/d) and severe (VA = 0 c/d) ON groups (A). A serial time-lapse oblique corrected T1W images from representative mice are presented to demonstrate the different degree of  $Mn^{2+}$ -enhancement of optic nerves from sham and EAE mice from 1.1 – 5.5 hours post-injection (B).  $Mn^{2+}$ -enhancement of optic nerves clearly increases with time. At the end time point, mice with the lower VA exhibited less  $Mn^{2+}$ -enhancement reflecting slower axonal transport.

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#### Figure 2.

A T1W image of 2% agar gel was used to compensate the B1-inhomogeneity effect in the raw data set generating the corrected T1W images. Three representative images are raw T1W image of mouse brain (A), T1W image of 2% agar gel (B), and the corresponding corrected T1W image (C), which was generated from raw T1W image of mouse brain (A) divided by T1W image of 2% agar gel (B) voxel by voxel. Three vertical (solid lines, A and C) and three horizontal (round dots, A and C) profiles were randomly drawn in each of five mouse-brain images of raw and corrected T1W, respectively. The group averaged raw profile showed linear decrease from top to bottom in vertical orientation (D). Even though there is no obviously variation with the profile from left to right in horizontal profiles were stable (D and E) and suggested that B1 inhomogeneity was compensated successfully.

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#### Figure 3.

The ROI of optic nerve and reference area of muscle, where  $Mn^{2+}$  does not reach, were defined on the corrected T1W oblique image at each time point (A). The group average of the normalized optic nerve signal intensity from sham, moderate ON and severe ON mice was obtained for each time point from 0.55 - 5.5 hours after injection at a 0.55 hours resolution. The higher rate of  $Mn^{2+}$  accumulation over time was associated with the better VA (B). The group averaged slope of the normalized signal intensity over time was defined as the optic nerve accumulation rate of total  $Mn^{2+}$ . The box plots reveal that  $Mn^{2+}$  accumulation rate of severe ON optic nerves was slower than that of the moderate ON nerves, which was slower than that of the same nerves (B and C). \* indicates p < 0.05

\*\* indicates p < 0.005



## Figure 4.

To estimate Mn<sup>2+</sup> transport rate in mm/hour, line-ROIs were defined to match the optic nerve length (A). The arrival of  $Mn^{2+}$  in optic nerves was defined by the T1W enhancement of the optic nerves referencing to the line-ROI of the non-loaded eye. To visualize the extent of Mn<sup>2+</sup>-enhancement, representative oblique-corrected T1W images from each group were displayed after subtracting the mean intensity of the reference line-ROI (B, C, and D). Three representative subtracted images of sham, moderate ON and severe ON mice (VA = 0.4, 0.25, and 0, respectively) show different degree of  $Mn^{2+}$  transport at 1.1, 3.3, and 5.5 hours post-injection (B, C, and D). For quantification of the transport rate, the arrival of Mn<sup>2+</sup> was determined using **non-subtracted** images at each time point by identifying line-ROI voxels of the loaded eye with intensity higher than two standard deviation of the mean from the reference line-ROI of the non-loaded eye. The group averaged displacements, normalized to the total number of voxels of each nerve (red line, panel E), of  $Mn^{2+}$  over time revealed different rate of Mn<sup>2+</sup> transport among the three groups of mice examined (E). Box plot shows transport rate distribution of each group in mm/hour by converting normalized voxel displacement to mm (F). The results demonstrated that Mn<sup>2+</sup> transport rate of sham optic nerves were significantly faster than moderated ON (p < 0.005) and severe ON (p < 0.005) suggesting the presence of axonal transport impairment at the onset of ON in EAE mice. \* indicates p < 0.05

\*\* indicates p < 0.005

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#### Figure 5.

Representative immunohistochemical staining of optic nerves from sham, moderate ON and severe ON mice (A). Images displayed are 56% field-of-view from the  $60 \times$  magnification of mictrotubule-associated  $\beta$ III-tubulin (TUJ1, green), phosphorylated neurofilament (SMI-31, green), myelin basic protein (MBP, red), and 4', 6-dianidino-2-phenylindole (DAPI, blue). Reduced density of TUJ1 (microtubulins) and SMI-31 (phosphorylated neurofilaments) positive axons were seen in optic nerve from moderate and severe ON mice. Areas of increased TUJ1 and SMI-31 positive patches were observed with increased severity of VA, probably reflecting axonal beading or debris (A, yellow arrows). Decreased density of MBP positive axons and increased DAPI positive nuclear staining was also seen with increased VA impairment. Box plots demonstrate the difference in axonal pathologies among the three groups examined (B).

Scale Bar: 25  $\mu$ m \*p < 0.05 \*\*p < 0.005

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Figure 6.

# Table 1

Group averaged accumulation and transport rates of sham (n=6), moderate ON (n=5) and severe ON (n=5)

	Sham (n=6)	Moderate ON (n=5)	Moderate ON (n=5)
Accumulation Rate	$0.16\pm0.01$	$0.13\pm0.01$	$0.10\pm0.02$
Transport Rate	$0.92\pm0.14$	$0.52\pm0.17$	$0.32\pm0.21$

Accumulation Rate (a.u./hour): mean  $\pm$  S.D.

Transport Rate (mm/hour): mean  $\pm$  S.D.