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1 **Highlights**

- 2 • We model hydroxyapatite particle mixing within a gelatin solution in a stirred tank
- 3 • The stirred tank geometry and configuration allow to obtain homogeneous suspensions
- 4 • Discrete or continuous graded bone scaffolds can be obtained from these suspensions
- 5 • Results help to design small stirred tanks for automated bone scaffold fabrication

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1 **CFD modelling of a mixing chamber for the realisation of**
2 **functionally graded scaffolds**

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1 **Abstract**

2 Biological tissues are characterised by spatially distributed gradients, intricately linked with
3 functions. It widely accepted that ideal tissue engineered scaffolds should exhibit similar
4 functional gradients to promote successful tissue regeneration. Focusing on bone, in previous
5 work we proposed simple methods to obtain osteochondral functionally graded scaffolds (FGSs),
6 starting from homogeneous suspensions of hydroxyapatite (HA) particles in gelatin solutions.
7 With the main aim of developing an automated device to fabricate FGSs, this work is focused on
8 designing a stirred tank to obtain homogeneous HA-gelatin suspensions. The HA particles
9 transport within the gelatin solution was investigated through computational fluid dynamics
10 (CFD) modelling. First, the steady-state flow field was solved for the continuous phase only.
11 Then, it was used as a starting point for solving the multi-phase transient simulation. CFD results
12 showed that the proposed tank geometry and setup allow for obtaining a homogeneous
13 suspension of HA micro-particles within the gelatin solution.

14

15 **Keywords:** Computational fluid dynamics; stirred tank; particle suspension; functionally graded
16 scaffolds; tissue engineering

17

18 **1. Introduction**

19 Biologically inspired approaches have been widely accepted in designing better implants as well
20 as in manufacturing artificial tissues. In general, tissues are characterised by hierarchical
21 structures with spatially distributed gradients of properties and composition, that are intimately
22 linked with functions (Miyamoto, Kayser, Rabin, Kawasaki, & Ford, 1999). For instance, bone

1 tissue, with its stiff external region (i.e. cortical bone) gradually changing to a porous spongy
2 honeycombed internal one (i.e. cancellous bone), demonstrates how the functional gradation has
3 been used in biological adaptation to optimise the material response to external loadings. The
4 current consensus is that an ideal tissue-engineered scaffold should recapitulate most of the
5 native tissue characteristics to provide cells with an optimal micro-environment promoting cell
6 growth and differentiation. Therefore, functionally graded scaffolds (FGSs) are critical for the
7 successful engineering of biological tissues. A variety of manufacturing methods for the
8 fabrication of FGSs have been proposed, including multiple tape casting (Werner, Linner-
9 Krčmar, Friess, & Greil, 2002), injection molding (Zhang, Chang, Lu, Lin, & Ning, 2007),
10 multiple and differentiated impregnations (A Tampieri, Celotti, Sprio, Delcogliano, & Franzese,
11 2001), modified sponge replication (Hsu, Turner, & Miles, 2007) and freeze-casting (Macchetta,
12 Turner, & Bowen, 2009). However, the development of new manufacturing methods that can
13 tightly control the gradient of properties in a cost-effective way is still a challenge (Miao & Sun,
14 2009). Focusing on bone tissue, which is mainly composed by hydroxyapatite (HA) and collagen
15 (Col), we have recently investigated simple methods to obtain osteochondral FGSs with either
16 discrete or continuous gradient profiles. In particular, discrete FGSs were prepared by stacking
17 homogeneous HA-gelatin (HA/Gel) suspensions with different HA/Gel weight ratios (Jelen et
18 al., 2013), while continuous FGSs were obtained using the gravitational sedimentation of HA
19 particles that occurs during the controlled cross-linking of homogeneous HA/Gel suspensions
20 (Mattei, Tirella, & Ahluwalia, 2012). These methods are very suited for developing an
21 automated device to realise either discrete or continuous FGSs for tissue engineering
22 applications. Mechanical agitation is widely used in industrial processes involving solid-liquid

1 flows, with the typical requirement of suspending the solid phase for dissolution, enhanced
2 reaction, or to obtain uniform suspensions, as in our case. Among the various approaches to
3 provide mechanical agitation (e.g. sonication, vortexing, stirring, etc.) we chose to suspend
4 particles through mixing in a small stirred tank. Understanding the fluid dynamics in the stirred
5 tank is critical to properly design a mixing chamber that ensures a homogeneous suspension of
6 HA micro-particles (secondary solid discrete phase) within the gelatin solution (primary liquid
7 phase) prior to be transferred into a mold. Multi-phase computational fluid dynamics (CFD)
8 modelling significantly helps in designing the stirred tank, limiting the expensive and time-
9 consuming *trial-and-error* experimental approach. CFD modelling has become a powerful tool
10 for the prediction of flow fields and mixing in stirred tanks, being very helpful for estimating
11 important process parameters such as the homogenisation time (t_H , i.e. the time required to
12 achieve a fully-mixed state) and the requested power input. Several approaches to modelling
13 solids transport were proposed, including both Lagrangian and Eulerian techniques. The Eulerian
14 multiphase model is of particular interest, since it uses separate sets of Navier-Stokes equations
15 for the liquid and the solids (or granular) phases, coupling the interactions between them. Using
16 Eulerian-Eulerian models, Micale et al. predicted particle distribution at low particle
17 concentrations in single and multiple impeller stirred vessels (Micale, Montante, Grisafi,
18 Brucato, & Godfrey, 2000). Even though their results were in good agreement with experimental
19 axial measurements of solids concentration, they used correction factors to fit the numerical
20 predictions to experimental data, concluding that improved single-phase simulations and
21 incorporation of the so-called four-way interactions (i.e. fluid-particle, particle-fluid, particle-
22 particle and particle-turbulence) would enhance model applicability and reliability. The Eulerian

1 Granular Multiphase (EGM) model accounts for the four-way coupling between and within
2 phases, providing a fully predictive solution of the solids transport in the stirred tank. The
3 strongly coupled momentum equations of granular and liquid phases require a transient solution
4 (Massah & Oshinowo, 2000).

5 In this paper, multiphase CFD modelling is used to study the distribution of HA micro-particles
6 in a gelatin solution at 40 °C (modelled as water) within a stirred tank. In particular, the transient
7 start-up of a purposely designed mixing tank driven by a 4 blade radial paddle (RP4) is
8 presented, considering the HA secondary phase initially located at the bottom of the tank, at a
9 given homogenous concentration. The rest of the domain is composed of HA-free gelatin
10 solution. This case is of particular interest for the realisation of discrete FGS by stacking
11 different homogeneous HA/Gel layers, as we proposed. In fact, the FGS fabrication can be
12 automated by designing a device which integrates and controls a small stirred tank with an
13 actuated bottom that can be opened and closed to transfer the HA/Gel suspension to an
14 underlying mold. In particular, first a homogeneous HA-rich suspension is prepared in the stirred
15 tank and partially transferred into the mold, realising the subchondral bony layer of the
16 osteochondral FGS. Then, the remaining HA/Gel mixture in the stirred tank is sequentially
17 diluted with a HA-free gelatin solution, obtaining less HA-rich suspensions for intermediate FGS
18 layers. The latter are sequentially cast into the mold towards a HA-free region, resembling the
19 cartilaginous layer. The stirred tank should be properly designed to guarantee a homogeneous
20 particle suspension after each dilution. The pre-processor MixSim 2.0 (Fluent Inc., USA) was
21 used to create the computational grid with multiple reference frames (MRF), while numerical
22 calculations in the agitated vessel were solved using ANSYS FLUENT (Ansys Inc., USA).

1 Computations were performed assuming a standard k - ε model of turbulence and modelling the
2 multiphase flow using the EGM. First the steady-state flow field was solved for the continuous
3 phase only (i.e. gelatin solution), and then used as a starting point for the multi-phase transient
4 simulation. Steady-state flow field in the stirred tank and time-varying concentrations of HA
5 particles obtained from the numerical simulations will be presented and discussed.

6

7 **2. Material and methods**

8 **2.1. Experimental problem description**

9 According to the experimental protocols showed in (Jelen et al., 2013; Mattei et al., 2012), a
10 mixing chamber with a volume of about 2 mL was designed and modelled to prepare the
11 homogeneous HA/Gel suspension to realise discrete or continuous FGS. The stirred tank has a
12 flat bottom and an inner diameter of $T = 14$ mm (Fig. 1). The liquid level is $T = H = 14$ mm. The
13 off-bottom clearance is $C = T/4 = 3.5$ mm. The custom made centric shaft has a diameter of 2
14 mm and ends with an integrated 4 blade radial paddle impeller (RP4). The latter moves in
15 clockwise direction at a constant rotational speed $N = 240$ rpm, chosen on the basis of
16 experimental tests previously performed in our laboratory with a similar setup. The RP4 impeller
17 has a diameter of $D = 9$ mm $\sim 0.64 T$, in agreement to the typical dimensions reported in the
18 literature, i.e. 0.5 - $0.8 T$ (Inglezakis & Poulopoulos, 2006). Blades are $B = 3$ mm in height and 1
19 mm in thickness. The 2 mm cylindrical core at the centre of the impeller (Fig. 1b) guarantees a
20 geometrical continuity with the shaft, enhancing the overall mechanical stability of the rotating

1 elements and improving the fluid dynamics at the blades crossing point, avoiding any zone of
2 stagnation, with respect to sharp perpendicular angles.

3 According to the geometry described, the resultant volume of liquid within the stirred tank was
4 2.0742 mL. Since we used the multiple reference frame (MRF) approach for CFD calculations
5 (section 4), this volume was divided in two domains: a rotating zone around the impeller (*radial*
6 *paddle*) and an external region (*continuum*) with no assigned motion. Considering the sequential
7 dilution approach to obtain discrete FGSs previously described, we studied the transient mixing
8 between a HA-rich gelatin suspension initially located in the *radial paddle* region only and a
9 HA-free gelatin solution located in the rest of the stirred-tank liquid volume (i.e. *continuum*
10 zone). The primary liquid phase was represented by a 5% w/v gelatin solution at 40°C, here
11 modelled as water (density, 1 g/cm³; viscosity, 1 cP). The volume fraction of HA micro-particles
12 (density, 3.157 g/cm³; average diameter, 10 µm) in the *radial paddle* region was set to 0.037,
13 resembling the remaining portion of a 70/30 HA/Gel suspension, previously prepared for the
14 bony layer of the osteochondral FGS (Mattei et al., 2012; Anna Tampieri et al., 2008).

15

16 **2.2. CFD calculations**

17 The software package from Fluent Inc. was used for the CFD simulations. In particular, MixSim
18 2.0, a specialised pre-processor for mixing applications, was used for defining the mixing tank
19 configuration and for generating the computational grid. The model was then solved using
20 ANSYS FLUENT.

21 **2.2.1. Multiphase flow model**

1 The multiphase model for CFD calculations is commonly selected using two parameters: i) the
 2 average inter-particle space (L/d_p) and ii) the Stokes number (St). The former can be estimated
 3 according to Crowe et al. (Crowe, Sommerfeld, & Tsuji, 1998). In the *worst* case of higher HA
 4 volume fraction (i.e. $\alpha_{HA} = 0.037$), a value of $L/d_p = 2.42$ is obtained, where d_p represents the
 5 HA particle diameter equal to 10 μm . The Stokes number is defined as the ratio between the
 6 particulate relaxation time and the system response time, $St = \tau_s/t_{sys}$, where $\tau_s = \frac{\rho_s d_p^2}{18\mu_f}$ and t_{sys}
 7 is based on the characteristic length (L_{sys}) and the characteristic velocity (V_{sys}) of the system
 8 under investigation: $t_{sys} = L_{sys}/V_{sys}$. Considering $L_{sys} = T = 14$ mm (i.e. tank diameter) and V_{sys}
 9 $= 2\pi \cdot (N/60) \cdot (D/2) = 0.113$ m/s (i.e. the velocity at the extremity of a radial paddle blade, equal to
 10 the maximum velocity in the stirred vessel) we obtain $St = 1.41 \cdot 10^{-4}$. In case of low particulate
 11 loading (i.e. $L/d_p > 1$) and very low Stokes number ($St \ll 1$) the coupling between the phases is
 12 one-way, i.e. the fluid carrier influences the particles via drag and turbulence, but the particles
 13 have no influence on the fluid carrier.

14 However, in this work we chose the Eulerian modelling approach, the most rigorous among the
 15 multiphase models, to model multiple separate, yet interacting phases. It is based on a multi-fluid
 16 approach and treats the multiple phases as interpenetrating continuums: a single pressure is
 17 shared by all phases, while a separate set of continuity and momentum equations is solved for

1 each phase. The interaction between phases is modelled through the momentum exchange terms
 2 and includes the drag exerted by the continuous phase on the dispersed phase. Solid-phase
 3 stresses in the Eulerian granular multiphase (EGM) model are derived making an analogy
 4 between the random particle motion (arising from particle-particle collisions) and the thermal
 5 motion of molecules in a gas (Dimitri Gidaspow, 1994). Therefore, a stress tensor based on the
 6 kinetic theory for granular flow is included in the granular momentum equation. The kinetic
 7 energy associated with the particle velocity fluctuations is represented by a “pseudo-thermal” or
 8 granular temperature, which is proportional to the mean square of the random motion of
 9 particles, hence an additional transport equation for granular temperature (or solids fluctuating
 10 energy) is modelled.

11 **2.2.2. EGM model: fundamental equations**

12 Fundamental equations used to solve the EGM model are presented below in their general form,
 13 where q refers to the analysed phase, while p represents one of the n phases of the model.

14 Symbols used are listed in the Nomenclature section at the end of the manuscript.

15 The mass conservation or continuity equation for a phase q is:

$$16 \quad \frac{\partial}{\partial t}(\alpha_q \rho_q) + \nabla \cdot (\alpha_q \rho_q \vec{v}_q) = \sum_{p=1}^n (\dot{m}_{pq} - \dot{m}_{qp}) + S_q \quad (1)$$

17 Since no mass transfer occurs in our system and as no species sources are present, both mass
 18 transfer terms (\dot{m}_{pq} and \dot{m}_{qp}) and source term S_q are null within the presented mixing model.

19 The momentum balance for a phase q can be expressed as:

$$\begin{aligned}
& \frac{\partial}{\partial t} (\alpha_q \rho_q \vec{v}_q) + \nabla \cdot (\alpha_q \rho_q \vec{v}_q \vec{v}_q) = -\alpha_q \nabla p + \nabla \cdot \bar{\bar{\tau}}_q + \alpha_q \rho_q \vec{g} + \\
& \sum_{p=1}^n (\vec{R}_{pq} + \dot{m}_{pq} \vec{v}_{pq} - \dot{m}_{qp} \vec{v}_{qp}) + (\vec{F}_q + \vec{F}_{lift,q} + \vec{F}_{vm,q})
\end{aligned} \tag{2}$$

where \vec{v}_{pq} is the interphase velocity related to the mass transfer term \dot{m}_{pq} , hence null, and $\bar{\bar{\tau}}_q$ represents the q^{th} phase stress-strain tensor expressed below (Eq. 3).

$$\bar{\bar{\tau}}_q = \alpha_q \mu_q (\nabla \vec{v}_q + \nabla \vec{v}_q^T) + \alpha_q (\lambda_q - \frac{2}{3} \mu_q) \nabla \cdot \vec{v}_q \bar{\bar{I}} \tag{3}$$

The lift force ($\vec{F}_{lift,q}$) acts on a particle mainly due to velocity gradients in the primary-phase flow field. Since it is generally more relevant for larger particles and rather insignificant compared to the drag force, $\vec{F}_{lift,q}$ is neglected in the computational model. The *virtual mass effect* (VME) occurs when a secondary phase p accelerates relative to the primary fluid phase q , as the inertia of the primary-phase mass encountered by accelerating particles exerts a *virtual mass force* on the particles, represented by $\vec{F}_{vm,q}$ in Eq. 2. The VME effect is not considered in the model, since it is significant only when the secondary phase density is much smaller than that of the primary phase.

EGM model equations must be closed with appropriate expressions for the interphase force (\vec{R}_{pq} in Eq. 2), depending on friction, pressure, cohesion, and other effects, and subjected to the conditions that $\vec{R}_{pq} = -\vec{R}_{qp}$ and $\vec{R}_{qq} = 0$. ANSYS FLUENT models this force using a simple interaction (Eq. 4), where K_{pq} ($=K_{qp}$) represents the interphase momentum exchange coefficient.

$$1 \quad \sum_{p=1}^n \vec{R}_{pq} = \sum_{p=1}^n K_{pq} (\vec{v}_p - \vec{v}_q) \quad (4)$$

2 Generally, the momentum exchange between phases in granular flows depends on fluid-fluid,
 3 fluid-solid and solid-solid exchange coefficients respectively termed K_{ll} , K_{sl} and K_{ls} . Since the
 4 modelled system consists only of a primary liquid phase (gelatin solution) and a secondary
 5 granular phase (HA particles), the fluid-fluid exchange coefficient can be neglected. The
 6 Gidaspow model (D. Gidaspow, Bezburuah, & Ding, 1992) is chosen for the fluid-solid
 7 exchange coefficient, while the solid-solid exchange coefficient between particles is modelled
 8 according to Syamlal et al. (Syamlal, 1987).

9 The granular-phase momentum equation contains a solid pressure term composed of a kinetic
 10 term and a second term due to particle collisions. The Lun et al. formulation (default settings in
 11 ANSYS FLUENT) is chosen to compute solids pressure. The probability of collisions between
 12 particles changes when the solid granular phase becomes dense. This phenomenon is modelled
 13 through a correction factor called radial distribution function. Since our mixing problem involves
 14 only a single solid phase, the latter is represented according to Lun et al. (Ogawa, Umemura, &
 15 Oshima, 1980).

16 The maximum volume fraction of randomly packed solid objects ($\alpha_{s,\max}$) is defined using the
 17 packing limit, an important empirical parameter with no precise geometric definition:
 18 theoretically, it depends on the number and the diameter of particles dispersed within a given
 19 volume. In case of mono-dispersed spherical particles, random close packing cannot exceed a

1 density limit of 0.634 (Song, Wang, & Makse, 2008). In our model, this theoretical (default)
2 value is considered for the packing limit.

3 Shear and bulk viscosities arising from particles momentum exchange (due to translation and
4 collision) are contained in the solid stress tensor. The solid shear viscosity is the sum of
5 collisional, kinetic and frictional components. The granular viscosity model of Syamlal and
6 O'Brien is adopted for the collisional and kinetic parts (Syamlal, Rogers, & O'Brien, 1993),
7 while the frictional component is neglected in the numerical model, since it accounts for the
8 generation of frictional stresses between particles, which is relevant only for dense flow at low
9 shear. The resistance of the granular particles to compression and expansion is accounted in the
10 solids bulk viscosity term, here modelled according to Lun et al. (Lun, Savage, Jeffrey, &
11 Chepurniy, 1984).

12 The granular temperature is solved using an algebraic formulation (default settings in ANSYS
13 FLUENT), thus neglecting convection and diffusion in the transport equation. Surface tension
14 between fluid and granular solid phase is not considered in the model. Turbulence in the liquid
15 phase is modelled using the standard k - ϵ model, while turbulence generation by the secondary
16 granular phase is neglected.

17

18 **2.3. Numerical procedure and solution strategy**

19 The pre-processor MixSim 2.0 (Fluent Inc., USA) is used to create the computational grid with
20 multiple reference frames (MRF), defining the geometry of the vessel, type of the impeller,
21 geometry and density of the numerical grid and part of the boundary conditions. An unstructured

1 3D computational grid mainly composed of tetrahedral cells is generated. The assignment of grid
2 density can be specified in different parts of the vessel, setting the initial mesh size or the size of
3 a grid cell on the basis of the impeller, shaft, baffles and other components used in the tank.
4 Initial mesh sizes are kept at default software values. The impeller motion is modelled using the
5 multiple reference frame (MRF) approach. The vessel is divided in two parts, a moving frame
6 around the impeller (*radial paddle*) and a stationary frame (*continuum*) attached to the vessel
7 wall. The dimensions of the rotating fluid zone for MRF are evaluated on the basis of the
8 impeller geometry using default expressions provided by MixSim 2.0. The computational grid
9 obtained is shown in Fig. 2: it has 75053 cells, characterised by an average *skewness* of 0.34,
10 thus being an excellent grid for 3D flow problems (Sun, 2007).

11 Governing equations were solved numerically using ANSYS FLUENT. No slip boundary
12 conditions are applied on all tank walls and shaft with the latter moving at the prescribed
13 rotational velocity of $N = 240$ rpm. The free surface of the suspension is characterised by zero
14 gradients of velocity and all other variables. Since the shear stress is null, it can be interpreted as
15 a zero-shear slip wall, hence it is modelled with symmetry boundary conditions. The impeller
16 motion at $N = 240$ rpm is modelled using the MRF approach. Materials properties are set as
17 outlined in Section 2 and gravity is fixed at 9.81 m/s^2 . After obtaining the continuous liquid
18 phase flow field, HA particles are patched only in the *radial paddle* region, at a volume fraction
19 of 0.037, as discussed in Section 2. Then the time-dependent HA-gelatin mixing problem is
20 solved using the EGM model. The starting time-step is 0.005 s, then it is increased to 0.01 s after
21 solving the first second of the transient. CFD calculations are performed until a steady-state
22 solution is obtained, i.e. after the homogenisation time, t_H , determined using the coefficient of

1 variation (CoV) of the HA volume fraction within the stirred tank (Coroneo, Montante, Paglianti,
2 & Magelli, 2011). The $CoV(t)$ is defined as the ratio of the standard deviation of HA volume
3 fraction at time t to its final equilibrium value (equal to 0.0115 for the modelled problem). The
4 homogenisation time (t_H) is taken as the instant at which the CoV becomes stable in time and
5 below 0.05, according to many published works using the t_{95} , i.e. the mixing time after which the
6 concentration of a species has reached and remains within a 5% range of the final equilibrium
7 value (Moštěk, Kukukova, Jahoda, & Macho\v{n}, 2005; Ochieng, Onyango, & Kiriamiti, n.d.).

8

9 **3. Results and discussion**

10 The flow field within the stirred tank generated by the RP4 impeller rotation at $N = 240$ rpm is
11 shown in Fig. 3. Velocity profiles at the axial cross-sections of the vessel passing in the middle
12 of the RP4 blades ($\theta = 0^\circ$) and through the blades ($\theta = 45^\circ$) are shown in Fig. 3a and 3b,
13 respectively. When the flow impacts on the tank wall, it splits up into two parts and changes the
14 direction. Then, the split flow returns to impeller region and accelerated again. Repeating this
15 process, two circulation loops of different directions were generated in the upper and lower part
16 of the tank, respectively. Vector plots clearly highlight these loops, which are indispensable for
17 suspending HA particles within the stirred tank. Radial velocity profiles for two sections parallel
18 to the tank bottom, located at 3.5 mm and 10.5 mm above it, are presented in Fig. 3c. The fluid
19 flow is highest near the impeller, reaching its maximum velocity at the tip of the RP4 blades
20 (equal to $2\pi \cdot (N/60) \cdot (D/2) = 0.113$ m/s), while it becomes relatively low near the free surface.

1 The distribution of HA volume fraction versus time while stirring is shown in Fig. 4 using
2 contour plots at the same axial cross-sections chosen for the velocity field, i.e. $\theta = 0^\circ$ and $\theta =$
3 45° . Moreover, the axial distributions of the dimensionless HA volume fraction over time
4 (defined as $\alpha_{HA}(z, t)/\alpha_{HA,eq}$, with $\alpha_{HA,eq} = 0.0115$) evaluated for the dimensionless radial
5 coordinate $r^* = r/R = 0.5$ ($R = T/2 = 7$ mm) belonging to the $\theta = 0^\circ$ axial cross-section plane are
6 shown in Fig. 5. At time 0, the HA was homogeneously suspended in the *radial paddle* region
7 only, at the prescribed volume fraction of 0.037. Then, the two circulation loops generated by the
8 RP4 impeller agitation, draw the gelatin primary phase down to the HA-rich lower region of the
9 vessel. To compensate this, HA particles start to rise up, mixing in an ever-increasing volume of
10 HA-free gelatin solution with time. As a result, the maximum volume fraction of HA decreases
11 with time while stirring, until an almost homogenous HA distribution is reached within the
12 vessel after the homogenisation time t_H .

13 To estimate the homogenisation time, the coefficient of variation (CoV) of the HA volume
14 fraction is calculated considering values computed for the whole stirred tank volume, thus being
15 a better indicator of the suspension homogeneity with respect to considering a point, a line or a
16 surface only. The CoV versus mixing time is shown in Fig. 6.

17 According to the adopted definition, the homogenisation time can be taken as $t_H = 50$ s, in
18 correspondence to which the CoV value is equal to 0.02, demonstrating that HA particles are
19 almost homogeneously suspended within the stirred tank. Suspension quality (or homogeneity)
20 can be evaluated as $1 - \text{CoV}$, with 1 representing a theoretically perfect homogeneous
21 suspension (i.e. particle volume fraction independent of the position within the vessel). The

1 suspension homogeneity for the modelled problem is 0.98, obtained after 50 s of mixing, and did
2 not change by increasing the mixing time, thus confirming that a stable steady state is reached
3 after the t_H , as expected.

4

5 **4. Conclusions**

6 The mixing of HA micro-particles within a gelatin solution in a custom stirred tank has been
7 investigated through CFD modelling, with the main aim of designing the latter to obtain
8 homogenous HA-gelatin suspensions for fabricating either discrete or continuous osteochondral
9 FGSs. The tank geometry and experimental configuration as well as multi-phase CFD model
10 setup have been described in detail throughout the manuscript. First, only the continuous fluid
11 phase (i.e. gelatin solution) has been considered in the CFD model for solving the steady-state
12 flow field. Then, the initial distribution of HA particles has been defined and the HA-gelatin
13 mixing investigated by solving a time-dependent multi-phase CFD model. Computational results
14 showed that a homogeneous HA-gelatin suspension was obtained after 50 s mixing at a rotational
15 speed of 240 rpm.

16 In general, this modelling framework can be used to simulate every mixing problem between
17 suspensions with different homogeneous initial particle concentrations. For the sake of easiness
18 in setting-up the CFD model, only two suspensions have been considered in the present work,
19 patching the initial particle distribution in one of the two region requested for solving the single-
20 phase fluid flow within the stirred tank. However, more complex models can be implemented by
21 defining the requested number of domains (> 2 , in general) for both setting-up the stirring fluid-

1 dynamic problem and patching the initial particle distribution, while generating the stirred tank
 2 computational grid.

3

4 **Nomenclature**

5 Symbols are listed in order of appearance within equations shown in the paper.

6 α_q q^{th} phase volume fraction

7 ρ_q q^{th} phase density

8 \bar{v}_q q^{th} phase velocity

9 \dot{m}_{pq} mass transfer from phase p to phase q

10 S_q q^{th} phase source term

11 p pressure (shared by all phases)

12 $\bar{\bar{\tau}}_q$ q^{th} phase stress-strain tensor

13 \bar{g} acceleration due to gravity

14 \bar{R}_{pq} interphase force

15 \bar{v}_{pq} interphase velocity

16 \bar{F}_q external body force

17 $\bar{F}_{lift,q}$ lift force

- 1 $\vec{F}_{vm,q}$ virtual mass force
- 2 μ_q q^{th} phase shear viscosity
- 3 λ_q q^{th} phase bulk viscosity
- 4 K_{pq} interphase momentum exchange coefficient
- 5 \vec{I} identity tensor
- 6 d_s s^{th} solid phase particle diameter

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2 **Figure Legends**

3 **Fig. 1** The experimental geometry: a) stirred tank setup and dimensions; b) detail of the impeller
4 design showing its cylindrical core (arrow).

5 **Fig. 2** a) 3D rendering of the stirred tank; b) 2D view of the computational grid for a 2D axial
6 plane passing through the RP4 impeller blades; c) 3D view of the computational grid generated
7 for the rotating impeller zone (i.e. *radial paddle*), shown in grey.

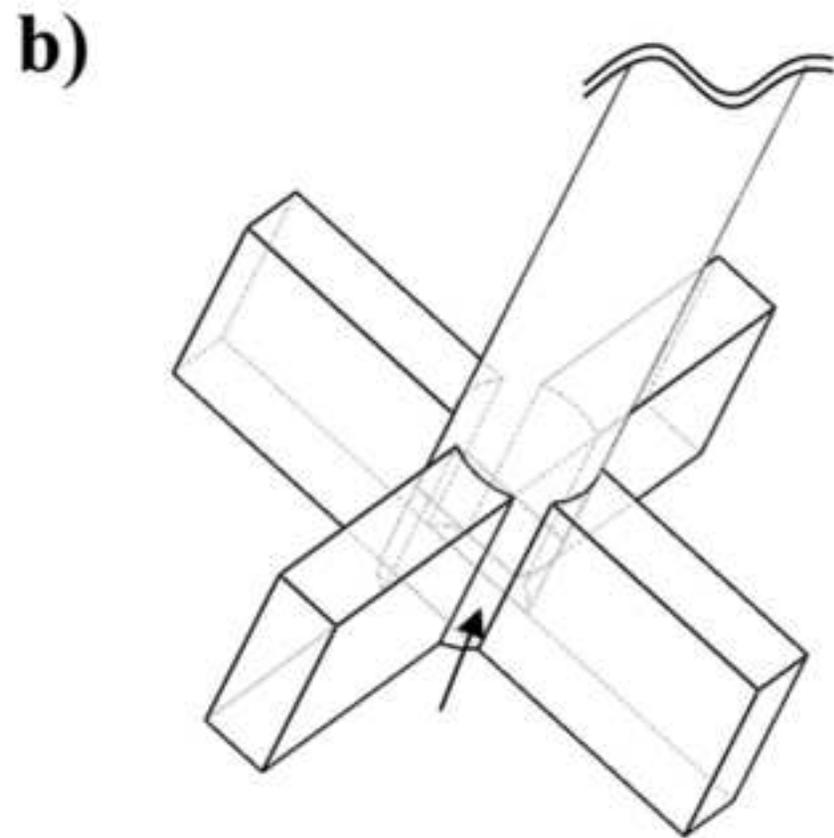
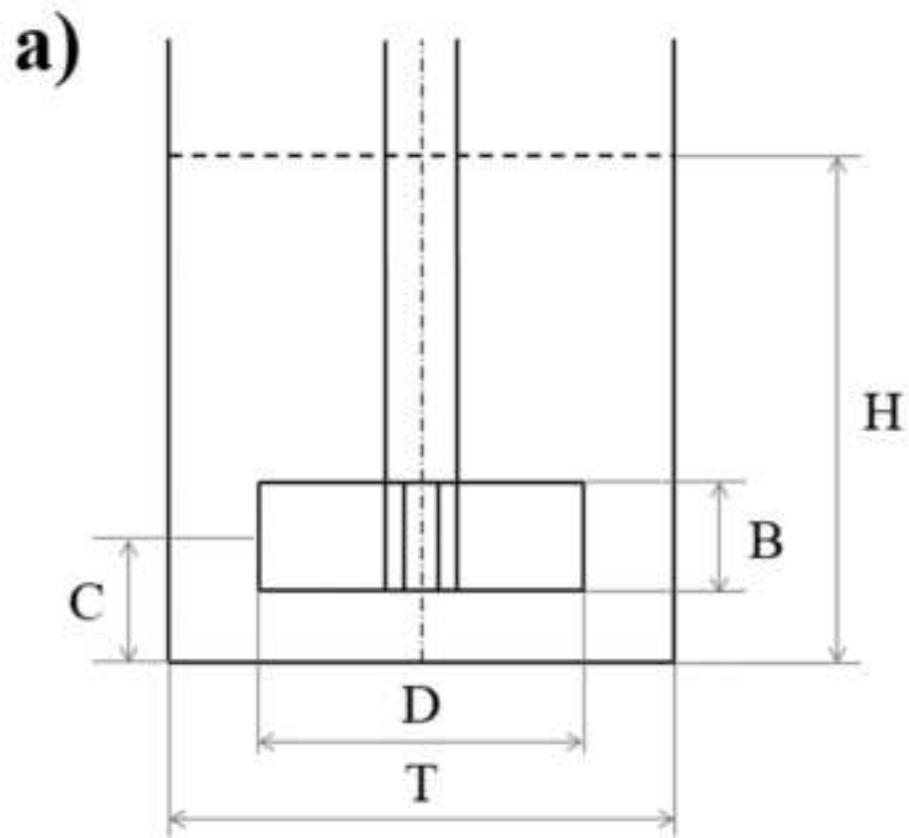
8 **Fig. 3** Flow field within the stirred tank at 240 rpm. Distributions of the fluid velocity vectors at
9 the axial cross-section of the vessel passing a) in the middle of the RP4 blades and b) through the
10 blades. c) Radial velocity profiles for two sections parallel to the tank bottom, located at 3.5 mm
11 and 10.5 mm above it.

12 **Fig. 4** CFD modelled HA volume fraction distribution in time while stirring. Contour plots in the
13 first line are referred to the $\theta = 0^\circ$ axial cross-section, while those in the second line are referred
14 to the $\theta = 45^\circ$ one.

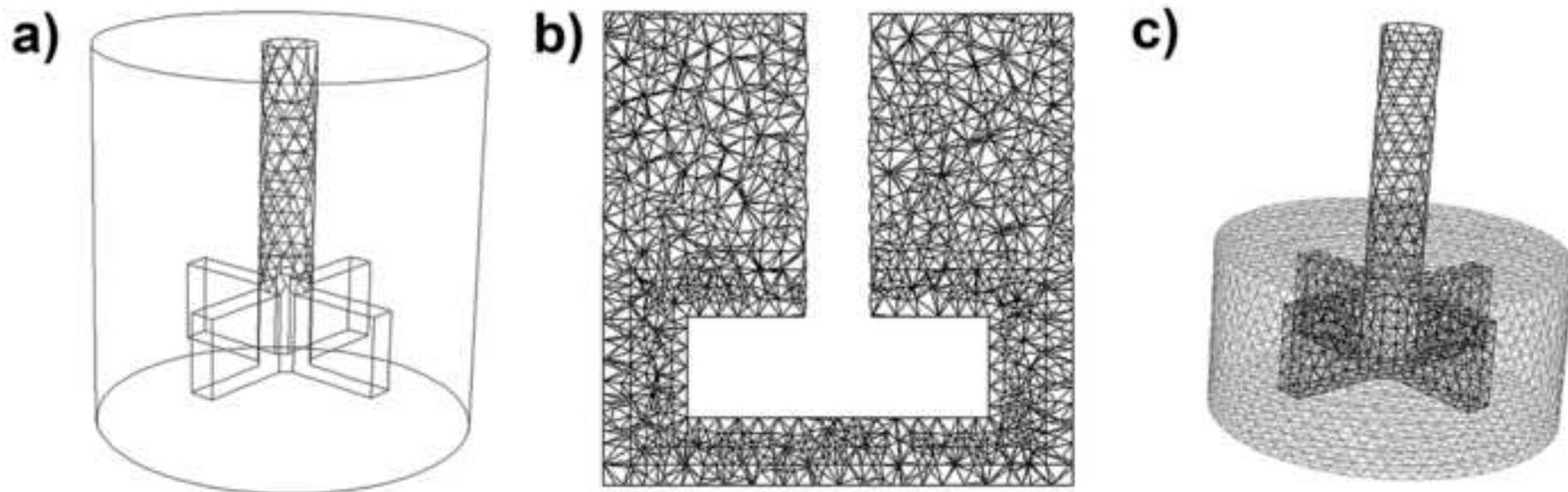
15 **Fig. 5** Axial distribution of the dimensionless HA volume fraction in time (α/α_{eq}) evaluated for
16 the dimensionless radial coordinate $r^* = 0.5$ belonging to the $\theta = 0^\circ$ axial cross-section. In figure,
17 z/H represents the dimensionless axial coordinate, with $H = 14$ mm.

18 **Fig. 6** Coefficient of variation of the HA volume fraction calculated for the whole stirred tank
19 volume. A stable plateau value of 0.02 is reached after 50 s of mixing, corresponding to the
20 homogenisation time.

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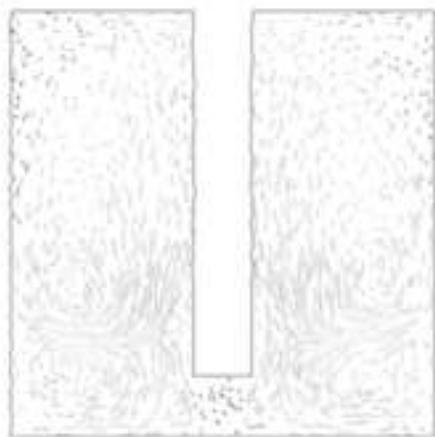


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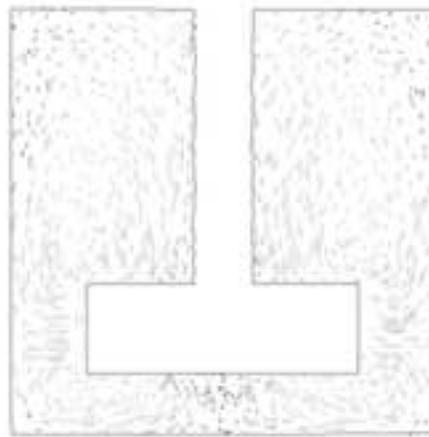


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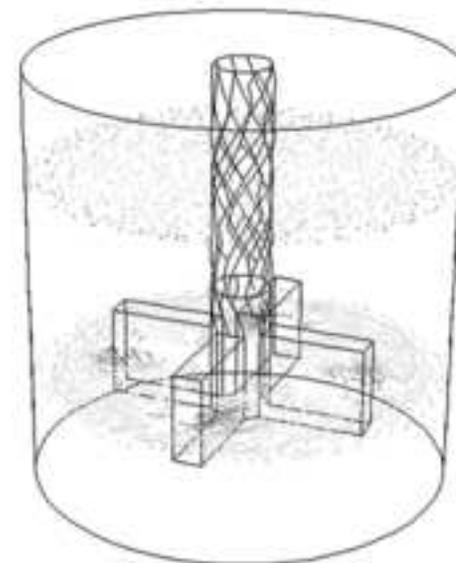
Velocity magnitude (m/s)



a



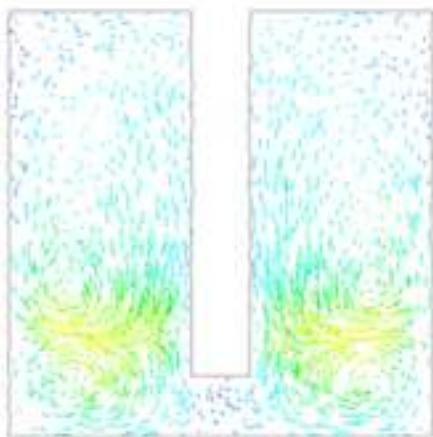
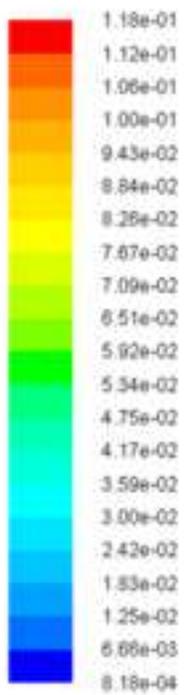
b



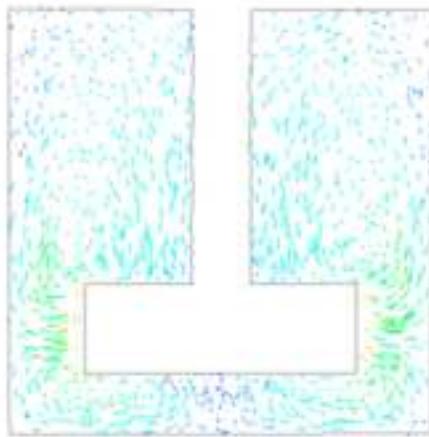
c

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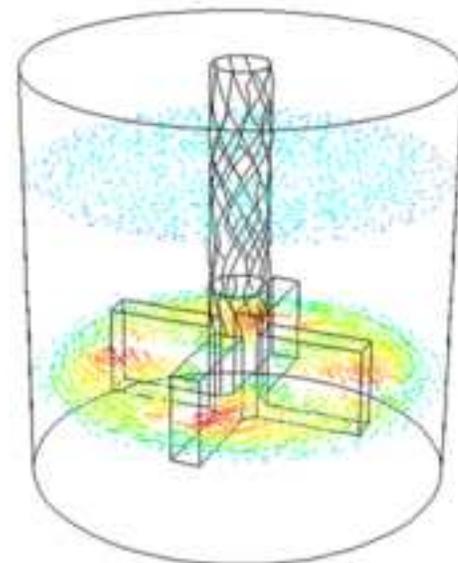
Velocity magnitude (m/s)



a

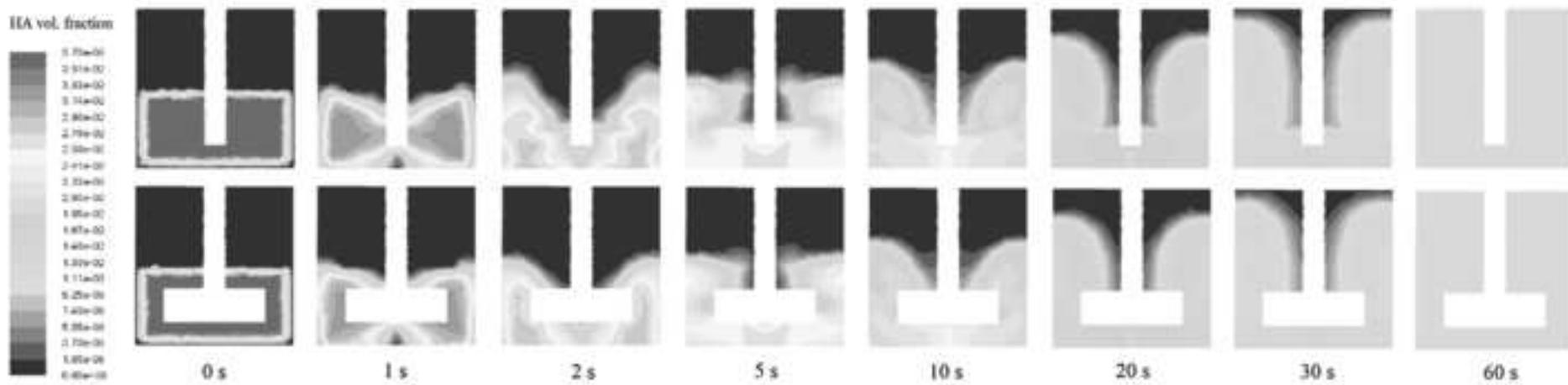


b



c

Fig 4 (B&W, print)



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