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3	Full title: Hierarchical learning of statistical regularities over multiple timescales of sound
4	sequence processing: A dynamic causal modelling study
5	Short title: Hierarchical learning during sound sequence processing: A DCM study
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22 Abstract

23 The nervous system is endowed with predictive capabilities, updating neural activity to 24 reflect recent stimulus statistics in a manner which optimises processing of expected future states. This process has previously been formulated within a predictive coding framework, 25 where sensory input is either "explained away" by accurate top-down predictions, or leads to 26 27 a salient prediction error which triggers an update to the existing prediction when inaccurate. 28 However, exactly how the brain optimises predictive processes in the stochastic and multi-29 faceted real-world environment remains unclear. Auditory evoked potentials have proven a 30 useful measure of monitoring unsupervised learning of patterning in sound sequences through 31 modulations of the mismatch negativity component which is associated with "change 32 detection" and widely used as a proxy for indexing learnt regularities. Here we used dynamic 33 causal modelling to analyse scalp-recorded auditory evoked potentials collected during 34 presentation of sound sequences consisting of multiple, nested regularities and extend on 35 previous observations of pattern learning restricted to the scalp level or based on single-36 outcome events. Patterns included the regular characteristics of the two tones presented, 37 consistency in their relative probabilities as either common standard (p = .875) or rare deviant (p = .125), and the regular rate at which these tone probabilities alternated. Significant 38 39 changes in connectivity reflecting a drop in the precision of prediction errors based on learnt 40 patterns were observed at three points in the sound sequence, corresponding to the three 41 hierarchical levels of nested regularities: (1) when an unexpected "deviant" sound was 42 encountered; (2) when the probabilities of the two tonal states altered; and (3) when there was 43 a change in rate at which probabilities in tonal state changed. These observations provide 44 further evidence of simultaneous pattern learning over multiple timescales, reflected through 45 changes in neural activity below the scalp.

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47 Author summary

48 Our physical environment is comprised of regularities which give structure to our 49 world. This consistency provides the basis for experiential learning, where we can 50 increasingly master our interactions with our surroundings based on prior experience. This 51 type of learning also guides how we sense and perceive the world. The sensory system is 52 known to reduce responses to regular and predictable patterns of input, and conserve neural 53 resources for processing input which is new and unexpected. Temporal pattern learning is 54 particularly important for auditory processing, in disentangling overlapping sound streams 55 and deciphering the information value of sound. For example, understanding human language 56 requires an exquisite sensitivity to the rhythm and tempo of speech sounds. Here we elucidate 57 the sensitivity of the auditory system to concurrent temporal patterning during a sound 58 sequence consisting of nested patterns over three timescales. We used dynamic causal 59 modelling to demonstrate that the auditory system monitors short, intermediate and longer-60 timescale patterns in sound simultaneously. We also show that these timescales are each 61 represented by distinct connections between different brain areas. These findings support 62 complex interactions between different areas of the brain as responsible for the ability to 63 learn sophisticated patterns in sound even without conscious attention.

65 Introduction

66 The alignment of neural activity to reflect recent stimulus statistics is a fundamental 67 feature of the nervous system. Exponential reductions in neural firing with stimulus repetition 68 form the physiological basis for a range of neural processes including sensory adaptation (1-69 4), associative learning (5,6), and simple change detection (7,8). Empirical and theoretical 70 studies also suggest that predictive properties extend beyond single neurons and are applied 71 with greater complexity throughout neural networks to actively generate inferences about 72 future states in a manner consistent with Bayesian learning (9–13). Learnt causal 73 relationships between stimuli and the structure of the environment are adaptive; they permit 74 the pre-selection of adaptive behaviour and conserve processing resources for predicted 75 events (14). Yet, the mechanisms by which the brain can optimise these associations in a 76 complex and ever-changing natural environment remain unclear.

77 The natural environment comprises a multitude of regularities which constantly 78 change and do so at different rates, with varying degrees of reliability. The brain is assumed 79 capable of differentiating these states through a temporal hierarchy where different brain 80 regions are sensitive to representing dynamics at different temporal scales. At the lowest 81 level, sensory cortices encode fast-timescale dynamics underlying simple sensory processing, 82 whilst the highest level involves the prefrontal cortex engaging the more complex functions 83 required to represent slower-changing environmental states such as consistent variability in a 84 given context (15,16). At the neural level, individual neurons have time constants on the scale 85 of milliseconds, post-synaptic gain control modulates precision on the scale of tens or 86 hundreds of milliseconds, whilst connection strengths encode causal regularities that emerge 87 more slowly (17). Computational models incorporating these hierarchical dependencies have 88 been shown to predict actual neural responses and behaviour with a good degree of accuracy, 89 and provide a suitable framework for hierarchical learning over multiple temporal scales (18-

90 20). These hierarchical generative models of predictive coding assume that each neural 91 population must reconcile existing predictions about input from the higher/more frontal level 92 above with sensory input from the lower/more temporal level below, resulting in current 93 input either being "explained away", or a "prediction error" which drives for an update to the 94 existing prediction. At each point these prediction errors are weighted by precision, or the 95 strength and reliability of predictions and input, which determines the rate of new learning or 96 readiness to update predictions accordingly (21,22). Precision weighting is assumed to be 97 implemented as neural gain modulation mediated by classical neuromodulators and N-methyl 98 d aspartate (NMDA) dependent plasticity (23), however empirical data confirming the 99 neurophysiology which supports this complex learning is limited. 100 Auditory evoked potentials (AEPs) provide a mode to study predictive processes 101 within an implicit learning framework. AEPs are automatic, non-invasive and easily 102 translated to populations including infants, clinical groups and the elderly. The N2a or 103 mismatch negativity (MMN) is a negative deflection in AEP amplitude which emerges when 104 comparing the response to an unexpected or low-probability sound to that of an expected, 105 repetitive or high-probability sound (24–26). MMN increases in magnitude with the degree of 106 deviance and is therefore considered an indicator of relative "surprise" (27). Modulations of 107 MMN amplitude have been used as a proxy for surprise in a breadth of studies of perceptual 108 inference and learning, including as evidence for hierarchical learning processes (e.g., 28-109 30). However, the majority of these studies have focused on single-trial MMNs elicited 110 following a simple deviation from a local pattern only (e.g., the traditional oddball paradigm 111 and roving paradigms), and there is limited research into the impact of deviance occurring in 112 a broader statistical context. More recently, growing evidence of the impact of varying 113 degrees of uncertainty on precision weighting has been empirically shown via systematic

modulations of the MMN observed in scalp-recorded AEPs during a multiple-timescaleparadigm (31–35).

116 The multiple-timescale paradigm has used AEPs to reveal hierarchical learning during 117 sound sequences consisting of multiple nested temporal regularities to create varying degrees 118 of surprise. Early studies of this kind employed two tones which were presented with either 119 standard (p = .875) or deviant probability (p = .125; local surprise), and alternated in these 120 roles at a regular rate of every 0.8 minutes in "unstable" sequences or every 2.4 mins in 121 "stable" sequences to create an additional, intermediate level of surprise when the relative 122 probabilities of the two tones suddenly change (31,32,36,37). Despite local equivalence in 123 sound probability ratios between standard and deviant across the two block types overall, 124 sequences designed in this way have demonstrated AEP data consistent with a primacy effect, 125 seen as higher precision in the prediction models for blocks consistent with how the sequence 126 begins (large MMN throughout for the original block) relative to the blocks that represent the 127 alternate probabilities (small MMN initially that increases with local stability within reversed 128 blocks; (35,36,38). This differential precision is likened to lower and higher levels of 129 expected uncertainty respectively, derived from an estimate of the volatility (conditional 130 variance) of the current environment (39). In the absence of any existing priors, the model for 131 the original block type is thought to be formed with high learning rates and high precision as 132 the probabilities are rapidly used to predict the sound environment. The level of uncertainty 133 drops rapidly and significantly over time as the model proves effective in predicting this 134 context. In contrast, the model associated with the reversed block type develops in response 135 to a gross violation in the existing high-precision model (which by then is associated with 136 low expected uncertainty) when the initial deviant begins to repeat triggering a series of 137 prediction errors. In this respect, this second context may be associated with a higher level of 138 estimated volatility in the environment, as the transition to this context represents a

substantial contextual change and learning rates are elevated accordingly. This error
frequency is associated with a high level of surprise triggering a drop in model precision and
an elevation in uncertainty whilst the internal model is updated.

142 The most recent iteration of the multiple-timescale paradigm introduced a third level 143 of patterning within the sound sequences to investigate the sensitivity of the perceptual-144 cognitive system to regularities which unfold over even longer timescales, and the impact on 145 learning when these higher order patterns are violated (34; see also 35). In this study, the 146 previously mentioned "stable" and "unstable" sequences were concatenated in order to 147 introduce a third level of "superordinate" surprise when the regular rate of alternation in tone 148 tendency changes during a sequence by transitioning from "stable" sequence components 149 comprised of 2.4-minute blocks to relatively more unstable sequence components comprised 150 of 0.8-minute blocks, or vice versa. This modification resulted in the presentation of an 151 "increasing-stability" sequence followed by a "decreasing-stability" sequence as represented 152 in Figure 4 (see Materials and Methods).

Specific patterns of AEP modulation observed in this study showed that block type (intermediate-level predictability) remained influential until block length regularity was broken. When the original block type violated block length predictions (i.e., either by changing sooner or later than expected), MMN amplitude to this "first deviant" decreased, likely explained by a significant drop in precision due to superordinate surprise (34; see also 35). In contrast, MMN amplitude to deviants in the alternate block type (i.e., "second deviants") were unaffected by the block length violation.

Whilst multiple-timescale studies have been informative in revealing the sensitivity to hierarchical patterning in sound through distinct modulations of scalp-recorded MMN, it remains unclear exactly where in the temporal hierarchy of the brain these changes occur due

163 to the poor spatial acuity of sensor-level analyses and their limited focus on select electrodes, latencies and components. Here we used dynamic causal modelling (DCM) as an alternative 164 165 method which explains the entire time-course and scalp topography of these data in terms of 166 neurobiologically plausible mechanisms at the source level (i.e., arising from interactions 167 between neural populations within and between sources; 40,41). This method provides a 168 plausible mechanistic explanation of the observed data which cannot be offered by AEP 169 alone, and therefore has greater sensitivity to test assumptions about underlying 170 neurophysiology. DCM is also shown to have a greater sensitivity than neural data to 171 variance in the population which is useful in the investigation of clinical groups (42). 172 The present study will apply DCM to data from the most recent multiple-timescale 173 study by Fitzgerald and Todd (34) with the expectation that we will see evidence of 174 differential modulation of connectivity and precision associated with different levels of 175 surprise (local, intermediate, and superordinate). Timescale effects will be modelled using a 176 DCM of a six-source hierarchical network consisting of sources in bilateral primary auditory cortex (A1), superior temportal gyri (STG) and inferior frontal gyri (IFG) given their best 177 178 model evidence in previous DCM studies of the MMN (43–46). We expect to see the impact 179 of pattern violations expressed differently in the network in a hierarchical manner dependent 180 on the relative timescale of violation. More specifically we hypothesize that 181 predictions/prediction errors will lead to connectivity change at hierarchically lower levels 182 for violations of short timescales, and at higher levels for violations of long timescales. In 183 doing so we seek to further establish the ability of the sensory system to perform sensory 184 learning within unstable and oft-changing environments, and the underlying neural network 185 which is employed in service of this aim.

187 **Results**

188 Sensor space results

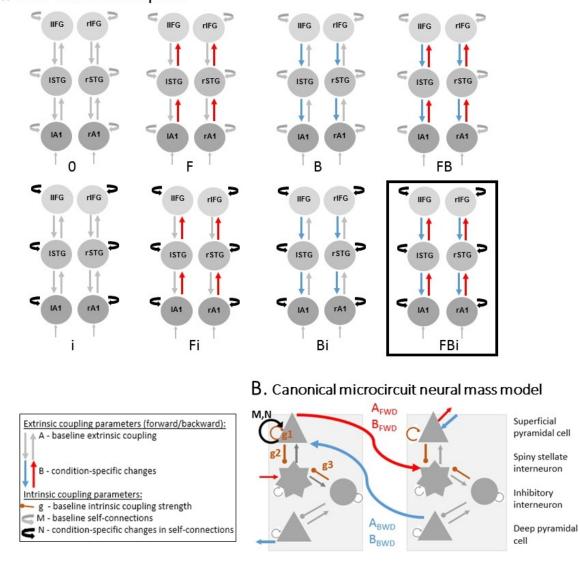
189 The sensor space results derived from the common-average referenced AEPs 190 replicated those observed by Fitzgerald and Todd (34), and a detailed outline is provided in 191 S1 Appendix. Pertinent to the current DCM analysis is the observation that MMN to the first 192 deviant (60 ms) showed clear modulation across the sequence where it was consistently 193 smaller after a change in block length for decreasing stability (t(18) = -2.52, p < .05, 194 corrected) and increasing stability (t(18) = 2.72, p < .05, corrected), with no significant 195 change in MMN amplitude to the second deviant (30 ms) for either conditions. Given that 196 DCM captures the entire epoch, analysis of mean amplitude of the P3 component was also 197 conducted and revealed that P3 was significantly larger (more positive) for the 60 ms tone 198 after a superordinate structure violation for the decreasing stability sequence only t(18) = -2.50, p < .05, corrected). 199

200 Two-tailed t-tests of standard and deviant AEPs (per (62); p < .05, corrected) also 201 replicated the finding that order-driven effects on MMN amplitude were evident in the 202 deviant AEP, and significant differences in the deviant AEP between the two sequences were 203 observed for the 60 ms tone only (i.e. the tone that was heard first as a local deviant). 204 confirming the apparent insensitivity of the 30 ms deviant (i.e., the tone that was heard first 205 as a local standard) AEP to order effects. The confinement of this differential sensitivity in 206 responses to the two tones to the first-deviant AEP specifically emphasises order-driven 207 effects in difference waveforms as related to a difference specifically in how these two 208 contexts are treated, an assertion we aimed to assess using DCM.

209 Connectivity effects

The effects of local deviance (standard vs deviant), superordinate (heard-first vs heard
second) deviance and their interaction were first modelled separately for the 30 ms and 60 ms

212 tone, whilst the effects of intermediate deviance (second/30 ms vs first/60 ms deviant) 213 superordinate deviance (heard-first vs heard second) and their interaction were modelled on 214 both tones together for deviant responses only in the second analysis. In both analyses, effects 215 on connectivity were modelled within a six-source cortical network comprised of bilateral 216 sources A1, STG and IFG. This choice was motivated by the goal of elucidating the 217 hypothesised rostro-caudal temporal hierarchy in the brain where lower and higher levels are 218 differentially sensitive to prediction errors at shorter and longer timescales respectively 219 (18,28). This specific selection of nodes is also in accordance with the sources chosen in 220 previous DCM analyses of auditory MMN paradigms (43,44). The full model permitted 221 changes in ascending, descending, and intrinsic coupling between sources (model FBi in 222 Figure 1), and was compared with a set of reduced models consisting of changes in each 223 parameter alone, each combination, and a null model permitting no changes, resulting in a 224 total of 8 x 8 models for comparison (see Figure 1 for representation of full model space).



A. First-level model space



BMR at the group-level was performed on all 64 models. The overall winning model was the most complex model permitting changes in ascending, descending and intrinsic connections (i.e., model FBi; see Figure 1A). This model was favoured in 100% of individual subjects in all analyses (30 ms and 60 ms tone modelled separately and modelled together), with a posterior probability exceeding 0.99 in all cases.

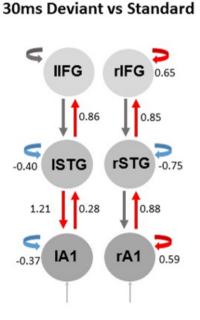
231 Local deviance – Deviant relative to standard

Bayesian parameter averages for each connection type demonstrated similar

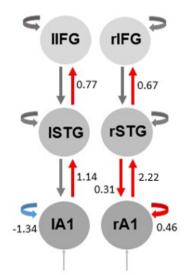
directions of changes in connectivity for both the 30 ms and 60 ms tones when encountered

234 as a local deviant relative to when encountered as a local standard. The direction and 235 magnitude of these significant connectivity changes are displayed in Figure 2, and a full 236 summary of parameter averages is provided in Table S1 and Table S2. Local deviance was 237 associated with an increase in connection strength in all ascending connections for both tones. 238 consistent with increased prediction error signalling. Local deviance was similarly associated 239 with an asymmetrical change in intrinsic connectivity at A1 characterised by decreased 240 intrinsic feedback at left A1 and increased intrinsic feedback at right A1 reflecting changes in 241 the inhibitory self-suppression of prediction error at each of these sources when encountered 242 as a deviant relative to standard. The significant (p < .005) changes in intrinsic connectivity 243 were more widespread across the hierarchy for the second deviant (30 ms) than first deviant 244 (60 ms) tone, with a decreased self-inhibition at bilateral STG and increased self-inhibition at 245 rIFG for the 30 ms tone only reflecting increased and decreased gain of prediction error 246 signalling at each of these sources, respectively. There was a specific unilateral increase in 247 the strength of descending connections from STG to A1 which differed in location for the 248 two tones, occurring from left STG to A1 for a 30 ms deviant, and right STG to A1 for a 60 249 ms deviant.

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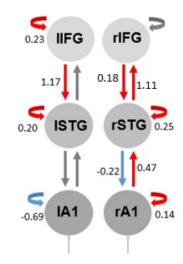
60ms Deviant vs Standard



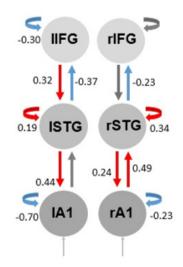
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252 Higher-order effects – First vs Second deviant; Before versus after a block length change Given that sensor space analyses revealed the differences in MMN to be driven by 253 254 modulation of evoked responses to the tones as deviants as in previous multiple timescale 255 MMN studies (e.g., 32,34–36,38), the impact of higher-order changes on the inferential 256 network was assessed in a separate DCM analysis comprised of deviant AEPs only. Planned 257 contrasts between deviant responses to the 30 ms and 60 ms tones, the two sequence 258 components (before and after a change in superordinate structure) and their interaction were 259 conducted to test for significant differences in connectivity associated with an order-driven 260 modulation based on initial tone roles and with a superordinate pattern violation. This analysis revealed significant (p < .005) interactions throughout the network whereby changes 261 262 related to superordinate sequence structure had differential impacts on network connectivity 263 dependent on whether the deviant was a 60 ms or 30 ms tone. This differential effect is 264 visually apparent in the plots of estimated parameter changes for the two tones over the entire 265 sound sequence and specifically after a superordinate change, as displayed in Figure 3. A full 266 summary of parameter averages is provided in Table S3 and Table S4.









269 First, significant differences in connectivity dynamics were observed when comparing 270 the coupling changes associated with the deviant in the second block context (30 ms tone) 271 compared to the deviant in the first block context (60 ms tone) across the overall sequence 272 (Figure 3, left). The 30 ms tone, which was always the second deviant and therefore the 273 initially repetitive standard, was associated with a significantly higher level of increased 274 ascending error signalling, and a significantly higher level of increased inhibitory gain 275 throughout most of the hierarchy (with the exception of IA1 and rIFG) compared to the 60 ms 276 tone. The 30 ms tone was also associated with a higher level of increased descending 277 message passing from higher levels (IFG), and comparatively lower descending message 278 passing from lower levels (rSTG to rA1) relative to the 60 ms tone as deviant. In general, the 279 lower precision of 30 ms prediction errors was therefore associated with higher forward 280 coupling change and higher model revisions after errors (backward coupling changes) 281 relative to the 60 ms tone consistent with models undergoing more revision in the second block than first block context. 282

283 Next, the difference in change in connectivity modulation associated with the deviant 284 in the second block context (30 ms tone) was compared to that of the deviant in the first block 285 context (60 ms tone) as a function of superordinate surprise or before versus after the change 286 in block length. The right panel of Figure 3 therefore reflects the connections that were 287 differentially affected by the interaction between local and superordinate surprise for a 288 deviant in the second block context relative to first block context. As expected, violation of 289 superordinate patterning was associated with significant differences in the changes in 290 connectivity for the two tones which were marked by increased ascending connectivity at 291 lower levels (A1-STG), decreased ascending connectivity at higher levels (STG-IFG) and 292 greater descending connectivity generally for the second deviant when compared to the first 293 deviant after the change in block length. Relative to the first-deviant (60 ms) tone, the

294 second-deviant (30 ms) tone was additionally associated with reduced self-inhibition 295 (increased gain) at bilateral A1 and decreased gain at bilateral STG after the superordinate 296 change. These differences in connectivity change are consistent with greater influence of 297 low-level prediction errors (A1 to STG) for the second deviant compared to the first deviant 298 after superordinate patterning is violated, but a comparatively lower level of impact of 299 higher-level prediction errors (STG to IFG) for the second deviant relative to the first deviant 300 following this change. The observed connectivity changes could be considered consistent 301 with the patterns of MMN amplitude modulation observed here (see Figure S1) and in 302 previous AEP studies (34,35), where the conflict between greater gain at lower levels (PE for 303 local deviations) and greater PE suppression (descending predictions) throughout the 304 hierarchy for the second-deviant tone might explain the smaller net MMN modulation for this 305 tone than the first-deviant tone after the block length change. It is also consistent with the 306 notion that after superordinate change, the occurrences of the first deviant have a more 307 prominent influence over the remodelling of longer-term predictions reflected in the 308 comparatively higher connectivity in forward connections between STG and IFG for the 60 309 ms tones.

310

311 Discussion

The present study involved the novel application of DCM to examine brain responses elicited by the violation of hierarchical regularities in sound. This analysis revealed differential changes in connectivity in underlying brain networks before and after violations of local, intermediate and superordinate patterns during the sound sequence, and differed for the two tones based on their relative probability at sequence onset. These results provide further evidence that the brain is capable of unsupervised learning over multiple timescales simultaneously, and that prediction models are not a veridical representation of the local 319 context but are modulated by higher-order representations. These findings are in concert with 320 order effects previously observed in AEPs from scalp recordings, and give validity to the use 321 of AEPs to study hierarchical inference and learning. Furthermore, the DCM supports a 322 structural and functional architecture that is consistent with hierarchical predictive coding 323 (18), and its neurobiological implementation within the canonical microcircuit model (55). In 324 previous studies of the multiple-timescale paradigm, differential patterns of MMN 325 modulation to the two tones were assumed to reflect how the updating of predictions in 326 response to surprise at a given level will be constrained by internal models held at multiple 327 levels of hierarchical inference. Here we will consider how each of these levels of surprise 328 are substantiated within the hierarchical levels of the DCM, and more specifically how 329 changes in predictions, prediction error and precision are reflected in changes in ascending, 330 descending, and intrinsic connectivity respectively.

331 Local deviance – Deviant relative to standard

332 Local surprise occurred at any given point throughout the sequence and was 333 represented by the occurrence of the relatively less probable deviant among a series of 334 relatively more probable standard tones, as in traditional oddball paradigms. Similar patterns 335 of connectivity change were observed for deviants in both the first and second block context 336 (i.e., both the 60 ms and 30 ms tone as deviant). The increase in inhibitory gain at rA1 and 337 network-wide increase in ascending connectivity are consistent with previous modelling of 338 deviant responses (e.g., (63,64)) and are interpreted to reflect an increase in bottom-up 339 prediction error signalling when a tone is deviant relative to standard. However, the increase 340 in backward connectivity is surprising, and may reflect a true increase in the modulatory 341 influence and/or remodelling of top-down predictions for a deviant relative to standard tone, 342 or an absent decrease relative to standards. In either case it is possible that this anomalous result could reflect the impact of hierarchical learning, unique to the present study's novel 343

modelling of the multiple-timescale paradigm, on how prediction errors are modulated overthe course of the overall sound sequence.

346 The deviant in the second block context (30 ms tone) was further associated with 347 reduced self-inhibition (i.e., increased gain) at bilateral STG, consistent with increased 348 prediction error signalling at higher levels required to increase new learning and override the 349 suppression of PE associated with this tone having previously been redundant, with this 350 reflected in the AEPs as MMN amplitude gradually increasing over time for the second 351 deviant (34). These changes are consistent with a theoretical predictive coding treatment 352 where deviance is assumed to trigger increased ascending error signalling and changes in the 353 self-suppression of prediction errors in order to drive new learning and revise descending 354 predictions, and are in keeping with previous DCM analyses of deviant versus standard tones 355 in auditory oddball and roving standard paradigms (43,44).

356 Intermediate deviance – First vs Second deviant

357 The impact of higher-order surprise was investigated at two levels: intermediate 358 surprise represented by changes in the specific tendencies of each tone between the original 359 to reversed block type, and superordinate surprise represented by the change in block length 360 defined by regular alternation in tone tendencies. Having established the connectivity changes 361 associated with a deviant versus standard tone in general, we looked for distinct patterns of 362 connectivity change in deviant responses before and after these specific points in the 363 sequence, which might reflect how responses to local deviance are weighted by changes in 364 the precision of higher order predictions when violated. The impact of intermediate surprise 365 was investigated by comparing connectivity underlying the response to second deviants (30) 366 ms tone), relative to first deviants (60 ms tone). Relative to the first deviant, second deviant 367 responses were associated with increased descending coupling from bilateral IFG to STG, 368 increased self-inhibition (decreased gain) at higher levels (STG and IIFG) and gain changes

at A1 resembling that seen for a local deviant (decreased self-inhibition at IA1 and increasedat rA1).

371 These patterns of difference in the connectivity changes are largely consistent with the 372 theory that the precision of prediction errors, and subsequently the rate of new learning, were 373 lower in the second block context where the 30 ms tone is deviant. Lower precision is evident 374 in the increased strength of descending connections and decreased gain on superficial 375 pyramidal cells at higher levels reflecting the greater influence of descending predictions (i.e. 376 deviant occurrence leading to model updating) and stronger suppression of ascending 377 prediction errors for this initially redundant tone compared to the 60 ms tone which was 378 initially deviant. Meanwhile, the gain changes at bilateral A1 and increased ascending 379 connections resembling that seen for a local deviant are consistent with the idea that this tone 380 is still recognised as a new deviant, however is likely associated with a slower learning rate 381 within this block due to lower precision. This interpretation is consistent with previous AEP 382 studies of the multiple-timescale sequence demonstrating a gradual increase in MMN 383 amplitude within blocks to the second deviant only, presumably due to a reduced rate of 384 learning about this previously redundant tone as deviant (e.g., 38).

385

386 Superordinate deviance – Before versus after a block length change

The final, superordinate level of surprise inherent in the sound sequence involved violation of the regular rate at which tone probabilities change (i.e., every 0.8 min in unstable components and every 2.4 min in stable components). Learning about this regularity occurred over the longest timescale and was violated only twice within the paradigm– once in the transition from unstable to stable components (increasing-stability sequence), and once in the transition from stable to unstable components (decreasing-stability sequence). When

393 comparing the connectivity associated with each tone as deviant after this superordinate 394 violation, the second context deviant (30 ms tone) was associated with lower ascending 395 connectivity to IFG, greater descending connections, increased gain at A1 and decreased gain 396 at STG relative to the first context deviant (60 ms tone). These differences are consistent with 397 first deviant errors being treated as more informative and the first-deviant context being 398 assigned high model precision, leading to a more significant impact on precision weightings 399 for this tone when higher order patterning is violated. When the block length is violated, the 400 assumptions underlying the block length predictions must be revisited (the model must be 401 updated) and these are purported to be represented in higher levels of the network (18). The 402 comparatively lower level of model precision (less descending influence) for the first context 403 deviant after higher order patterning is broken, alongside the increase in gain and forward 404 error signalling to higher levels (STG-IFG) and lower gain of PE associated with local 405 deviations for the first context deviant tone after the superordinate change are all consistent 406 with remodelling of higher order predictions based on this tone. This result supports the 407 hypothesised role of higher hierarchical levels in longer term pattern learning and an 408 adjustment to the weighting of this influence when these more global patterns are violated.

409 The Bayesian brain hypothesis purports that learning rates are dynamically adjusted to 410 best minimise surprise by differentially weighting prediction errors at various levels to 411 distinguish reliable changes from random fluctuations in the world. We propose that this 412 accounts for the differential patterns of AEP amplitude and associated connectivity changes 413 observed to the two tones throughout the sequence. Namely, that in the absence of any 414 existing priors, high precision is afforded to the binary categorisation of the two tones as 415 more or less probable at sequence onset (local surprise), leading to a lower accumulation of 416 precision in the new tendency of these tones (intermediate surprise) after tone probabilities 417 change. This is observed as a lower precision of prediction errors associated with the

418 previously redundant tone in the second context through decreased gain on deviant response 419 relative to the first context. Similarly, a more distributed pattern of disinhibition of superficial 420 pyramidal cells is seen for a second context deviant following local surprise compared to a 421 first context deviant, likely reflecting the increased learning rate required to override prior 422 learning of the 30 ms tone as uninformative in the first context. Meanwhile, superordinate surprise requires the revision of beliefs about the general volatility of tone probabilities, 423 424 which similarly shows lower precision associated with the second context deviant through 425 less marked gain modulation, and higher influence of descending connectivity compared to 426 the initial deviant (60 ms) tone specifically after the superordinate change.

427 In previous studies, differential modulations of MMN amplitude to the first and 428 second deviant tone have persisted across as many as four repetitions of the same sound 429 sequences (36), and are shown only to be altered when superordinate patterning is abolished 430 or violated (35,65) or if the participant has prior experience with the sounds (48) or prior 431 knowledge of the sequence structure (66). The apparent failure to override a first-impression, 432 even after four repetitions of the same sound sequence, implies that the system maintains 433 differential precision weightings for the two deviants unless a substantive level of surprise is 434 encountered (36). In the present data, these assumptions are reflected in a higher backward 435 coupling strength for the second-deviant 30 ms tone compared to the first-deviant 60 ms tone 436 overall, generally lower precision of the 30 ms than 60 ms deviant, and the precision of 437 prediction errors becoming more precise for 30 ms than 60 ms deviants at lower levels after 438 the superordinate change (at A1), but comparatively less precise than 60 ms deviants at the 439 higher levels (STG) after the higher-order pattern violation when block lengths change.

The results also lend further support to the assertion that perceptual inference engages a hierarchical network architecture where more rostral projections such as those to the prefrontal cortex should be responsible for generating and updating beliefs about longer-term

443 patterns whilst more caudal regions are sensitive to short-timescale change (18). The DCM 444 demonstrated that selective deviant-specific disruptions in these more rostral projections from 445 STG to PFC were primarily seen when the superordinate pattern was violated. These data are 446 consistent with the notion that superordinate patterns must be present and learned for the 447 effect to be seen given previous observation that order-effects are abolished when no 448 superordinate patterning is available (65) or the participant (and therefore the prefrontal 449 cortex and selective attention) is otherwise engaged by a cognitively demanding visual task 450 (66).

451 In the present study we have drawn exclusively on AEPs as a vehicle through which 452 to study perceptual inference and learning, with extension to underlying network connectivity 453 through the application of DCM. The auditory MMN and AEPs more generally are an ideal 454 candidate for tracking this type of statistical learning given the importance of temporal 455 regularity in audition (e.g., to decipher grammar and semantics in human language), the ease 456 at which the statistics of sound sequences can be manipulated, and the established sensitivity 457 of the AEP to changes in these statistics. AEPs further confer an ease of measurement 458 through their accessibility, automaticity and simplicity of the paradigms through which they 459 are elicited, and are suited to the study of more difficult populations such as clinical groups, 460 infants and the elderly. Traditional analyses of the AEP are often restricted to chosen 461 electrodes and latencies based on the component of interest and draw interpretations about 462 neural activity as observed at the scalp. DCM, in contrast, is applied to the entire time-course 463 and sensor space of the epoch and is more sensitive in generating a biologically informed 464 mathematical models of neural activity below the scalp. Whilst DCM has previously proven 465 useful in elucidating the auditory MMN in an oddball sequence, this study is the first to our 466 knowledge to implement DCM of AEPs within a nested hierarchical sequence. Our results 467 confirmed hypotheses about underlying neural mechanisms derived from scalp-level AEP

data (32,34,35,38,48,65,66), and demonstrate the utility of DCM to extend on the use of
AEPs as a proxy for learning processes within multiple timescale paradigms.

The two methods are different in that DCM analysis captures the entire epoch where 470 471 previous AEP analyses of the multiple timescale paradigms have restricted analysis to the 90-472 210 ms window surrounding the MMN. DCM is not limited to a priori components, but 473 rather is sensitive to the contribution of any number of different AEP components occurring 474 up to 300 ms post-stimulus (e.g., P3a) to the observed connectivity change. The changes 475 presented, despite reflecting activity across the entire epoch, remain consistent with 476 interpretations offered for the patterns shown previously in AEPs extracted from a smaller 477 sampling window representative of the MMN, suggesting that the impact of additional components to the observed order effects are minimal, or are subject to the same patterns of 478 479 order-driven modulation as seen for the MMN.

480 A limitation of the DCM is in model selection, where relative evidence is calculated only for the model space which is pre-defined. This entails the possibility that the data could 481 482 be more accurately explained by an alternative model which is not captured in the model 483 space. The chosen model space represents that which is to our knowledge best supported by 484 the literature pertaining to auditory change detection and MMN generation (43-45). We are 485 confident it represents the best estimate of a plausible model for generation of the observed 486 responses based on current knowledge and also, how connectivity changes within a 487 commonly accepted inferential network structure can account for our data. Additional 488 assumptions were made in the process of source selection and again represent best-practice 489 estimation through the use of MNI coordinates consistent with previous DCM studies 490 (43,44,46). A further complication of DCM is that interpreting the complex and nonlinear 491 dynamics of the brain it is designed to capture is not straightforward, as a number of 492 interactions between underlying subpopulations could give rise to the observed connectivity

change (e.g., see (43,67) for discussion). There could therefore be many causes of the
observed connectivity changes, however we have suggested the most likely interpretation that
could be drawn based on previous studies in concert with the present data.

496 Whilst the present study is also limited in its focus on applying DCM to AEPs, recent 497 trial-by-trial analyses have supported Bayesian learning across multiple levels of volatility 498 during a multi-feature visual roving standard paradigm (68), and similar models of 499 hierarchical Bayesian belief updating have also been successfully applied in DCM studies of 500 visuospatial attention (69). The current findings could therefore be interpreted as supporting 501 hierarchical Bayesian inference as a general framework for multi-modal inference and 502 learning in the brain, rather than merely a specific feature of auditory processing. The current 503 results lend support to hierarchical models of Bayesian learning, however may also have 504 parallels to the Hierarchical Gaussian Filter (HGF), a recently formulated generative model 505 of perceptual learning which employs Bayesian principles to trial-by-trial data (20,39,68). 506 The HGF estimates hidden states from limited sensory input using hierarchical belief 507 updating over multiple levels which are representative of the varying degrees of volatility in 508 the environment. For example, the first level represents overall beliefs about possible states, 509 the second level represents the current belief in the relative probability of encountering each 510 state, and a third level represents the likelihood that these probabilities will change – levels 511 which could be considered analogous to the various degrees of patterning in the present 512 study's sound sequence (see (65) for further discussion). Future studies may therefore look to 513 directly embed the HGF model within DCM in order to provide conclusive empirical support 514 for this form of learning within neural circuitry. Further, applications of DCM can contribute 515 to more specific predictions about functional architecture and neurobiology given their 516 increased sensitivity to mechanisms underlying the responses observed at the sensor level 517 (42). Elucidating the neurophysiological basis for perceptual inference and learning in the

healthy brain has further been considered to have important implications for understanding
the etiology of disorders such as schizophrenia where these inference processes differ
significantly (e.g., 66,67).

521 Materials and Methods

522 Participants

523Participants were 19 healthy adults (15 female; aged 18-53 years, M = 25.26 years,524SD = 11.44 years) recruited from undergraduate psychology students at the University of525Newcastle and community volunteers. Exclusion criteria included current diagnosis of, or526treatment for, a mental disorder per *Diagnostic and Statistical Manual of Mental Disorders –*527*Fifth Edition* (47) criteria, history of head injury or neurological disorder, hearing loss,

528 regular recreational drug use, heavy alcohol use or a first-degree relative with schizophrenia.

529 *Ethics Statement*

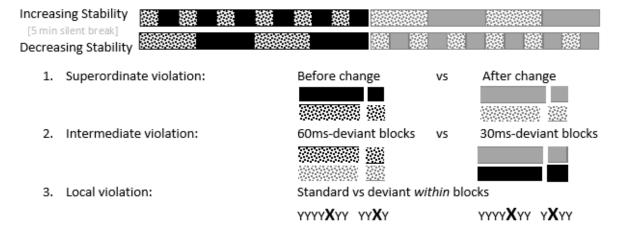
All participants provided written informed consent to participate in the study protocol as approved by the University of Newcastle Human Research Ethics Committee prior to participating (approval number H-2012-0270). Reimbursement was provided in the form of course credit for students or gift vouchers for volunteers as compensation for time and expenses incurred.

535 Stimuli and Sequences

Sound sequences were arranged as outlined by Fitzgerald and Todd (34), and consisted of 1000 Hz pure tones, presented over binaural Sennheiser HD280pro headphones at 75 dB with a 300 ms stimulus onset asynchrony. Sounds were a 30 ms and 60 ms tone created with a 5ms rise/fall time and a 20 ms and 50 ms pedestal respectively. Sound sequences consisted of the two tones alternating in the role of repetitive standard (p = .875) and rare deviant (p = .125) across blocks at two different regular rates to form a stable and

relatively unstable sequence component, which were further arranged to create one
increasing-stability and one decreasing-stability sequence. The general arrangement of sound
sequences was used in a number of previous studies of auditory processing across multiple
timescales (32,35–38,48), with the specific variation used by Fitzgerald and Todd (34)
depicted in Figure 4.

Experiment Structure and Levels of Violation



548

549 Within these sound sequences, local, intermediate and superordinate regularity 550 violations were represented by low-probability deviants, change in tone probabilities between 551 the first and second block contexts (solid vs spotted blocks in Figure 1), and change in block 552 lengths (black vs grey blocks in Figure 1) respectively. Importantly, each stable component 553 consisted of 4 blocks of 480 tones and each unstable component consisted of 12 blocks of 554 180 tones – each adding to a total of 9.6 mins duration, 1960 tones in total and an equivalent 555 number of standard and deviant tones overall. The only difference between sequence 556 components was the maximum period of time over which tone roles remained stable. All 557 participants heard the two sequences in the same order as depicted in Figure 1 - an558 "increasing-stability" arrangement consisting of the unstable followed by stable component,

559	before a "decreasing-stability" arrangement consisting of the stable followed by unstable
560	component. The two sequences were separated by a 5 minute silent break where participants
561	were permitted to move to minimise discomfort and for the predictive system to "reset".
562	Previous multiple-timescale sequences have demonstrated no differences in order-driven
563	effects between counterbalanced sequences when separated by a 2-5 minute break (31).

564

565

5 EEG data collection and pre-processing

566 Fitzgerald and Todd (34) obtained a continuous electroencephalography (EEG) 567 recording during presentation of the sound sequences via a SynAmps2 Neuroscience© 568 system using a 1000 Hz sampling rate, high-pass 0.1 Hz, low-pass 70 Hz, notch filter 50 Hz 569 and fixed gain of 2010. The EEG setup consisted of 64 electrodes in accordance with the 570 International 10 ± 10 system with Modified Combinatorial Nomenclature (49) and included 571 one electrode at the nose and each of the bilateral mastoids for use as reference. Additional 572 electro-oculogram electrodes were placed 1cm from the outer canthi of each eye, and directly 573 above and below the left eye to monitor eye movements. Impedances were reduced to below 574 $5k\Omega$ prior to recording.

575 The continuous EEG recordings from Fitzgerald and Todd (34) were re-processed using Neuroscan Edit[©] software for suitability to the current DCM analysis. Adjustments 576 577 involved band-pass filtering to a range of 0.5 to 40 Hz with 12dB drop-off and zero phase. 578 Manual artefact rejection and bad channel exclusions were carried over from the previous 579 analysis. Eye blink corrections were also completed in the previous analysis using a EEG-580 VEOG covariance analysis, linear regression and point-by-point subtraction procedure (50). 581 Data was epoched from 50 ms pre-stimulus to 300 ms post-stimulus, and any epochs 582 containing frequencies exceeding $\pm 70 \,\mu\text{V}$ discarded prior to averaging.

All subsequent processing steps were undertaken using Statistical Parametric Mapping (SPM) software (version 12, revision 6906). SPM is a freely available academic software package specialised for the spatially extended statistical analysis of brain imaging data and which is suitable for DCM analyses (51).

587 Data were common average referenced as recommended for the application of DCM 588 of EEG data (52) and a revised baseline correction from 25 ms pre-stimulus to 25 ms post-589 stimulus was applied to improve the existing baseline for present purposes. Single-subject 590 and grand averages were subsequently generated for the response to each tone (60 ms, 30 ms) 591 as standard and deviant in each sequence component (stable, unstable) and structure 592 (increasing-stability, decreasing-stability) resulting in 16 grand averages in total.

Data was re-organised for analysis to specifically test the effects of local, intermediate 593 594 and superordinate pattern violations by comparing the same tone as standard versus deviant 595 (local violation), the first-context versus second-context deviant (i.e., 60 ms vs 30 ms tone; 596 intermediate violation), and the two tones as deviants before versus after a change in block 597 length (superordinate violation) respectively. Block length (stable, unstable) was not a factor 598 in the current analysis, given that a change in block length from stable to unstable sequence 599 components produced the same MMN modulation patterns to a change from unstable to 600 stable (i.e., the changes were tied to a change in block length rather than specifically related 601 to block length, (34). Since we focused only on robust effects in the data for subsequent 602 DCM analysis, order was therefore collapsed over block length, with first-heard components 603 (unstable in increasing and stable in decreasing) compared to second-heard (stable in 604 increasing and unstable in decreasing) components (i.e., the sequence components 605 differentiated by black vs grey colouring in Figure 1). The remaining sections will refer 606 exclusively to factors of role (standard, deviant), tone (30 ms, 60 ms) and order (heard-first, 607 heard-second) accordingly. Analysis by role represents local violations by comparing

standard vs deviant, analysis by tone represents intermediate violations by comparing the two
deviant types, and analysis by order represents superordinate violations by comparing the two
global sequence structures.

611 Sensor space analyses

612 The common-average referenced ERP waveforms were analysed to confirm the 613 presence of the same characteristic patterns previously observed in the mastoid-referenced 614 data by Fitzgerald and Todd (34). To assess for sensitivity to deviant tones and changes in the 615 tendency of these tones we compared ERPs to standards and deviants separately for each tone 616 (30 ms vs. 60 ms), using family-wise-error corrected paired *t*-tests to test for significant (p < 1617 .05) differences in these responses at each sampling point within the epoch (corrected over sampling points). For statistical analyses of ERP time-series, data were extracted from the F4 618 619 channel given that both MMN and previous observations of order-driven effects have been 620 shown to be frontal and right-hemisphere maximal (e.g., 34,53,54). Sensitivity to higher-621 order pattern violations was investigated by family-wise-error corrected *t*-tests investigating 622 for significant (p < .05) differences in the ERP to each tone as deviant before and after a 623 change in block length in each condition over the entire epoch at F4.

624 Dynamic causal modelling

625 Further analysis was undertaken using DCM to estimate population output and 626 connectivity parameters associated with the three key patterns observed in AEP data: 627 sensitivity to tone probabilities (local violation), changes in the probabilities of the two tones 628 (intermediate violation), and changes in the volatility of these probabilities (superordinate 629 block-length violation). DCM allows for a mapping from data measured at the sensor level to 630 source-level activity, in a sparse network of interconnected sources, each consisting of a set 631 of neural populations based on a canonical microcircuit architecture (55). The activity in each 632 source evolves as described using coupled differential equations which model the dynamics

of postsynaptic voltage and current in each neural population. These populations (spiny
stellate cells, superficial and deep pyramidal cells, and inhibitory interneurons) have distinct
connectivity profiles of ascending and descending projections linking different sources
(extrinsic connectivity) and coupling neural populations within each source (intrinsic
connectivity). DCM based on canonical microcircuits has been used in several other studies
of mismatch responses (e.g., 56,57), and validated using invasive recordings in humans (58).

639 Model inversion in DCM is susceptible to local maxima issues due to the inherently non-linear nature. To overcome this potential issue we implemented Parametric Empirical 640 641 Bayes (PEB), an iterative hierarchical implementation of the empirical Bayesian inversion 642 method (59) where group-level effects are inferred by fitting the same model to each 643 participant's data under group constraints (e.g., the assumption that model parameters are 644 normally distributed in the participant sample) updating the posterior distribution of the 645 individual DCMs and re-inverting the model over several iterations. This process was applied using the built-in SPM 12 function spm dcm peb fit.m. 646

647 The DCM adopted a standard electromagnetic forward model based on the Boundary 648 Elements Model (BEM) in Montreal Neurological Institute space as the default SPM 12 649 template (52). Lead-fields specified by the forward model were used to reconstruct AEP 650 responses at all electrodes and latencies (0-300 ms) from six cortical sources considered for 651 inclusion in the DCM: bilateral primary auditory cortex (A1), bilateral superior temporal 652 gyrus (STG) and bilateral inferior frontal gyrus (IFG), using the following MNI coordinates 653 (43,46): left A1 [-42, -22,7], right A1 [46, -14, 8], left STG [-61, -32, 8], right STG [59, -25, 654 8], left IFG [-46, 20, 8], right IFG [46, 20, 8]. Changes in extrinsic (between cortical sources) 655 or intrinsic (within cortical sources) connections were quantified as model parameters giving 656 rise to differences between AEPs. The free-energy approximation to model evidence was 657 used as a metric of model fit to the data, penalised by model complexity.

658 DCM analyses were conducted in two steps. The first analysis modelled changes in 659 standard and deviant responses to assess for the expected effects of deviance on connectivity 660 parameters (e.g., ascending connections) and confirm the validity of this application of DCM 661 to data extracted from the multiple-timescale paradigm, whilst also modelling the effect of 662 local violation represented by a deviant relative to standard tone. The second analysis 663 modelled changes in the deviant AEP only given that order-driven effects on MMN 664 amplitude modulations are driven primarily by the deviant AEP (see Results), and focused on 665 differential changes in connectivity associated with intermediate violations (second/30 ms vs 666 first/60 ms deviant) and superordinate violations (before vs after a change in block length). Given that the modulations of interest are based on order rather than tone properties, in the 667 668 first analysis responses to the second deviant (30 ms) and first deviant (60 ms) tone were 669 modelled separately to give a pure measure of network changes to a deviant which were not 670 conflated with the task of explaining variance due to order effects.

671 Individual model inversion was conducted fitting separate models to the two levels of 672 intermediate deviance (30 ms as deviant vs. 60 ms as deviant) over two factors - local 673 deviance (standard versus deviant), superordinate deviance (before and after a change in 674 block length) - and their interaction. In the second analysis tone type was included as a factor 675 within a single DCM to permit the direct contrast of how order driven effects differentially 676 impact connectivity underlying responses to the two tones after a superordinate change. Here 677 individual model inversion was conducted fitting the single DCM over the two factors of 678 intermediate deviance (second deviant/30 ms tone vs.first deviant/60 ms tone) and 679 superordinate deviance (heard-first versus heard-second), and their interaction. In both 680 analyses individual model inversion was applied using empirical priors over the six-source 681 network permitting changes in ascending, descending and intrinsic gain parameters.

682 Bayesian model reduction (BMR) was used to identify the parameter changes that 683 best explained the observed AEP data and estimate the variation in these parameters caused 684 by local, intermediate and superordinate deviations in the respective analyses. BMR uses 685 inversion of the "full" model incorporating changes in all identified parameters to estimate 686 model evidence for a range of "reduced" models where some parameters are not permitted to 687 vary (60). The chosen model space in both analyses examined each combination of changes 688 in ascending connections, descending connections and modulatory gain parameters for each 689 factor, resulting in 8x8 factorial models (ascending, descending, ascending/descending and 690 null, each with and without modulatory gain changes).

691 The winning models were next entered into PEB to hierarchically estimate the 692 variation in parameters which explained systematic changes in response to each factor, 693 comparing a standard relative to deviant in the first analysis, second deviant (30 ms) relative 694 to first deviant (60 ms) tone in the second analysis, and first-heard relative to second-heard 695 sequence component in both analyses. This approach permits estimation of a general linear 696 model for model parameters across individually inverted (first-level) DCMs. Regressors in 697 the second level model included the group mean for each factor (local and superordinate 698 deviance in the first analysis, intermediate and superordinate deviance in the second analysis) 699 and random subject effects. In the first analysis intermediate deviance formed an additional 700 second-level regressor given that the 30 ms and 60 ms tone were modelled separately for 701 each participant. BMR was subsequently applied to identify significant changes in parameters 702 due to these second level factors. Parameters at the second level were derived from the 703 canonical microcircuit model for DCM and included baseline estimates describing extrinsic 704 connections (between sources; A), intrinsic connections (between neural populations within 705 cortical sources; G), and activity-dependent effects on intrinsic connections (modelled as 706 activity-dependent superficial pyramidal cell self-inhibition; M), as well as modulatory

707 parameters describing the effects of the experimental manipulations on extrinsic and intrinsic 708 connections (B) and the activity-dependent effects on intrinsic connections (N). The BMR 709 generated outputs of estimated free-energy approximation to the log-evidence for each 710 second level model (used to compare models and select the winning model), the parameter 711 changes associated with local and superordinate violations, and a Bayesian 95% confidence 712 interval for each as a measure of uncertainty in the estimates. Significance testing followed a 713 recently developed procedure for empirical Bayes that is considered more robust to repeated 714 testing than t-tests and involves estimating the proportion of the probability distribution that 715 falls either side of zero for each parameter against a statistical threshold of 0.995 (61). 716 Acknowledgements 717 KF acknowledges receipt of an Australian Government Research Training Program 718 (RTP) Scholarship. We thank Gavin Cooper for his assistance in programming these 719 experiments and Professor Michael Breakspear for comments on an early version. This 720 research was supported by funds provided by the National Health and Medical Research

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722 References

- Kohn A. Visual adaptation: Physiology, mechanisms, and functional benefits. J
 Neurophysiol. 2007;97(5):3155–64.
- Laughlin SB. The role of sensory adaptation in the retina. J Exp Biol. 1989;146(1):39–
 62.
- Barlow HB, Hill RM. Evidence for a physiological explanation of the waterfall
 phenomenon and figural after-effects. Nature. 1963;200(4913):1345–7.
- 729 4. Hosoya T, Baccus SA, Meister M. Dynamic predictive coding by the retina. Nature.

730 2005;436(7047):71–7.

731	5.	Hebb DO.	Organization	of behavior.	J Clin Psychol.	1950;6(3):307-307.
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- Kempter R, Gerstner W, van Hemmen JL. Hebbian learning and spiking neurons. Phys
 Rev E. 1999 Apr 1;59(4):4498–514.
- 7. Schröger E, Winkler I. Presentation rate and magnitude of stimulus deviance effects on
 human pre-attentive change detection. Neurosci Lett. 1995 Jul 7;193(3):185–8.
- Vlanovsky N, Las L, Nelken I. Processing of low-probability sounds by cortical
 neurons. Nat Neurosci. 2003 Apr 24;6(4):391–8.
- Friston K. The free-energy principle: a rough guide to the brain? Trends Cogn Sci.
 2009;13(7):293–301.
- Friston K. The free-energy principle: a unified brain theory? Nat Rev Neurosci. 2010
 Feb 13;11(2):127–38.
- 11. Rao RPN, Ballard DH. Predictive coding in the visual cortex: a functional

743 interpretation of some extra-classical receptive-field effects. Nat Neurosci.

744 1999;2(1):79–87.

- 745 12. Chopin A, Mamassian P. Predictive properties of visual adaptation. Curr Biol. 2012
 746 Apr 10;22(7):622–6.
- Wang R, Shen Y, Tino P, Welchman AE, Kourtzi Z. Learning predictive statistics:
 Strategies and brain mechanisms. J Neurosci. 2017 Aug 30;37(35):8412–27.
- 14. Laughlin SB, Sejnowski TJ. Communication in neuronal networks. Science (80-).
 2003;301(5641):1870–4.

751	15.	Hasson U, Yang E, Vallines I, Heeger DJ, Rubin N. A hierarchy of temporal receptive
752		windows in human cortex. J Neurosci. 2008 Mar 5;28(10):2539-50.
753	16.	Kiebel SJ, Garrido MI, Friston KJ. Dynamic causal modelling of evoked responses:
754		The role of intrinsic connections. Neuroimage. 2007;36(2):332–45.
755	17.	Friston K, Garrido MI, Gosseries O, Bruno M-A, Boveroux P, Schnakers C, et al.
756		Modalities, modes, and models in functional neuroimaging. Science. 2009 Oct
757		16;326(5951):399–403.
758	18.	Kiebel SJ, Daunizeau J, Friston KJ. A hierarchy of time-scales and the brain. PLoS
759		Comput Biol. 2008;4(11):e1000209.
760	19.	Kiebel SJ, Daunizeau J, Friston KJ. Perception and hierarchical dynamics. Front
761		Neuroinform. 2009;3.
762	20.	Mathys CD, Lomakina EI, Daunizeau J, Iglesias S, Brodersen KH, Friston KJ, et al.
763		Uncertainty in perception and the Hierarchical Gaussian Filter. Front Hum Neurosci.
764		2014 Nov 19;8.
765	21.	Yu AJ, Dayan P. Uncertainty, neuromodulation, and attention. Neuron. 2005 May
766		19;46(4):681–92.
767	22.	Lawson RP, Mathys C, Rees G. Adults with autism overestimate the volatility of the
768		sensory environment. Nat Neurosci. 2017 Jul 31;20(9):1293-9.
769	23.	Friston K. A theory of cortical responses. Philos Trans R Soc L B Biol Sci.
770		2005;360(1456):815–36.
771	24.	Näätänen R, Gaillard AW, Mantysalo S. Early selective-attention effect on evoked

772		potential reinterpreted. Acta Psychol. 1978;42(4):313–29.
773	25.	Näätänen R. Attention and Brain Function. Hillsdale, NJ: Erlbaum; 1992.
774	26.	Näätänen R, Alho K. Mismatch negativity-a unique measure of sensory processing in
775		audition. Int J Neurosci. 1995;80:317–37.
776	27.	Wacongne C, Changeux JP, Dehaene S. A neuronal model of predictive coding
777		accounting for the mismatch negativity. J Neurosci. 2012;32(11):3665-78.
778	28.	Garrido MI, Sahani M, Dolan RJ. Outlier responses reflect sensitivity to statistical
779		structure in the human brain. Sporns O, editor. PLoS Comput Biol. 2013 Mar 28;9(3).
780	29.	Todorovic A, de Lange FP. Repetition suppression and expectation suppression are
781		dissociable in time in early auditory evoked fields. J Neurosci. 2012 Sep
782		26;32(39):13389–95.
783	30.	Wacongne C, Labyt E, van Wassenhove V, Bekinschtein T, Naccache L, Dehaene S.
784		Evidence for a hierarchy of predictions and prediction errors in human cortex. Proc
785		Natl Acad Sci. 2011;108(51):20754–9.
786	31.	Todd J, Provost A, Cooper G. Lasting first impressions: a conservative bias in
787		automatic filters of the acoustic environment. Neuropsychologia. 2011;49(12):3399-
788		405.
789	32.	Todd J, Provost A, Whitson LR, Cooper G, Heathcote A. Not so primitive: context-
790		sensitive meta-learning about unattended sound sequences. J Neurophysiol.
791		2013;109(1):99–105.
792	33.	Todd J, Provost A, Whitson L, Mullens D. Initial uncertainty impacts statistical

793		learning in sound sequence processing. J Physiol Paris. 2016;110(4):497–507.
794	34.	Fitzgerald K, Todd J. Hierarchical timescales of statistical learning revealed by
795		mismatch negativity to auditory pattern deviations. Neuropsychologia. 2018 Nov
796		1;120:25–34.
797	35.	Mullens D, Winkler I, Damaso K, Heathcote A, Whitson L, Provost A, et al. Biased
798		relevance filtering in the auditory system: A test of confidence-weighted first-
799		impressions. Biol Psychol. 2016;115:101-11.
800	36.	Frost JD, Winkler I, Provost A, Todd J. Surprising sequential effects on MMN. Biol
801		Psychol. 2016;116:47–56.
802	37.	Todd J, Heathcote A, Whitson L, Mullens D, Provost A, Winkler I. Mismatch
803		negativity (MMN) to pitch change is susceptible to order-dependent bias. Front
804		Neurosci. 2014;8(180).
805	38.	Todd J, Heathcote A, Mullens D, Whitson LR, Provost A, Winkler I. What controls
806		gain in gain control? Mismatch negativity (MMN), priors and system biases. Brain
807		Topogr. 2014;27(4):578–89.
808	39.	Mathys CD, Daunizeau J, Friston KJ, Stephan KE. A Bayesian foundation for
809		individual learning under uncertainty. Front Hum Neurosci. 2011 May 2;5:39.
810	40.	Friston KJ, Harrison L, Penny W. Dynamic causal modelling. Neuroimage. 2003 Aug
811		1;19(4):1273–302.
812	41.	David O, Kiebel SJ, Harrison LM, Mattout J, Kilner JM, Friston KJ. Dynamic causal
813		modeling of evoked responses in EEG and MEG. Neuroimage. 2006;30(4):1255–72.

814	42.	Brodersen KH, Deserno L, Schlagenhauf F, Lin Z, Penny WD, Buhmann JM, et al.
815		Dissecting psychiatric spectrum disorders by generative embedding. NeuroImage Clin.
816		2014;4:98–111.
817	43.	Garrido MI, Kilner JM, Kiebel SJ, Friston KJ. Dynamic causal modeling of the
818		response to frequency deviants. J Neurophysiol. 2009;101(5):2620-31.
819	44.	Garrido MI, Kilner JM, Kiebel SJ, Stephan KE, Baldeweg T, Friston KJ. Repetition
820		suppression and plasticity in the human brain. Neuroimage. 2009 Oct 15;48(1):269-
821		79.
822	45.	Garrido MI, Kilner JM, Kiebel SJ, Stephan KE, Friston KJ. Dynamic causal modelling
823		of evoked potentials: a reproducibility study. Neuroimage. 2007;36(3):571-80.
824	46.	Phillips HN, Blenkmann A, Hughes LE, Bekinschtein TA, Rowe JB. Hierarchical
825		organization of frontotemporal networks for the prediction of stimuli across multiple
826		dimensions. J Neurosci. 2015 Jun 24;35(25):9255-64.
827	47.	American Psychiatric Association. Diagnostic and Statistical Manual of Mental
828		Disorders. 5th ed. Washington, DC; 2013.
829	48.	Mullens D, Woodley J, Whitson L, Provost A, Heathcote A, Winkler I, et al. Altering
830		the primacy biashow does a prior task affect mismatch negativity?
831		Psychophysiology. 2014;51(5):437-45.
832	49.	American Clinical Neurophysiology Society. American Clinical Neurophysiology
833		Society Guideline 5: Guidelines for Standard Electrode Position Nomenclature 1
834		[Internet]. 2006 [cited 2018 Jun 6]. Available from:
835		https://www.acns.org/pdf/guidelines/Guideline-5.pdf

836	50.	Semlitsch H V, Anderer P, Schuster P, Presslich O. A solution for reliable and valid
837		reduction of ocular artifacts, applied to the P300 ERP. Psychophysiology.
838		1986;23(6):695–703.
839	51.	Statistical Parametric Mapping [Internet]. 2016 [cited 2018 Nov 28]. Available from:
840		http://www.fil.ion.ucl.ac.uk/spm/software/spm12/
841	52.	Litvak V, Mattout J, Kiebel S, Phillips C, Henson R, Kilner J, et al. EEG and MEG
842		Data Analysis in SPM8. Comput Intell Neurosci. 2011;(852961).
843	53.	Giard MH, Lavikainen J, Reinikainen K, Perrin F, Bertrand O, Pernier J, et al.
844		Separate representation of stimulus frequency, intensity, and duration in auditory
845		sensory memory: An event-related potential and dipole-model analysis. J Cogn
846		Neurosci. 1995 Apr;7(2):133–43.
847	54.	Paavilainen P, Alho K, Reinikainen K, Sams M, Näätänen R. Right hemisphere
848		dominance of different mismatch negativities. Electroencephalogr Clin Neurophysiol.
849		1991;78(6):466–79.
850	55.	Bastos AM, Usrey WM, Adams RA, Mangun GR, Fries P, Friston KJ. Canonical
851		microcircuits for predictive coding. Neuron. 2012 Nov 21;76(4):695–711.
852	56.	Moran RJ, Campo P, Symmonds M, Stephan KE, Dolan RJ, Friston KJ. Free energy,
853		precision and learning: the role of cholinergic neuromodulation. J Neurosci.
854		2013;33(19):8227–36.
855	57.	Auksztulewicz R, Friston K. Attentional enhancement of auditory mismatch responses:
856		A DCM/MEG study. Cereb Cortex. 2015 Nov;25(11):4273-83.
857	58.	Papadopoulou M, Friston K, Marinazzo D. Estimating directed connectivity from

858		cortical recordings and reconstructed sources. Brain Topogr. 2019 Sep 9;32(4):741-52.
859	59.	Friston K, Zeidman P, Litvak V. Empirical bayes for DCM: A group inversion
860		scheme. Front Syst Neurosci. 2015;9.
861	60.	Friston K, Penny W. Post hoc Bayesian model selection. Neuroimage. 2011 Jun
862		15;56(4):2089–99.
863	61.	Friston K, Litvak V, Oswal A, Razi A, Stephan KE, van Wijk BCM, et al. Bayesian
864		model reduction and empirical Bayes for group (DCM) studies. Neuroimage.
865		2016;128:413–31.
866	62.	Guthrie D, Buchwald JS. Significance testing of difference potentials.
867		Psychophysiology. 1991;28(2):240-4.
868	63.	Garrido MI, Friston KJ, Kiebel SJ, Stephan KE, Baldeweg T, Kilner JM. The
869		functional anatomy of the MMN: a DCM study of the roving paradigm. Neuroimage.
870		2008;42(2):936–44.
871	64.	Dima D, Frangou S, Burge L, Braeutigam S, James AC. Abnormal intrinsic and
872		extrinsic connectivity within the magnetic mismatch negativity brain network in
873		schizophrenia: A preliminary study. Schizophr Res. 2012 Mar;135(1-3):23-7.
874	65.	Todd J, Petherbridge A, Speirs B, Provost A, Paton B. Time as context: The influence
875		of hierarchical patterning on sensory inference. Schizophr Res. 2018;191:123-31.
876	66.	Frost JD, Haasnoot K, McDonnell K, Winkler I, Todd J. The cognitive resource and
877		foreknowledge dependence of auditory perceptual inference. Neuropsychologia. 2018
878		Aug 1;117:379–88.

Chen CC, Henson RN, Stephan KE, Kilner JM, Friston KJ. Forward and backward
connections in the brain: A DCM study of functional asymmetries. Neuroimage.
2009;45(2):453–62.
Stefanics G, Heinzle J, Horváth AA, Stephan KE. Visual mismatch and predictive
coding: A computational single-trial ERP study. J Neurosci. 2018;38(16):4020-30.
Vossel S, Bauer M, Mathys C, Adams RA, Dolan RJ, Stephan KE, et al. Cholinergic
stimulation enhances Bayesian belief updating in the deployment of spatial attention. J
Neurosci. 2014;34(47):15735-42.
Friston K, Brown HR, Siemerkus J, Stephan KE. The dysconnection hypothesis.
Schizophr Res. 2016;176(2–3):83–94.
Powers AR, Mathys C, Corlett PR. Pavlovian conditioning-induced hallucinations
result from overweighting of perceptual priors. Science. 2017;357(6351):596-600.

893 Figure Legends

894

895	Figure 1. Representation of model space. Effects of local, intermediate and superordinate
896	deviance were modelled within a six-source coupled network comprised of bilateral A1, STG
897	and IFG, and permitting changes in ascending, descending and intrinsic connectivity. The
898	same subset of parameters was allowed to vary for all factors resulting in a total of 8 discrete
899	models shown in Figure 2A. Winning model FBi is indicated by a square outline. Each
900	source within the model space was represented according to the canonical microcircuit neural
901	mass model shown in Figure 2B, where intrinsic coupling parameters estimate the
902	connectivity between superficial pyramidal cells, spiny stellate interneurons, inhibitory
903	interneurons and deep pyramidal cells which contribute to condition-specific changes in
904	extrinsic connectivity between sources.

905

906 Figure 2. Connectivity changes associated with local deviance. Coloured arrows indicate 907 significant increases (red) and decreases (blue) in ascending (upward arrows), descending 908 (downward arrows) and intrinsic (curved arrows) connectivity strength associated with a 30 909 ms (left panel) and 60 ms (right panel) tone when encountered with deviant probability (p =910 .125) as relative to the same tone encountered with standard probability (p = .875). Values 911 represent magnitude of difference in Bayesian parameter estimates relating to the significant 912 modulation of extrinsic connections (B parameters; ascending/descending) and activity-913 dependent effects on intrinsic connectivity (N; within-source). Significance was assessed 914 against a critical value of p < 0.005 using the procedure outlined in the Method.

916 Figure 3. Connectivity changes associated with intermediate and superordinate deviance. 917 Estimated changes in Bayesian connectivity parameters associated with a 30ms tone as deviant 918 compared to a 60 ms deviant in general, reflecting intermediate deviance (left panel), and 919 significant changes in connectivity for a 60 ms deviant as compared to a 30ms deviant 920 specifically after a change in superordinate sequence structure (right panel). Coloured arrows 921 indicate significant increases (red) and decreases (blue) in ascending (upward arrows), 922 descending (downward arrows) and intrinsic (curved arrows) connectivity strength. Values represent magnitude of difference in Bayesian parameter estimates. A critical value of p < p923 924 0.005 was applied for significance testing using the procedure outlined in the Method.

925

926 Figure 4. Representation of sound sequence structure and levels of pattern violation nested 927 within the sound sequence. Local violation occurred within all blocks by presentation of a 928 rare deviant (p = .125; represented as X) amongst a series of repetitive standards (p = .875; 929 represented as Y), intermediate violation occurred following the change in contexts where 930 tone probabilities alternated from a 60 ms deviant and 30 ms standard (first-context block) to 931 a 30 ms deviant and 60 ms standard (second-context block; spotted vs solid blocks), and 932 superordinate violation occurred following a change in block length in each of the sound 933 sequences (black vs grey blocks).

934

936 Supporting Information Legends

937

Figure S1. SPM output highlighting significant spatio-temporal increases (F-test, p < .05family-wise error-corrected) in deviant relative to standard responses across 2D sensor space and time (left panels) and at peak (right panel) for the 30 ms and 60 ms tone.

941

942 Figure S2. Grand average difference waveforms at F4 (where the MMN is maximal) for the 943 second deviant/30 ms (black lines) and first deviant/60 ms tone (grey lines) when heard 944 before (solid lines) and after (broken lines) a change in block length in unstable (left panel) 945 and stable (right panel) sequence components. Shaded bars indicate the latency windows over which mean amplitudes were extracted for quantification of the MMN (160-180 ms) and P3 946 947 (240-260 ms) components, based on a 20ms window capturing the common peak for a 948 majority of individual averages across conditions. Significant differences in mean amplitude 949 are indicated by an asterisk (p < .05).

950

951 Figure S3. Grand average AEPs to the 30 ms (black lines) and 60 ms (grey lines) tone as 952 deviant (A; top panel) and standard (B; bottom panel) when heard before (solid lines) and 953 after (dashed lines) a change in block length for unstable and stable sequence components. 954 Horizontal bars in (B) indicate periods of significant difference between standard and deviant 955 waveforms elicited to the 30 ms (black) and 60 ms (grey) tones across orders, and periods of 956 significant difference between heard-first and heard-second components in the deviant 957 response for the 60 ms tone (blue; one-tailed *t*-test, p < .05, using the procedure outlined by 958 (62) for statistical analysis of EEG waveforms). There were no periods of significant 959 difference in the deviant waveforms for a 30 ms tone when heard first versus heard second.

960 **Tables (Supplementary)**

961

962 30ms, deviant vs standard (local deviance)

Forward	Backward	Intrinsic
0.282*		
0.880*		
0.865*		
0.852*		
	1.211*	
	0.061	
	-0.075	
	0.176	
		-0.371*
		0.586*
		-0.402*
		-0.745*
		0.081
		0.653*
	0.282* 0.880* 0.865*	0.282* 0.880* 0.865* 0.852* 1.211* 0.061 -0.075

Table S1. Estimated changes in forward, backward and intrinsic connections within/between sources associated with a 30 ms tone when encountered with deviant probability as compared to when encountered as a standard. Significant changes are marked by an asterisk, and were assessed as 99.95% of the estimated probability distribution demonstrating a change greater or less than zero.

969 60 ms, standard vs deviant (local deviance)

	Forward	Backward	Intrinsic
lA1-lSTG	1.135*		
rA1-rSTG	2.215*		
ISTG-IIFG	0.770*		
rSTG-rIFG	0.671*		
ISTG-IA1		-0.192	
rSTG-rA1		0.314*	
lIFG-1STG		0.246	
rIFG-rSTG		<-0.001	
rA1			-1.342*
lA1			0.462*
rSTG			-0.254
ISTG			0.210
rIFG			-0.064
lIFG			-0.004

Table S2. Estimated changes in forward, backward and intrinsic connections within/between
sources associated with a 60 ms tone when encountered with deviant probability as compared
to when encountered as a standard. Significant changes are marked by an asterisk, and were
assessed as 99.95% of the estimated probability distribution demonstrating a change greater
or less than zero.

975

976

	Forward	Backward	Intrinsic
lA1-lSTG	-0.057		
rA1-rSTG	0.470*		
ISTG-IIFG	0.033		
rSTG-rIFG	1.11*		
ISTG-IA1		0.010	
rSTG-rA1		-0.216*	
lIFG-1STG		1.168*	
rIFG-rSTG		0.181*	
rA1			-0.686*
lA1			0.144*
rSTG			0.202*
lSTG			0.250*
rIFG			0.228
lIFG			0.147

Table S3. Estimated changes in forward, backward and intrinsic connections within/between
sources associated with a 30 ms tone as deviant compared to a 60 ms tone as deviant.

981 Significant changes are marked by an asterisk, and were assessed as 99.95% of the estimated

982 probability distribution demonstrating a change greater or less than zero.

983

984

985

	Forward	Backward	Intrinsic
lA1-lSTG	-0.018		
rA1-rSTG	0.486*		
ISTG-IIFG	-0.368*		
rSTG-rIFG	-0.225*		
ISTG-IA1		0.437*	
rSTG-rA1		0.244*	
lIFG-1STG		0.316*	
rIFG-rSTG		-0.039	
rA1			-0.702*
lA1			-0.228*
rSTG			0.186*
ISTG			0.337*
rIFG			-0.303*
lIFG			0.147

987 30 ms vs 60 ms deviants after block change (superordinate deviance)

Table S4. Estimated changes in forward, backward and intrinsic connections within/between sources associated with a 30 ms tone as deviant compared to a 60 ms tone as deviant before versus after the change in block length. Significant changes are marked by an asterisk, and were assessed as 99.95% of the estimated probability distribution demonstrating a change greater or less than zero.

993