

Phonocardiogram Classification Using 1-Dimensional Inception Time Convolutional Neural Networks

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Abstract

Murmurs are sounds caused by turbulent blood flow that are often the first sign of structural heart disease. These sounds are detected by auscultating the heart using a stethoscope, or more recently by a phonocardiogram (PCG). We aim to identify the presence, absence, or unclear cases of murmurs, as well as predict normal or abnormal clinical outcome from PCG recordings using machine learning.

We trained and tested two 1-dimensional convolutional neural networks (CNN) on a PCG data set from a pediatric population of 1568 individuals. One model predicted murmurs, while the other model predicted clinical outcomes. Both models were trained to give recording-wise predictions, while the final predictions were given for every patient (patient wise predictions).

This paper describes our participation in the George B. Moody PhysioNet Challenge 2022 whose objective was to identify heart murmurs and clinical outcome from PCGs. Our team, Simulab, trained a clinical outcome classifier that achieved a challenge cost score of 12419 (ranked 14th out of 39 teams) and the murmur classifier achieved a weighted accuracy of 0.593 (ranked 30th out of 40 teams) on the test set.

1. Introduction

Cardiovascular diseases are one of the major causes of death, and represent 32% of all global deaths [1]. Heart sounds provide an important source of information to a clinician in detecting abnormal murmurs which might be a sign of structural heart disease [2]. The most common and cost-effective tool for acquiring heart sounds is the stethoscope [3]. Despite the advancement of new cardiac monitoring methods, the stethoscope still remains an important

tool for first-line cardiac screening, when performed correctly [4]. However, studies show that auscultation using a stethoscope is generally poorly performed both by medical students [5] and physicians [6], and many physicians cannot reliably distinguish abnormal from normal heart sounds, especially in children [7].

A phonocardiogram (PCG) is a digital representation of a heart sound and can be recorded by a phonocardiograph. A phonocardiograph is a stethoscope that transmits the sounds to a digital sampling device instead of transmitting them to the clinician's ears like a stethoscope. Figure 1 show an example of a PCG plotted in the time domain, and also the two most prominent peaks in a cardiac cycle which are called the first heart sound (S1) and the second heart sound (S2). S1 originates from the closing of mitral and tricuspid valves after blood flows from atria to ventricles, while S2 is caused by the closing of the aortic and pulmonary valve after blood is ejected from the two ventricles. Heart sounds are usually auscultated at the four different locations on the chest wall which corresponds to the aortic, pulmonary, tricuspid and mitral valves.

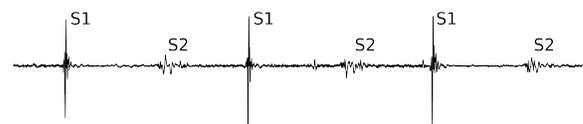


Figure 1. An example of a phonocardiogram showing three cardiac cycles

Back in 1987 Rangayyan, R. M., & Lehner, R. J. stated that: “The heart sound signal has much more information than can be assessed by the human ear or by visual inspection of the signal tracings on paper as currently practiced” [8] and since then, several attempts have been made to pro-

cess [9], analyse [10] and classify PCG recordings using deep learning methods [11].

This paper describes our approach towards achieving the objective in George B. Moody PhysioNet Challenge 2022. We report our methodology and results and from developing two algorithms that identify murmurs as present, absent or unclear and classify the clinical outcome of a patient as normal or abnormal from PCG. Furthermore, we discuss the results and end our paper with a conclusion.

2. Method

We use a supervised machine learning approach, a convolutional neural network (CNN), to detect murmurs and classify the clinical outcome of a patient using a single PCG signal. We implemented the models in Python (3.8.9) using Tensorflow (2.8.2). The code is open sourced and published on GitHub ¹.

2.1. Data

The data set used in this work consists of 5272 PCGs from a pediatric population of 1568 individuals [4, 12]. 3163 PCGs from 942 individuals were used for training. The remaining 2109 PCGs from 149 and 477 patients, only available to the organizers of the challenge, were used for validation and testing respectively. Each patient could have one or more PCG recordings taken from a location close to the aortic valve, pulmonary valve, tricuspid valve, mitral valve or in some cases unknown.

Each patient was labeled with a clinical outcome (abnormal/normal) and murmur (present/unknown/absent), annotated by a clinical expert [3]. In cases of present murmur, the location of the recorded murmur was given in the training set.

2.2. Pre-processing

2.2.1. Signal processing

The PCG signals in the training data were recorded with a sampling frequency of 4000Hz. We downsampled all signals to 100Hz. In addition, we zero padded all signals such that all signals were of a length equal to the longest signal in the training data, which was 6451 samples after down sampling to 100Hz. 6451 samples were also used as the length threshold for the validation and test data after down sampling to 100Hz. Signals with length $l < 6451$ were given a zero-padded tail of length $6451 - l$ and signals longer than 6451 were truncated.

¹This link will be valid after the challenge is finished: <https://github.com/Bsingstad/Heart-murmur-detection-2022-private>

2.2.2. Label processing

The data set was relabeled from patient-wise labeling to recording-wise labeling. This was done by labeling all PCGs from a patient with the same clinical outcome as the original overall label. The recording-wise relabeling of murmurs is shown in Algorithm 1.

Algorithm 1 : Patient to recording wise murmur labels

Input: p = patient, r = PCG record,
 t = total population, l = label
Output: r_l = recording wise labels
for n in t **do**
 if $p_{n_l} = Absent$ **then**
 all r_l **in** $p_n = Absent$
 else if $p_{n_l} = Unknown$ **then**
 all r_l **in** $p_n = Unknown$
 else if $p_{n_l} = Present$ **then**
 for m in p_{n_r} **do**
 $r_{l_m} = Present$
 end for
 end if
end for

2.3. Models

Two classification models were trained; one model to classify murmurs and the other to classify outcomes. Both models were 1 dimensional CNNs with an Inception Time architecture [13]. The murmur model was a multi-class classifier, set to classify whether a murmur was present/absent/unknown in the heart sound recording. The outcome model was a binary classifier used to classify whether the patient would have a normal or abnormal outcome. The murmur classifier was trained using weighted categorical cross entropy, while the clinical outcome classifier was trained using weighted binary cross entropy. The weights in both models were determined to be inversely proportional to the prevalence of the classes.

2.4. Post-processing

The recording-wise predictions from the model were finally converted back to patient-wise predictions. The murmur conversion is shown in Algorithm 2 and the clinical outcome conversion is shown in Algorithm 3.

2.5. Model selection (local development)

To estimate the performance of the models we did local training and validation on the training set, using using 5-fold cross-validation (CV), using 5-fold cross-validation (CV), before submitting the final model to the organizers

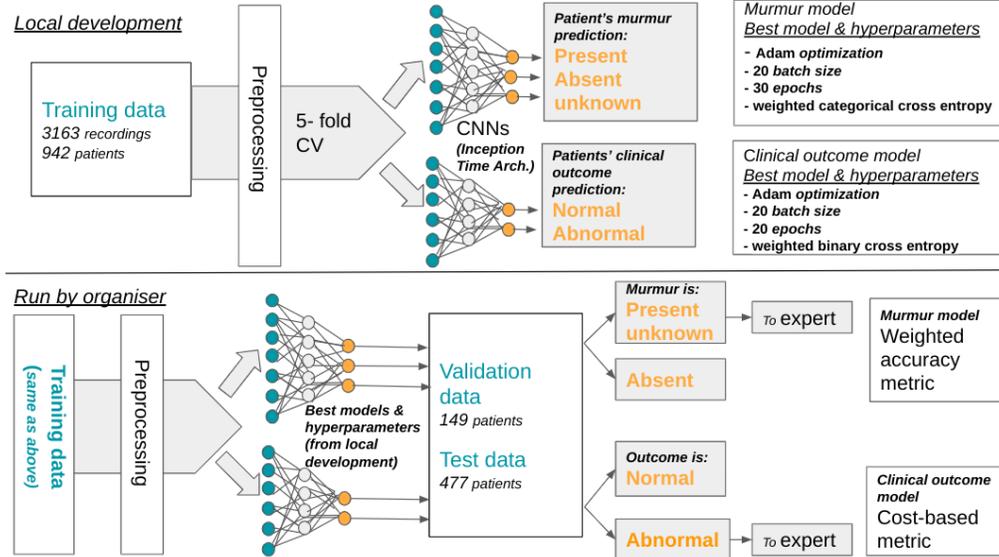


Figure 2. Detailed overview of the local development of the model and the submitted code run by the organizers.

of the challenge. The CV folds were stratified on patient level, and new models were trained and validated each successive round.

Algorithm 2 : Murmur algorithm

Input: p = patient, r = PCG record,
 t = total population, l = label
Output: p_{n_l} = patient wise labels
for n **in** t **do**
 if any r_l **in** p_n = Absent **then**
 p_{n_l} = Absent
 else if any r_l **in** p_n = Present **then**
 p_{n_l} = Present
 else if any r_l **in** p_n = Unknown **then**
 p_{n_l} = Unknown
 end if
end for

Algorithm 3 : Outcome algorithm

Input: p = patient, r = PCG record,
 t = total population, l = label
Output: p_{n_l} = patient wise labels
for n **in** t **do**
 if any r_l **in** p_n = Abnormal **then**
 p_{n_l} = Abnormal
 else if any r_l **in** p_n = Normal **then**
 p_{n_l} = Normal
 end if
end for

2.6. Submitted model

The best models and hyper-parameters from local development were submitted to the organizers using a Docker image. The models were trained on the public training set and then applied to the hidden validation set and the best performing model on the validation set were finally applied on the test set.

The murmur classifier was trained for 30 epochs while the clinical outcome classifier was trained for 20 epochs. Both models were trained using a batch size of 20, and an Adam optimizer starting at a learning rate = 0.001.

3. Results

Table 1 shows the CV results on the training data set as well as the results on the hidden validation and test set. The ranking on the murmur task was determined by the weighted accuracy score. The clinical outcome task on the other hand, used clinical cost score.

Model	Metric	Training	Validation	Test	Rank
Murmur	W. acc.*	0.497 ± 0.083	0.585	0.593	30th
	Cost metric	13158 ± 1283	8866	13134	
	Accuracy	0.446 ± 0.070	0.423	0.497	
	F measure	0.403 ± 0.055	0.384	0.398	
Outcome	W. acc.*	0.713 ± 0.042	0.732	0.703	14th
	Cost metric	12315 ± 903	8720	12419	
	Accuracy	0.510 ± 0.047	0.537	0.537	
	F measure	0.465 ± 0.061	0.530	0.503	

Table 1. Scores obtained by the murmur and clinical outcome classifier on the training set (5-fold cross-validation) and the hidden validation and test set. The ranking is based on the performance on the test set.

* Weighted accuracy

4. Discussion and Conclusion

The challenge scores achieved by the clinical outcome model on the test set were consistent with the performance on the training set. However, the performance on the validation set was significantly better and even outperformed all other participants' models in the challenge. It should be noted that the validation set was relatively small compared to the training and test sets. This could cause a higher variance in performance by chance. Since each team got 10 attempts to test their algorithm on the validation set, we might have indirectly overfitted the models to a data set that is not representing the variation in the training and test set. This emphasizes the importance of having a large enough, diverse and completely untouched data set when testing and reporting results from machine learning studies

Pre-training models were also tested using the 2016 PhysioNet Challenge data set [14, 15]. Different approaches on training the pre-trained models were explored. However, there were no significant improvements during CV on the public training set and the performance on the validation set was actually lower compared to no pre-training.

Both murmur and the clinical outcome classifiers were trained using single PCG recordings, and the auscultation location was not taken into consideration. However, in the preliminary phase of the challenge, we also tested multi-channel PCG classifiers, but they were outperformed by the single-channel classifiers. This observation taken into account in addition to the performance of our classifier and other challenge participants' classifiers, supports the hypothesis that a CNN can detect abnormalities from PCG recordings regardless of the auscultation location. This finding add to the development of CNN-based PCG classifiers. However, further studies are needed to provide an in-depth explanation of how these CNNs interpret the PCGs. A greater focus on the explainability of these models may produce interesting findings that could be of clinical relevance.

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